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Joan Yamil Martinez Western Michigan University, Jnmart@gmail.com

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## APPLICATIONS OF IMAGE PROCESSING TECHNIQUES AND SPATIAL DATA ANALYTICS FOR PRESSURE MAPPING ANALYSIS

by

Joan Yamil Martinez

A dissertation submitted to the Graduate College in partial fulfillment of the requirements for the degree of Doctor of Philosophy Industrial Engineering Western Michigan University April 2020

Doctoral Committee:

Steven Butt, Ph.D., Chair Tycho Fredericks, Ph.D., CPE Lee Wells, Ph.D. Ikhlas Abdel-Qader, Ph.D.

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### APPLICATIONS OF IMAGE PROCESSING TECHNIQUES AND SPATIAL DATA ANALYTICS FOR PRESSURE MAPPING ANALYSIS

Joan Yamil Martinez, Ph.D.

Western Michigan University, 2020

The technological advancements in sensors, monitoring systems, and tracking devices are changing how we study our environment; big data sets are becoming more and more prevalent due to the increase of information gathered with ease. One system benefiting from these technological improvements is pressure mapping technology, an easy-to-use and cost-effective solution for assessing contact pressure distributions. Pressure mapping systems generally produce data sets of very large volume, especially when used for continuous tracking and monitoring, and are widely used for research in fields of ergonomics, sports, industries, and health disciplines.

Pressure mapping systems are particularly important in the study of human-chair seating interactions. Researchers have widely used pressure mapping systems to study these interactions and their relationship with comfort/discomfort across different conditions. The analysis of seating pressure maps usually consists in evaluating descriptive pressure measures and using visual feedback for assessing pressure distributions. Unfortunately, current analytical techniques do not provide clear insights about pressure distribution patterns nor spatial relationships within seating pressure maps; these are needed to further understand human-chair interactions. The need for additional pressure distribution measures, along with quantitative techniques for assessing and comparing pressure maps, have also been emphasized in literature.

This work studies the applications of machine learning, spatial data analytics, digital image processing, and optimal image registration as new techniques for pressure mapping analysis, with the objective of implementing these techniques to pre-process, analyze, and compare seating pressure map images. The results of this study demonstrate the practicality and effectiveness of using these techniques for (1) removing extrinsic pressure artifacts (outliers) by using densitybased spatial clustering, (2) measuring distribution patterns and spatial relationships by using spatial autocorrelation and statistical features of images, and (3) aligning and comparing pressure map by using image registration and similarity/dissimilarity coefficients.

The use of DBSCAN and DENCLUE clustering algorithms were found to be suitable for identifying and eliminating extrinsic pressure artifacts (outliers), with obtained overall accuracies over ninety-nine percent. Moran's I spatial autocorrelation measure, and image statistical features of Skewness, Correlation (GLSD), Gradient Contrast/Mean (GLD), Gradient Second Moment (GLD), and Homogeneity (GLSD) were found to be appropriate for measuring unique aspects of pressure distributions within pressure maps. Image registration based on the minimization of the Mean Square Error (MSE) was also suitable for aligning pressure map images, with similarity and dissimilarity coefficients of Pearson Correlation Coefficient, Minimum Ratio,  $L_1$  Norm, and Intensity Ratio Variance being particularly unique when comparing aligned pressure maps.

These methodologies can help future seating research by providing additional analytical tools for a better understanding of user-chair interactions and their relationships with sitting comfort/discomfort, in both static and dynamic sitting environments. While findings in this study are in the context of task seating (i.e. mousing and typing), these techniques can also be tailored and employed in other seating research applications (e.g., automobile seating, aircraft pilot seats, and paraplegic seating), non-seating pressure map research (e.g., gait analysis, industrial applications, and sports fields), or research studies using spatially related three-dimensional datasets (e.g., surface topography, contour data, and heat maps).

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### Joan Yamil Martinez

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### CHAPTER I

### INTRODUCTION

<span id="page-23-0"></span>The technological advancements in sensors, monitoring systems, tracking devices, and the growth of Internet of Things (IoT) are changing how we interact and study our environment. Big data sets are becoming more and more prevalent due to the increase of information gathered with ease. A demanding emphasis in the analysis of such data sets is currently in place to help and support the decision-making process. One of the technologies benefiting from these improvements is pressure mapping systems, a practical and convenient solution for assessing contact pressure distributions. Pressure mapping systems generally produce data sets of very large volume, especially when used for continuous tracking and monitoring, and are widely used for research in fields of ergonomics, sports, industries, and health disciplines (Fredericks et al., 2016; Makhsous et al., 2012; Misiewicz et al., 2015; Nagel et al., 2008).

Pressure mapping systems are particularly important in the study of human-chair sitting interactions. Researchers have widely used pressure mapping systems to study these interactions and their relationship with sitting comfort/discomfort (Zemp et al., 2016). With employees spending more time than ever in a seated position, studies of sitting comfort/discomfort have been prevalent (Cascioli et al., 2011; De Looze et al., 2003; Openshaw, 2011; Zemp et al., 2015). The advent of computers and visual display units (VDUs) lead to high demands in jobs where tasks are mostly sedentary, with prolonged computer use being now common and expected in current working environments (Afanuh & Johnson, 2017; Studebaker & Murphy, 2014). Office-based workers, in particular, have been reported to spend between four to six hours of their working hours performing sedentary sitting tasks, with a high proportion of their sitting times accrued in bouts of at least 20 or 30 minutes of prolonged sitting (Hadgraft et al., 2016; Thorp et al., 2012).

Prolonged sitting time has been associated with workers' discomfort, dissatisfaction, fatigue and reduced performance (Chester et al., 2002; M. H. Liao & Drury, 2000; Pitman & Ntuen, 1996; Waongenngarm et al., 2015). The decrease in performance, as a result of prolonged sitting and the environmental stressors associated with it, has been a subject of study. As fatigue and discomfort levels increase, workers may shift their attention from the task at hand to the mitigation of discomfort, especially when high levels of discomfort are reported (M. H. Liao & Drury, 2000; Pitman & Ntuen, 1996). Prolonged sitting time may also have a drastic effect in workers' health. Several health issues have been reported due to improper sitting postures and prolonged sitting time with low levels of seating comfort. Musculoskeletal disorders in the back, neck, shoulders, arms and legs have been reported with Low Back Pain (LBP) being particularly common (Zemp et al., 2015, 2016). Lis et al. (2007) remarked that sitting by itself does not increase the likelihood of having LBP but rather the combination of awkward postures and sitting for more than half a workday. A comfortable and ergonomic-oriented working environment should be provided and aimed at promoting employees' health and well-being. Additionally, when considering the task and users' characteristics, matching a proper task chair with an ergonomics training program can be beneficial to worker's comfort and productivity. Studies have documented improvements in productivity and overall efficiency of over nine percent when investing in appropriate and comfortable chairs (Miles, 2001; Peck, 1992).

Researchers and chair manufacturers have constantly studied human-chair interactions across different conditions (Cascioli et al., 2016; Fenety et al., 2000; Makhsous et al., 2012; Stinson et al., 2002). Many of these studies have used objective measures, such as measurements of postures, body movements, electromyography, foot volume change, magnet resonance imaging and motion tracking systems (Zemp et al., 2015); however, the use of pressure measuring systems has been predominant in seating research for being an easy and cost-effective solution to assess the pressure measurements of seat pans and backrests (Zemp et al., 2016).

### <span id="page-25-0"></span>**Pressure Mapping**

Pressure mapping is an evaluation tool for assessing pressure distributions. A pressure mapping system consists of a pressure interface, a data acquisition unit, and a computer software. Different technologies are currently available for pressure measurement systems, with their differences lying in the type of sensor used: capacitive, resistive, piezoelectric, or piezoresistive (Ashruf, 2005; Bloss, 2011). Even if sensor technologies are manufactured under different principles, the underlying concept is the same: to output an electrical signal proportional to the measured pressure (Ashruf, 2005). The sensors in the pressure interface can be arranged as a gridbased mat, as single-point sensors, or designed for specific pressure solutions (see Fig. [1\)](#page-26-1). The sensors' output signals are sent to the data acquisition electronics for sampling and processing, and then sent to a computer (via wired or wireless connection) for collection and analysis using the proprietary software solution provided by the pressure mapping manufacturer.

A pressure mapping system measures the uniaxial pressure loads applied to the sensors, and records them as the interface pressure between two surfaces. Pressure mapping systems do not measure shear or contour forces (Fenety et al., 2000; A. R. Kumar, 2007). The reliability and accuracy of pressure mapping systems have been questioned by researchers. A calibration procedure, where a uniform pressure is applied across the interface, has been recommended by

researchers before a pressure mapping system is used. This procedure minimizes sensors' output variations and system errors, and it also mitigates problems of pressure drift, repeatability, linearity and hysteresis (Misiewicz et al., 2015). Researchers have also concluded that measures of pressure mapping systems are accurate, repeatable, and reliable (Misiewicz et al., 2015; Stinson et al., 2002, 2003).



Figure 1. Pressure mapping systems. Left: Mat (NexGen Ergonomics), Right: Glove (BodiTrak)

<span id="page-26-1"></span><span id="page-26-0"></span>There is no defined protocol for using pressure mapping systems in seating research; however, many researchers agree that pressure measures should be collected after a set amount of sitting time to avoid pressure drift. Several studies have shown that pressure values from pressure mapping systems will increase over time for the first few minutes of sitting time (Crawford et al., 2005; Stinson et al., 2002; Zemp et al., 2016). This increase in pressure has been partially attributed to a phenomenon known as pressure creep, where pressure values increase over time while the load on sensors remain constant (Stinson et al., 2002). Researchers recommend recording pressure maps after the first 2 to 8 minutes of sitting time, where values of pressure measures tend to stabilize after that period (Crawford et al., 2005; Stinson et al., 2002). Grid-based interfaces, or pressure sensing mats, are generally used in seating research. Their main purpose is to assess the contact pressure between a chair and its user. Figure [2](#page-27-1) shows an example of a subject's seating pressure map obtained using a pressure sensing mat. This figure shows values of pressure represented using a colormap, with the center of pressure displayed as a black cell.



<span id="page-27-0"></span>Figure 2. Example of a subject's pressure map (mmHg) during sitting

<span id="page-27-1"></span>Pressure sensing mats are commercially available in many sizes and resolutions. Researchers have used pressure sensing mats with sensors configured in a 15 x 15 array, a 16 x 16 array, or a 32 x 32 array (Crawford et al., 2005; Fredericks et al., 2016; Stinson et al., 2002; Zemp et al., 2016). Measurements of pressure obtained from pressure sensing mats are generally given in units of millimeters of mercury (mmHg) and are generally outputted as stacked columns, with each column representing a pressure map frame. The maximum sampling frequencies are a function of the number of sensing elements, the sensors' technologies, and the data acquisition system's capabilities. Sampling frequencies are generally set between 1 Hz and 10 Hz (Makhsous et al., 2012; Zemp et al., 2016). While more detail is provided when using high-resolution pressure mats (e.g., 32 x 32) and high-frequency data acquisition units (e.g., 10Hz sampling), it is important to note that this combination can easily produce large amounts of data in a short period of time.

Grid-base pressure mapping interfaces such as pressure mats are also prone to interferences due to torque forces, shear forces, pinches, and/or creases; these can create false or unwanted pressure readings in non-contact regions of the pressure interface (see Fig. [3\)](#page-28-1). The detection of these unwanted readings (i.e., extrinsic pressure artifacts) is essential before running any further analysis. Many of the pressure measures depicted in the next section are sensitive to these pressure artifacts, and the removal of these is of vital importance to obtain true and accurate results.



<span id="page-28-1"></span><span id="page-28-0"></span>Figure 3. Example of a subject's pressure map frame with marked pressure artifacts

### <span id="page-29-0"></span>**Seating Pressure Measures**

Researchers have used various seating pressure measures when assessing user-chair interactions during sitting (Butt et al., 2005; Fenety et al., 2000; Titus & Polgar, 2009; Zemp et al., 2015, 2016). [Table 1](#page-29-2) shows a comprehensive list of pressure measures commonly used in seating research along with their definitions.

<span id="page-29-2"></span>

<b>Seating pressure measure</b>	<b>Definition</b>	
Sum of pressure	Total amount of pressure of all sensors	
Mean pressure	Average of all non-zero sensor values	
Maximum pressure	Highest individual sensor value	
Contact area	Number of sensors with non-zero values	
Center of pressure	Point of application of the resultant forces of	
	all non-zero sensor values	
Coefficient of Variation	Ratio of the standard deviation of pressure to	
	the average pressure	
Pressure gradient	Change in pressure per unit distance for each	
	individual non-zero sensor value	
Maximum pressure gradient	Highest pressure gradient	
Mean pressure gradient	Average of pressure gradients	
$IT*$ dispersion index	Ratio of sum of pressure under ischial	
	tuberosities in relation to sum of pressure	

<span id="page-29-1"></span>Table 1. Seating pressure measures commonly used in seating research studies

\*Ischial Tuberosities

Pressure measures described in [Table 1](#page-29-2) were shown to be useful in describing human-chair interactions (Zemp et al., 2015). Most of these measures rely on basic measures of pressure map readings (e.g., average, maximum, and standard deviation), while others require expert knowledge to locate specific regions of interest (e.g., IT dispersion index). Unfortunately, many of these seating pressure measures have some limitations when describing the spatial relationship or pressure distribution patterns within a pressure map. Figure [4](#page-30-2) shows examples of pressure maps from two different subjects during sitting. This figure shows significant differences between respective pressure maps in terms of the shape, location, and pressure distribution patterns. However, when calculating commonly used pressure measures, such as sum of pressure, contact area, or coefficient of variations, there are no substantial differences between these measures (see [Table 2\)](#page-30-3). Due to information loss, one might incorrectly conclude that no significant differences are present between these pressure maps from the perspective of these objective measures. New pressure mapping measures are needed to detect these differences by recovering information loss.



<span id="page-30-2"></span><span id="page-30-1"></span>Figure 4. Example of subjects' pressure map differences during sitting

<span id="page-30-3"></span>

<b>Pressure measure</b>	<b>Sample 117-1-958</b> (Left)	<b>Sample 109-1-1141</b> (Right)	<b>Relative</b> $\Delta$ (%)
Sum of pressure (mmHg)	10,246.31	10,237.17	$-0.09\%$
Contact area	384	398	3.65 %
Coefficient of Variation	0.71	0.72	1.41 %

<span id="page-30-0"></span>Table 2. Seating pressure measures for pressure maps shown in Figure [4](#page-30-2)

Researchers have used the visual feedback provided by the pressure mapping systems' software as a way to identify differences or similarities between pressure maps (Stinson et al., 2003; Titus & Polgar, 2009). However, visual feedback assessment is not a practical approach when comparing numerous subjects' pressure maps, or when assessment of continuous pressure maps is needed during dynamic sitting. The need for new seating pressure measures and comparative techniques for pressure maps have also been emphasized in current literature (Zemp et al., 2015, 2016). These new techniques should be cross-functional for applications in static (i.e., single map) and dynamic (i.e., sequential temporal maps) environments.

The focus of this research is to study the applications of unsupervised machine learning techniques, spatial data analytics, digital image processing, and optimal image registration methods as additional analytical tools for pressure mapping analysis. The objectives are to (1) introduce new techniques for pre-processing pressure maps (data cleansing), (2) introduce new pressure measures, and (3) introduce a toolset for aligning and comparing pressure maps. New analytical tools are discussed and presented in the context of seating research, but extensions to other potential applications in research using non-seating pressure maps are briefly discussed in the conclusions.

A literature review is presented in the next chapter where the use and practicality of current seating pressure measures are discussed. A review of current analytical techniques used in dynamic sitting research and methods for pressure map aggregation/comparison is also presented. Literature on the use of interdisciplinary tools and their application in the context of seating research is also examined.

### CHAPTER II

#### LITERATURE REVIEW

#### <span id="page-32-1"></span><span id="page-32-0"></span>**Pressure Measures**

Researchers, along with chair manufacturers, have conducted sitting research using pressure mapping systems across different conditions (Crawford et al., 2005; Fenety et al., 2000; Fredericks et al., 2016; Makhsous et al., 2012; Stinson et al., 2002; Zemp et al., 2016). Zemp et al. (2015) examined the relationship between subjective comfort/discomfort and pressure measurements while sitting in office chairs. In their literature review, the authors identified several pressure measures used by researchers in their studies: sum of pressure, average pressure, peak pressure, contact area, and center of pressure. While some of these measures were suggested as suitable measures for assessing comfort/discomfort when sitting in office chairs, the authors emphasized the importance of using different parameters of pressure distribution, with applications in both static and dynamic environments, to further evaluate human-chair interactions.

Zemp et al. (2016) also evaluated the relationships between specific pressure measures and their usefulness in differentiating pressure distributions between office chairs. The authors listed several pressure measures such as mean pressure, pressure standard deviation, contact area, mass/force, peak pressure and transverse pressure gradients as commonly used among researchers. Measures of peak and mean pressures were particularly highlighted as the only measures used for evaluating and identifying different among the different office chairs and seating positions. The

authors also emphasized the need for suitable pressure measurements and/or methodologies in order to compare office chairs or seating positions.

In the study conducted by Zemp et al. (2016), another main objective was to understand the inter-relationships and correlation between pressure measures during sitting. To achieve this, the authors conducted a study using 20 subjects (15 males, 5 females), nine selected office chairs from six different manufacturers, and two pressure sensor mats placed on both the backrest and seat pan of each chair. The study task simulated the use of a visual display unit (VDU) in a workplace environment by requesting subjects to choose a sitting posture and place their fingers on a keyboard while fixing their eyes on the screen. After a one-minute sitting settling time, the authors obtained the average pressure readings collected during a 5-second time interval and proceeded to calculate various common measures of pressure distribution.

Early in the study, Zemp et al. (2016) emphasized the need of new pressure measures; however, the authors calculated seating pressure measures commonly used in the literature: peak pressure, mean pressure, standard deviation of pressure, total contact area, and force. The authors also included measures of pressure gradient, and defined the gradient as the geometrical addition of the pressure derivate of the two sensor mat directions  $(x, y)$  resulting in a  $m - 1 \times n - 1$ matrix (Zemp et al., 2016, p. 4). With the gradient matrix, the authors calculated measures of maximum gradient, mean gradient and standard deviation of the gradient. Partial correlation analysis was used as a dimension reduction technique to isolate possible meaningful pressure measures for evaluating office chairs. The authors found that four measures (contact area, force, maximum gradient, and mean gradient) could describe pressure distributions on the seat pan, and three measures were needed for the backrest (standard deviation of pressure, force, and standard deviation of gradient).

As one of the key objectives in the study was to evaluate the effectiveness of the pressure measures in comparing pressure distributions between office chairs, the use of the reduced set of measures – found during partial correlation analyses – to measure their effectiveness in comparing pressure distribution among different office chairs would have been insightful. However, the authors decided to use the entire set of calculated pressure measures during their analysis. Results from the study indicated that office chair differences were meaningful when evaluating the seat pan measures of max gradient, mean gradient, and standard deviation of gradient. The study also found that all measures, with the exception of contact area, were meaningful in finding differences between the backrests of the office chairs during a reclined position – when subjects where in full contact with the backrest. Zemp et al. (2016) acknowledged that differences in seat pan and backrest pressure measures among office chairs can be caused by many unknown factors, and that studied pressure measures were also limited to static evaluations of pressure distributions within their research work.

### <span id="page-34-0"></span>**Dynamic Sitting**

Research has also shown that sitting is a dynamic activity (Fenety, 1995; Fleischer et al., 1987). Seated subjects move continuously and more often according to tasks demands (Fenety et al., 2000). Dynamic sitting is considered a natural behavior for prolonged sitting subjects. It is common for subjects to constantly move to: (1) avoid undesirable static work postures, (2) reduce the discomfort from static loadings, and/or (3) increase the blood flow in weight bearing regions of the buttocks (Butt et al., 2005; Winkel, 1986). The use of dynamic sitting pressure measures, for analysis in continuous sitting applications, could be useful in understanding subjects' sitting behavior and user-chair dynamic interactions.

Bhatnager et al. (1985) and Fenety et al. (2000) have studied, to some extent, the relationship between discomfort and movement; both suggesting that sitting discomfort and seated movements are time dependent, where movements increase over time possibly due to discomfort. Others researchers have successfully incorporated continuous pressure measures, such as center of pressure, during in-chair-movement in their studies (Cascioli et al., 2016; Fenety et al., 2000). Unfortunately, relying solely on tracking and monitoring of the movement of the center of pressure does not provide clear insights about pressure distribution patterns during dynamic sitting (e.g., positional shifts, dynamic pressure redistributions, and/or postural changes).

Fujimaki & Mitsuya (2002) proposed the use of neural networks as an evaluation method for dynamic body pressure distributions. The authors found that it was possible to evaluate dynamic pressure mapping data by measuring the changes in ignited neurons over time. These neurons were then used as input for a clustering algorithm to identify pressure patterns related to discomfort. A drawback of tracking changes in neurons is that neural networks are created in a subject-by-subject basis and cannot be used as a generalizable measure of dynamic pressure redistributions.

### <span id="page-35-0"></span>**Pressure Maps Aggregation**

Standardizing and aggregating pressure maps have also been discussed in the literature. Interfaces in pressure mapping systems are usually configured for high sensitivity, making them capable of recording minor variations of pressure during a testing period. Some pressure mapping systems include data acquisition units that are also capable of recording many readings over a short period of time when using high frequency sampling. Nevertheless, results from pressure mapping analyses are often based on few pressure map readings collected in a short period of time. Some
researchers have used a single pressure map frame for their analyses, while others have used the average of pressure maps collected in less than a five seconds period – a technique commonly used for aggregating pressure maps (Butt et al., 2005; Zemp et al., 2016).

Since pressure mapping systems record raw pressure, direct comparison between subjects' pressure maps is often not appropriate due to differences in subjects' anthropometry. Butt et al. (2005) proposed a methodology for aggregating multiple pressure map readings into a standardized composite pressure map. The methodology described in the study use averages of multiple pressure maps frames, from an individual's recording session, to create an aggregate map. The aggregate maps were then normalized using the maximum pressure value recorded in the map. The resulting aggregate pressure maps are unitless and used to compare pressure maps between subjects. This aggregation method could also be useful when comparing within-subject pressure maps (e.g., different time intervals, different chairs used, or a pre- and post- clinical intervention). A composite pressure map method was also proposed by the authors where the unitless pressure maps were combined using unweighted averages.

#### **Image Processing**

Tan et al. (2001) speculated that pattern recognition algorithms developed for computer vision could be applied for interpreting sitting postures from the analysis of pressure distribution data. The authors introduced pattern recognition techniques using principal components analysis on grayscale images of pressure maps. Techniques such as these have been previously applied to the problem of computer face recognition (Pentland et al., 1994; Turk & Pentland, 1991). Tan et al. (2001) described that one of the disadvantages of using principal component analysis, in the

context of seating pressure distributions, is the lack of physical interpretations associated with eigen-posture spaces (p. 267).

Techniques from computer vision and image registration fields have been extensively applied to medical imaging (Kurani et al., 2004; Oliveira & Tavares, 2014; Tang & Chen, 2012); these techniques are primarily used to find matching alignments of medical images (Fig. [5\)](#page-37-0). Alignment of medical images is required when working with different imaging sources (e.g., tomography, magnetic resonance imaging, and positron emission tomography) or when working with spatiotemporal image sequences. Image processing techniques are also used to measure the similarity relationship between sets of images, extract global image descriptors, and/or apply image transformation functions (Goshtasby, 2012).





Figure 5. Magnetic resonance scan (left), Scanned brain tissue section (right) Source: Left (Januschka, 2006) CC BY-SA 3.0, Right (Dilmen, 2005) CC BY-SA 3.0.

<span id="page-37-0"></span>Bogie et al. (2008) introduced a multistage Longitudinal Analysis and Self-Registration (LASR) technique that emphasizes in real-time within-subject seating pressure image analysis. Unfortunately, the LASR algorithm requires certain conditions to be met for it to be implemented successfully. The algorithm assumes that the imaging scale is constant over time and that a symmetric pressure map is present. Pressure map symmetry is particularly important as the algorithm uses the midline of the pressure map image as a registration landmark. Other requirements include a replication of the seating position between evaluations, and collecting pressure maps with easily-identified pressure landmarks. Even with proper conditions in place, authors could see misalignments between pressure map images after applying the LASR algorithm.

While the benefits of introducing image processing techniques in the analysis of pressure mapping are evident, no other additional studies have been found to date where extensive use of image processing techniques are used for evaluating sitting pressure maps.

# **Spatial Data Analytics**

The evolution of Geographic Information Systems (GIS) has been possible thanks to advancements and developments in the field of spatial data analytics (Goodchild & Haining, 2003). Spatial data analysis is dynamically integrated with GIS to allow the manipulation of raw geographical, topological, and geometric information to analyze possible spatial relationships (Anselin, 1992). Many geographically-based studies require use of spatial analytics to find such relationships, with many implementing spatial dependency or autocorrelation measures in their studies (Banerjee, 2016; Menafoglio & Secchi, 2017; Reibel, 2007).

Applications and techniques used in spatial data analytics can be extended for evaluating and analyzing the spatial relationships in pressure maps. Grid-base pressure interfaces (i.e., pressure mats) measure and record pressure readings in a two-dimensional space. The resulting pressure maps can then be rendered as three-dimensional (3D) topographic surfaces by using the measured values of pressure on the z-axis (see Fig. [6\)](#page-39-0). To date, no studies have been found where spatial data analytics have been introduced for evaluating pressure maps.

Implementing spatial data analytics in pressure mapping analysis, while manipulating pressure maps as geographical and/or topographical surfaces, could help in identifying spatial relationships or space features descriptors. In particular, the use of spatial clustering can be a viable pre-processing technique for cleaning extrinsic pressure artifacts and outliersin raw pressure maps. To date, no studies were found where spatial outlier detection techniques are used in pressure mapping applications.



<span id="page-39-0"></span>Figure 6. Example of a 3D surface representation of a subject's pressure map frame

# CHAPTER III

# RATIONALE AND OBJECTIVES

### **Problem Statement**

Researchers have relied on pressure mapping systems to study human-chair-comfort interactions under various sitting conditions (Cascioli et al., 2016; Crawford et al., 2005; Fenety, 1995; Fenety et al., 2000; Fredericks et al., 2016; Higer & James, 2016; Stinson et al., 2003; Zemp et al., 2016). These systems collect pressure maps readings and analyze pressure measures such as sum of pressure, average pressure, peak pressure, contact area, coefficient of variation, and center of pressure. While some pressure measures have been considered suitable for assessing humanchair interactions and their relations to seating comfort/discomfort, researchers have emphasized the importance of using different measures of pressure distribution to further understand these interactions (Zemp et al., 2015).

Many of the analytical tools used in sitting research rely on simplified measures of pressure, such as calculating basic descriptive measures of pressure (see [Table 1\)](#page-29-0) or tracking of the center of pressure during dynamic sitting. These measures do not provide clear insights about spatial relationships (e.g., pressure correlation, location, and orientation) or pressure distribution patterns (e.g., pressure continuity, localized gradients, and homogeneity) in static or dynamic pressure maps. Furthermore, there are very few studies examining comparative techniques for seating research using pressure mapping technology; these techniques are important for the analysis and comparison of within-subject or between-subjects pressure maps.

Butt et al. (2005) proposed aggregation and normalization methods for comparing pressure maps, however, the described methods required pressure maps to be invariant to a maps' position and orientation. One important factor that needs to be considered when comparing or measuring similarities between pressure maps is scaling. Differences in subjects' anthropometry not only affect the magnitude of pressure readings, but the size and shape of the pressure maps is also affected by anthropometric differences. While scaling algorithms can be implemented for comparing pressure maps, it is not appropriate for research involving human subjects (e.g., seating research). Scaling algorithms will distort subject's anthropometry and cover dissimilarities due to true differences in size between subjects.

The need for new analytical tools for pressure mapping is clear. The following is a list summarizing some of the drawbacks of currently used pressure mapping measures and comparative techniques in the context of seating research.

- (1) Common pressure measures, such as sum of pressure, contact area, and coefficient of variation, lack information in regard to spatial relationships, pressure distribution patterns, localized gradients, or homogeneity within pressure levels.
- (2) Current dynamic measures, including center of pressure, do not provide clear insights about changes in pressure distribution patterns during positional shifts and/or postural changes.
- (3) The use of visual feedback assessment is not a practical approach for comparing pressure maps. Current quantitative comparative techniques expect pressure maps to be in a similar location and orientation, while other require certain conditions such as pressure maps symmetry and identifiable pressure landmarks to be met (e.g., LARS). Additionally, these quantitative techniques mostly rely on calculating individual differences between pressure readings; there is a need for global comparative measures with undemanding assessment.

# **Research Objective**

To address many of the drawbacks of current pressure mapping analysis, this study sought to evaluate new potential pressure measures and new methodologies for comparing pressure maps by using interdisciplinary tools from image processing and spatial data analytics. In a specific manner, the objectives of this study were to:

- (1) introduce methods for detecting and removing extrinsic pressure artifacts (i.e., pressure reading outliers) by implementing unsupervised machine learning and spatial data clustering as a pre-preprocessing data cleansing technique;
- (2) introduce new pressure measures, for both static and dynamic settings, by evaluating measures in spatial data analytics, digital image processing, and use of statistical features of images as new pressure measures; and
- (3) introduce a toolset for aligning and comparing static and dynamic pressure maps by using optimal image registration methods and similarity/dissimilarity coefficients.

Proposed pressure measures and analytical tools are discussed and presented in this study in the context of seating research, but extensions to other potential applications in research using non-seating pressure maps are briefly discussed in the conclusions.

### **Study Significance**

Findings from this study are aimed to providing researchers additional analytical tools for a better understanding of user-chair interactions, in both static and dynamic sitting environments, and to help further evaluate sitting comfort/discomfort. Concurrent validation of potential pressure measures is investigated by studying their relationship to commonly used pressure measures, with possible use and interpretations in the context of human-chair interactions.

# CHAPTER IV

# METHODS AND PROCEDURES

To evaluate potential techniques for pre-processing, measuring, and comparing pressure maps, a previously collected dataset containing a number of seating pressure maps is used in this study. Information about the participants, apparatus, and data collection procedures used for creating this dataset is discussed early in this chapter.

This chapter also introduces the spatial data analytics and image processing techniques that were evaluated as new methodologies for pressure mapping analysis. Presented techniques will be grouped according to their discipline and purpose as per the following categories: (1) spatial clustering, (2) spatial autocorrelation, (3) image statistical features, and (4) image registration and similarity/dissimilarity coefficients. In alignment with these categories, this study is divided in the following four research steps:

- (1) Evaluate the use of density-based spatial clustering techniques as pre-processing techniques for detecting and removing extrinsic pressure artifacts (i.e., outliers) within seating pressure maps.
- (2) Evaluate the use of spatial autocorrelation measures as new pressure measures for static and dynamic seating pressure map applications.
- (3) Evaluate the use of first-order and second-order image statistical features as new pressure measures for static and dynamic seating pressure map applications.

(4) Evaluate the application of image registration techniques as a pre-processing technique for aligning and matching pressure maps, and the subsequent use of similarity and dissimilarity coefficients as global comparative measures between registered pressure map images.

Thorough descriptions of the techniques and methodologies used in this study are presented in this chapter Details about data sampling strategies, testing procedures, and research outcomes are also presented for each research step. A case study is also used to demonstrate the use and application of selected techniques and methodologies under a dynamic sitting environment.

# **Dataset**

As explained earlier in this chapter, the dataset used in this study was collected previously, and it was used in studies where results from an applied-research perspective were reported (Hammond et al., 2018; Martinez et al., 2018). This dataset was originally collected to evaluate human-chair interactions under user-defined seat pan contours. These studies were approved by Human Subjects Institutional Review Board at Western Michigan University (see [Appendix A\)](#page-241-0).

This research uses the information of the pressure maps included in the dataset as a testing and validation platform for the various techniques presented in this chapter. A brief description of the participants, testing apparatus, and collection protocol used to create the dataset is described in the following subsections.

# **Participants**

Continuous pressure maps collected from 82 volunteers (35 males/47 females) are included in the dataset. Participants were recruited through word-of-mouth and classroom announcements among the WMU community. All participants indicated no pre-existing musculoskeletal disorders. Descriptive statistics of selected anthropometric measurements are presented in [Table 3.](#page-45-0)

<span id="page-45-0"></span>

Variable	<b>Mean</b>	<b>SD</b>	Min	<b>Max</b>
Age (years)	23.33	6.03	18.00	58.00
Height (mm)	1689.03	77.00	1552.00	1874.00
Mass (kg)	67.05	12.50	44.00	105.69
BMI $(kg/m2)$	23.46	3.88	17.08	35.24
Hip Breadth (mm)	365.38	66.80	210.00	495.00
Buttock-Popliteal Length (Right) (mm)	486.60	32.42	410.00	600.00

Table 3. Selected anthropometric measurements for 82 participants

# **Apparatus**

Participants used a custom test chair able to accommodate 95<sup>th</sup> percentile users with no armrests, a mesh backrest, and an adjustable seat pan. The adjustable seat pan used 49 electric linear actuators placed beneath a 1" PORON<sup>®</sup> padding foam in a 7 x 7 grid configuration. Each actuator provided a vertical stroke of 6 inches, with a swiveling plate attachment of 2.5 inches in diameter set at the clevis end for contouring purposes. By using these adjustable actuators, subjects created various contours and shapes in the seat pan. The pressure maps included in the dataset were recorded under the various user-defined seat pan contours given the adjustability of the actuators. This is particularly valuable to this study as new methodologies and potential pressure measures must be valid and reliable under various sitting contours (i.e., different chairs).

Interface contact pressure was measured using a pressure mapping interface attached on top of the chair's padding foam (FSA Industrial Seat and Back Systems, Verg Inc., USA). The pressure interface mat consisted of  $1024 (32 \times 32)$  rectangular pressure elements (sensors), each 15 mm x 15 mm in size, with a maximum pressure response of 300 mmHg. The distance between each sensor was approximately 19.37 mm in the horizontal (lateral) direction and 16.56 mm in the vertical (anterior-posterior) direction. The sampling frequency was set at an approximate rate of 5 Hz.

# **Data Collection Procedure**

This dataset contains continuous pressure mapping data for each participant recorded in three different sessions. A session, lasting up to 2 hours, consisted of activities where subjects performed simulated office-related tasks (typing and mousing) using a desktop computer. At the start of each session, participants were randomly exposed to a pre-defined starting pattern and were allowed to change the height of the actuators after each interval (5 minutes). Participants made the necessary changes to the seat pan according to their levels of comfort/discomfort.

# **Spatial Clustering**

The first application of spatial data analytics is integrating unsupervised spatial clustering algorithms for the analysis and evaluation of pressure maps. Numerous unsupervised clustering algorithms have been developed over time (Amini et al., 2014; N. Kumar & Sivasathya, 2014; Xu et al., 1997). The goal of clustering techniques is to group data streams into meaningful classes or groups. Unsupervised clustering algorithms can discover and cluster data without prior knowledge (training) of the number of clusters or types of groups. Among unsupervised clustering algorithms, density-based clustering algorithms have favorable characteristics due to their ability to identify arbitrary shapes and detection of outliers (Amini et al., 2014).

Application of density-based clustering algorithms can result in potential pre-processing techniques for the detection and removal of unwanted pressure readings that are caused by extrinsic pressure artifacts such as torque forces, shear forces, pinches, and/or creases in the pressure mapping interface. These pressure artifacts are considered "outliers" for the purpose of this study. Five potential pressure mapping outlier detection techniques are evaluated in this study based on the following unsupervised density-based clustering algorithms:

- DBSCAN (Ester et al., 1996):
	- o Clustering according to density-based connectivity analysis
- OPTICS (Ankerst et al., 1999):
	- o Extension of DBSCAN with a wider range of parameter settings
- DBCLASD (Xiaowei Xu et al., 1998):
	- o Clustering based on probability distribution of neighbor's distances
- DENCLUE (Hinneburg & Keim, 1998):
	- o Clustering based on sets of density distribution functions
- HDBSCAN (Campello et al., 2015):
	- o Clustering according to variations of local densities

[Table 4](#page-47-0) shows the list of parameters used for each density-based clustering algorithms being studied. As choosing correct combinations of parameters settings is crucial for the performance of any clustering method, appropriate ranges and/or combinations of parameter settings are also studied for each clustering method. The purpose of this step is to choose a densitybased clustering algorithm where the correct identification of extrinsic pressure artifacts and true contact pressure readings is maximized; in other words, increase the outlier and non-outlier detection accuracies.

Table 4. Parameters of Spatial Clustering Methods

<span id="page-47-0"></span>

<b>Method</b>		<b>Parameters</b>	
<b>DBSCAN</b>	Epsilon	Minimum samples	
<b>OPTICS</b>	Xi	Minimum samples Minimum Size	Epsilon
<b>HDBSCAN</b>	Minimum Size	Minimum samples Leaf Size	
<b>DENCLUE</b>	Epsilon	Minimum density	
<b>DBCLASD</b>	<b>Nearest Neighbors</b>		

The following list shows a brief description of each parameter shown in [Table 4:](#page-47-0)

- Epsilon: The maximum convergence threshold parameter (e.g. distance) between two samples for one to be considered as in the neighborhood of the other.
- **•** Minimum samples: The number of samples in a neighborhood for a point to be considered as a core point.
- Xi: Determines the minimum steepness on the reachability plot that constitutes a cluster boundary.
- Minimum size: Minimum number of samples in a cluster.
- Leaf size: The number of points in a leaf node of the tree.
- Minimum density: The minimum kernel density required for a cluster attractor to be considered a cluster and not noise.
- Nearest neighbors: Number of K-neighbors to find from a given point.

Clustering methods are primarily evaluated in their ability to correctly identify outlying and non-outlying pressure readings from a selection of pressure maps included in the dataset with known outlier readings. The computational demands of these algorithms are also examined when evaluating a single pressure map (i.e., static clustering) and continuous pressure maps (i.e., dynamic clustering).

### **Data Sampling**

To evaluate the outlier-detection accuracies of these clustering methods, a subset of the dataset consisting of twenty-eight samples (28) of pressure maps with known pre-identified outliers and twenty-eight samples (28) of pressure maps without outliers is used (named cluster data subset). Selected samples of pressure maps with and without outliers are shown in [Appendix](#page-274-0)  [F](#page-274-0) and [Appendix G](#page-282-0) respectively. The selection criteria for these pressure map samples were based on the different levels of contact area (i.e., number of contact cells). Additionally, pressure map

samples were obtained from different subjects to measure accuracies of clustering methods when considering pressure maps of different sizes and shapes.

Two variations of the cluster data subset are used as input for the clustering methods: (1) a subset with only the information of the locations of pressure readings (referred to as "location input data"), and (2) a subset with information about the locations and standardized pressure data of the pressure readings (referred to as "location-pressure input data"). All clustering algorithms are instructed to only consider non-zero pressure cells during computation.

A case study is also conducted where selected clustering methodologies are evaluated in a dynamic environment by using a 5-minute sitting interval sample that includes a number of sequential spatio-temporal pressure images from one of the subjects in the dataset (named dynamic data subset).

#### **Testing Procedures**

Using the cluster data subset with location input data, different combinations of parameter settings are tested for each clustering method with the goal of achieving the best outliers/nonoutliers detection performance (parameter settings are shown in [Table 9,](#page-80-0) Chapter 5). Each clustering method is evaluated based on their accuracies score (percent [%] of correctly classified outliers and percent [%] of correctly classified non-outliers). In a similar fashion, different combinations of parameter settings are tested for each clustering method when using the locationpressure input data (see [Table 9,](#page-80-0) Chapter 5). The objective is the identify cluster methods that can select naturally occurring pressure clusters from subjects' pressure maps. Validation of the performance of these clustering methods was also made via visual feedback.

The first section in the case study includes an evaluation of the applications of selected clustering methods to pre-process continuous seating pressure maps (i.e., detection and removal of outliers) while examining overall accuracies and computational demands. This pre-processed dynamic data subset is used for subsequent case study analyses.

Algorithms for clustering methods were coded and implemented using the Python programming language. A condensed form of the Python script used for running clustering algorithms and data visualization routines can be seen in [Appendix C.](#page-251-0)

# **Outcomes**

The following outcomes were pursued for this step: (1) Recommendations of clustering methods and suggested parameters settings, given cluster performance accuracies, for identifying outliers and non-outliers pressure readings in the context of sitting pressure maps, and (2) to examine the computational demands of using recommended algorithms for detecting outliers/nonoutliers pressure readings.

# **Spatial Autocorrelation**

The second application of spatial data analytics is integrating spatial autocorrelation measures for the analysis and evaluation of pressure maps. While many statistical approaches often assume that measured outcomes are independent of each other, measures of a spatial nature often exhibit some degree of spatial autocorrelation (UCLA: Statistical Consulting Group, 2020). Spatial autocorrelation measures the relationship of variable outcomes as related to their distance; more specifically, it measures the correlation between variable values that is strictly due to their proximity in a geographical space (Kalogirou, 2019).

In seating pressure maps, measures of pressure at different locations are generally not independent. The pressure readings in a seating pressure map are generally spatially related as the pressure measures at neighboring locations are usually similar to one another. For example, measurements in proximity to a prominent bony region, such as an ischial tuberosity, are closer in their pressure values than measurements made at other distant locations in the pressure map. The degree of the similarity among proximate pressure readings can be measured using spatial autocorrelation measures.

One important aspect when calculating spatial autocorrelation is defining the relationship between locations, which is generally based on the proximities and distances between them. A weight matrix  $w_{ij}$  is generally constructed to define the distance relationship between locations. This weight matrix, often row-standardized (i.e., sum of row weights is one), can be specified in many ways, but values in the weight matrix are generally up to the researcher's decision. Gunaratna et al. (2005) presented examples of the approaches used by researchers to calculating and specifying the spatial weight matrix; these are presented as follows:

- The weight for any two different locations is constant
- A constant weight for observations within a specified distance
- K nearest neighbors have a fixed weight, all others are zero
- Weight is proportional to the inverse distance (absolute, squared, or truncated)

Based on these examples, this study used three variations of contiguity-based weight matrices to evaluate the sensitivities of spatial autocorrelation measures to extreme values and/or variances in small neighborhoods. The weight matrices used in this study are described below with a graphical representation of the weight values shown in Figure [7.](#page-52-0)

- 1. Constant weight for the eight nearest observations (Queen)
- 2. Constant weight for observations within a  $2\sqrt{2}$  cell distance (Constant Distance)
- 3. Weight is inversely proportional within a  $2\sqrt{2}$  cell distance (Inverse Distance)

0	0	0	0	0		1	1	1		1				$0.35 \mid 0.45 \mid 0.50 \mid 0.45 \mid 0.35 \mid$	
0				0		1	1			1		$0.45 \mid 0.71$	$\mathbf{1}$		0.71 0.45
0			1	0		1				1	0.50				0.50
0			1	0		1	1			1		$0.45 \mid 0.71 \mid$	$\mathbf{1}$	0.71 0.45	
0	0	0	0	0						$\mathbf{1}$				$0.35 \, 0.45 \, 0.50 \, 0.45 \, 0.35$	
	(b) Constant Distance (c) Inverse Distance Queen (a)														

<span id="page-52-0"></span>Figure 7. Contiguity-based weight matrices for spatial autocorrelation measures

This study evaluated the selected weighting approaches using two different measures of spatial autocorrelation: Moran's I (Moran, 1950) and Geary's C (Geary, 1954). Given a weight matrix  $w_{ij}$  and a two-dimensional matrix X with  $n$  elements, the mathematical definitions of the spatial autocorrelation measures used in this study are as follow:

Eq. 1 - Moran's I

$$
I = \frac{n}{S_0} \frac{\sum_i \sum_j w_{ij} (x_i - \bar{x})(x_j - \bar{x})}{\sum_i (x_i - \bar{x})^2} \text{ ; where } S_0 = \sum_i \sum_j w_{ij}
$$

Eq. 2 - Geary's C

$$
C = \frac{n-1}{2S_0} \frac{\sum_i \sum_j w_{ij} (x_i - x_j)^2}{\sum_i (x_i - \bar{x})^2} \quad ; \quad \text{where} \quad S_o = \sum_i \sum_j w_{ij}
$$

The main objective in this step is to evaluate measures of spatial autocorrelation – such as Moran's I and Geary's C – to be used as global pressure map descriptors in a static (single pressure maps) and dynamic (continuous pressure maps) environments. In the context of seating pressure mapping, measures of spatial correlation could help measure the presence of localized high/low

pressure clusters (i.e., hot spots), measure pressure readings interconnectedness, and/or surface map smoothness and continuity.

# **Data Sampling**

To evaluate the application of spatial autocorrelation measures as global pressure map descriptors, a subset of the dataset consisting of twenty samples (20) of pressure maps from different subjects was used (named static data subset). To gain a better insight about the uniqueness and usefulness of spatial autocorrelation measures, selecting pressure maps exhibiting different levels of pressure variability was desired. Out the currently used pressure measures, the coefficient of variation is a good indicator of pressure variances within a pressure map; for this reason, the selection criteria used for obtaining the pressure map samples was based on various levels of coefficient of variation. Selected samples are shown in [Appendix H.](#page-287-0)

## **Testing Procedures**

For each pressure map sample included in the static data subset, measures of Moran's I and Geary's C were calculated using all three different weight matrices. To evaluate their statistical association, correlation analyses – using the Pearson product-moment correlation – were completed for all six variations of spatial autocorrelation measures, and also between some of the known pressure measures [\(Table 1\)](#page-29-0). When strong correlations ( $R^2 \ge 0.8$ ) appeared during the correlation analysis, regression models were conducted with emphasis in finding unusual observations (i.e., points with large leverage values or extreme standardized residuals). If a pressure map was marked as an unusual observation, a comparative visual feedback was used between the pressure map and a chosen reference pressure map with a similar predictor value. The objective was to identify possible differences – as global pressure map descriptors – between the highly correlated measures. Differences in terms of each measures' ability to detect presence of localized high/low pressure clusters, surface map smoothness, and pressure level contiguity were considered.

A section of the case study also includes an evaluation of spatial autocorrelation measures under a dynamic environment (i.e., dynamic sitting). The (pre-processed) dynamic data subset (after removing outliers with spatial clustering techniques) will be used to assess the practicality of using spatial autocorrelation as dynamic pressure measures. Using time series plots, emphasis is given in evaluating sequential indexes where considerable changes in measures of spatial autocorrelation occur. Comparative visual feedback of selected sequences of pressure maps is used to confirm detected in-chair-movements.

Algorithms for calculating spatial autocorrelation measures were coded and implemented using the Python programming language. A condensed form of the Python script used for calculating commonly known pressure measures, spatial autocorrelation measures, and data visualization routines can be seen in [Appendix D.](#page-259-0) The python script also contains correlation algorithms used to generate correlograms based on the Pearson product-moment correlation. The correlograms are created applying hierarchical clustering techniques and were used to visually identify clusters of correlated and non-correlated measures.

### **Outcomes**

The following outcomes were pursued for this step: (1) Recommendations for selecting a weight matrix for calculating spatial autocorrelation measures in the context of seating pressure maps, (2) use and interpretation of spatial autocorrelation measures in the context of humanseating interaction, and (3) to examine the computational demands of using various combinations of weight matrices and spatial autocorrelation measures.

# **Image Statistical Features**

Pressure mapping systems measure and collect information about contact pressure between a subject (or object) and a pressure interface, either using a single grid-based flexible mat or individual sensor pads. Collected data from such systems are recorded in common manometric units such as pound per square inch (PSI) or millimeters of mercury (mmHg). Using re-scaling techniques, contact pressure measures can be transformed into picture elements (pixels) with intensities ranging from 0 (black) to 255 (white) (Tan et al., 2001). Unfortunately, a consequence of this re-scaling technique is information loss. For pressure maps included in the dataset, range of possible pressure values will be reduced from 0 - 300 mmHg to 0 - 255 pixel intensities. To avoid information loss, this study modified image processing algorithms to accommodate discrete value ranges from 0 - 300 pixel intensities (see [Appendix D\)](#page-259-0).

After transforming pressure readings into pixels, the location of the sensors in the pressure interface are used to project these pixels into a scaled two-dimensional space. This results in a grayscale-image representation of the pressure map in raster graphics. This transformation ensures that the resolution of the resulting images matches the resolution of the pressure interface (i.e., 32 x 32). Obtaining these low-resolution images was favorable to this study given their low computational demand requirements. Image processing techniques, such as image statistical features, are now able to be applied to resulting grayscale images of the dataset' pressure maps.

Statistical features of images were evaluated as potential global descriptors of pressure maps, with the objective of supplementing pressure measures commonly used in seating research [\(Table 1\)](#page-29-0). The first- and second-order statistics of image intensities (i.e., pressure readings) characterize the statistical properties of an image. First-order statistics are based on the probabilities that pixels will have particular intensities in an image, while second-order statistics consider the probabilities that pixel pairs – in predefined positions with respect to each other – will have particular intensities in an image (Goshtasby, 2012).

**First-Order Statistical Features.** The probability distribution of intensities in an image needs to be defined first to be able to calculate first-order statistical features. Letting  $H(i)$  denote the number of pixels with discrete intensity  $i$ , and  $S$  the total number of pixels in an image, then

<span id="page-56-0"></span>Eq. 3 - Intensities probability distribution

$$
p(i) = \frac{H(i)}{S} \quad ; \quad i = 0, ..., 300 \text{ (max cell pressure)}
$$

First-order statistical features, such as peak pressure, average pressure  $(\mu)$ , and pressure variation  $(\sigma)$ , are already being used in seating research (see [Table 1\)](#page-29-0), but other unique features used to characterize images can also be calculated from the probability distributions shown in Equation [3.](#page-56-0) The skewness (see [Eq. 4\)](#page-56-1) is a statistical feature that measures the asymmetry of pixel intensities, while the kurtosis (see [Eq. 5\)](#page-56-2) is a statistical feature that measures the degree of similarity of the pixel intensity distribution to a normal distribution.

<span id="page-56-1"></span>Eq. 4 - Skewness

$$
\gamma = \frac{1}{\sigma^3} \sum_{i=0}^{255} (i - \mu)^3 p(i)
$$

<span id="page-56-2"></span>Eq. 5 - Kurtosis

$$
\kappa = \frac{1}{\sigma^4} \sum_{i=0}^{255} (i - \mu)^4 p(i) - 3
$$

Other first-order statistical features that could be helpful in describing properties of pressure map images are the ones based on Gray-Level Differences (GLD) of adjacent pixels. Intensity variations from adjacent pixels can be obtained from calculating gray-level differences in different directions (Goshtasby, 2012). If  $H(g|\theta)$  denotes the number of adjacent pixels in direction  $\theta$  that have an absolute intensity  $g = |i_1 - i_2|$ , and  $h(g|\theta) = H(g|\theta)/\sum_g H(g|\theta)$  is the probability that adjacent pixels have absolute intensity difference  $g$  when scanned in direction  $\theta$  (0°, 45°, 90° *or* 135°), the following statistical features can be calculated:

Eq. 6 - Gradient contrast

$$
GLD_1(\theta) = \sum_g g^2 h(g|\theta)
$$

Eq. 7 - Gradient second moment

$$
GLD_2(\theta) = \sum_g [h(g|\theta)]^2
$$

Eq. 8 - Gradient entropy

$$
GLD_3(\theta) = -\sum_g h(g|\theta) \log h(g|\theta)
$$

Eq. 9 - Gradient mean

$$
GLD_4(\theta) = \sum_g h(g|\theta)g
$$

Eq. 10 - Inverse-difference moment

$$
GLD_5(\theta) = \sum_{g} \frac{h(g|\theta)}{(g^2+1)}
$$

**Second-Order Statistical Features.** To determine second-order statistical features, a Gray-Level Spatial-Dependence (GLSD) or co-occurrence matrix (GLCM)  $(h(i_1, i_2 | \theta))$  is created with entries  $(i_1, i_2)$  showing the number of adjacent pixels at direction  $\theta$  with intensity  $i_1$  and  $i_2$  in the first and second pixel respectively. Since  $h(i_1, i_2 | \theta + \pi) = h(i_2, i_1 | \theta)$ , and the co-occurrence matrix for  $\theta$  and  $\theta + \pi$  contain the same information, a co-occurrence matrix for direction  $\theta$  $(0^{\circ}, 45^{\circ}, 90^{\circ} \text{ or } 135^{\circ})$  can be calculated as the sum of  $h(i_1, i_2 | \theta)$  and its transpose  $h(i_2, i_1 | \theta)$ (Goshtasby, 2012). Letting  $M$  be the number of columns in an image and  $N$  be the number of rows in an image, the Joint Conditional Probability Density (JCPD) can be obtained as follow:

Eq. 11 - GLSD joint conditional probability density

$$
p(i_1, i_2 | \theta) = \frac{h(i_1, i_2 | \theta) + h(i_2, i_1 | \theta)}{(M - 1)N}
$$

The following features can be calculated using the JCPD of the co-occurrence matrix:

Eq. 12 - Energy

$$
GLSD1(\theta) = \sum_{i_1} \sum_{i_2} [p(i_1, i_2 | \theta)]^2
$$

Eq. 13 - Contrast

$$
GLSD_2(\theta) = \sum_{i_1} \sum_{i_2} (i_1 - i_2)^2 p(i_1, i_2 | \theta)
$$

Eq. 14 - Correlation

$$
GLSD_3(\theta) = \sum_{i_1} \sum_{i_2} \frac{(i_1 - \mu_{i_1})(i_2 - \mu_{i_2})}{\sigma_{i_1} \sigma_{i_2}} p(i_1, i_2 | \theta),
$$

where  $\mu_{i_n}$ and  $\sigma_{i_n}$ denote the mean and std. dev of  $\;\;\;\;\;\;\;\;\; h(i_1,i_2|\theta)$  $i_{3-n}$ 

Eq. 15 - Entropy

$$
GLSD_4(\theta) = -\sum_{i_1} \sum_{i_2} p(i_1, i_2 | \theta) \log p(i_1, i_2 | \theta)
$$

Eq. 16 - Homogeneity

$$
GLSD_5(\theta) = \sum_{i_1} \sum_{i_2} \frac{p(i_1, i_2 | \theta)}{1 + (i_1 - i_2)^2}
$$

In a similar manner to the spatial autocorrelation research step, the main objective in this step is to evaluate first- and second-order statistical features as global descriptors of pressure maps images, with specific properties and applications in both static (single pressure maps) and dynamic (continuous pressure maps) environments. This step focuses in determining what each statistical feature is measuring, from a seating pressure mapping perspective, that commonly used sitting pressure measures [\(Table 1\)](#page-29-0) are not able to and, more importantly, how to interpret these statistical features in the context of human-chair interactions.

The common pressure measures shown in [Table 5](#page-59-0) were calculated to find their association with the first-order and second-order statistical features presented in this section. Measures of spatial autocorrelation are additionally considered during correlation analyses to also find their relationship with measures of statistical features.

Table 5. First-order statistical features

<span id="page-59-0"></span>

Contact Cells*	Sum of Pressure*	Standard Deviation*
Coefficient of Variation*	<b>Skewness</b>	<b>Kurtosis</b>

\* Common Pressure Measures

A scanning direction  $\theta$  (e.g., 0°, 45°, 90° or 135°) needs to be defined for calculating the first-order statistical features based on Gray-Level Differences (GLD). [Table 6](#page-60-0) shows the two

directions that are considered in this study, where  $\theta = 0^{\circ}$  measures differences in the horizontal or lateral direction (X) of the pressure map image, and  $\theta = 90^\circ$  measures differences in the vertical or anterior-posterior direction  $(Y)$  of the pressure map image. These same directions were also used for calculating the second-order statistical features based on Gray-Level Spatial-Dependence (GLSD) (see [Table 7\)](#page-60-1).

<span id="page-60-0"></span>

Direction: $\theta = 0^{\circ}$	Direction: $\theta = 90^{\circ}$
<b>Gradient Contrast X</b>	<b>Gradient Contrast Y</b>
<b>Gradient Second Moment X</b>	<b>Gradient Second Moment Y</b>
Gradient Entropy X	<b>Gradient Entropy Y</b>
Gradient Mean X	<b>Gradient Mean Y</b>
Inverse-Difference Moment X	<b>Inverse-Difference Moment Y</b>

Table 6. Gray-Level Differences (GLD) statistical features

Table 7. Gray-Level Spatial-Dependence (GLSD) statistical features

<span id="page-60-1"></span>

Direction: $\theta = 0^{\circ}$	Direction: $\theta = 90^{\circ}$
Energy X	Energy Y
Contrast X	Contrast Y
Correlation X	Correlation Y
Entropy X	Entropy Y
Homogeneity X	Homogeneity Y

# **Data Sampling**

The static data subset obtained in the spatial autocorrelation step is again used for this research step. The static data subset is used to evaluate these statistical features as global pressure map descriptors. An extra subset was also created consisting of ten (10) paired samples of static pressure maps from different subjects where no significant differences ( $|\Delta|$  < 5%) are seen between common pressure measures (named paired data subset). Figure [4](#page-30-0) and [Table 2](#page-30-1) (Chapter 1) shows an example of a paired sample from two different subjects where no significant differences are seen between common pressure measures. The selection criteria for these paired-pressure maps samples were based on different levels of contact area (i.e., number of contact cells), sum of pressure, and coefficient of variation. Selected sample pairs are shown in [Appendix J.](#page-293-0)

# **Testing Procedures**

All first-order and second-order statistical features were calculated for each pressure map sample in the static data subset. While calculating these statistical features, only non-zero pressure cells were considered. As with the previous step (i.e., spatial autocorrelation), correlation analyses using the Pearson product-moment correlation were performed within all statistical feature measures and known pressure measures [\(Table 5\)](#page-59-0) to evaluate their statistical association. All six variations of spatial autocorrelation measures were also included during correlation analyses.

It was expected that some of these features and measures were highly correlated in the context of seating pressure maps; dimension reduction techniques focused on feature selections (e.g., high correlation filters) were used to select features that can explain different user-chair interaction phenomenon. Hierarchical clustering was used in the resulting correlation matrix to find clusters of measures that have strong correlations ( $R^2 \ge 0.8$ ). Regression models within these correlated clusters were conducted with emphasis in finding unusual observations (i.e., points with large leverage values or extreme standardized residuals) between clustered measures.

For pressure maps marked as unusual observations, comparative visual feedback was used between the pressure maps and selected reference pressure maps (with a similar predictor values). The objective was again to identify possible differences – as global pressure map descriptors – between these highly correlated measures. Differences in terms of each measures' ability to detect presence of localized high/low pressure clusters, acute pressure points, surface map smoothness

and texture, and pressure level contiguity were considered. In addition, research evaluated these unusual observations by expanding their respective regression models with other clustered and non-clustered measures to find possible supplemental explanatory variables.

After dimension reduction techniques, selected spatial autocorrelation measures and selected first-order and second-order statistical features were evaluated to find any significant differences (|∆| > 5%) between corresponding paired samples of pressure maps included in the paired data subset. The main focus while doing this analysis is to determine – if significant differences are found – what each statistical feature is measuring, from a pressure mapping perspective, that common seating pressure measures are not able to by means of visual feedback.

For studying the dynamic application of measures of statistical features of images, firstorder and second-order statistical features were calculated for each continuous sitting interval sample included in the (pre-processed) dynamic data subset during the case study. Using time series plots, emphasis is given in evaluating sequential indexes where considerable changes in measures of statistical features occur. Comparative visual feedback of selected sequences of pressure maps was also used to confirm detected in-chair-movements.

Algorithms for calculating first-order and second-order statistical features were also coded and implemented using the Python programming language. A condensed form of the Python script used for calculating statistical features of pressure map images is also included in [Appendix D.](#page-259-0) The same python code used to generate the correlation correlograms based on hierarchical clustering techniques also include these image statistical features.

### **Outcomes**

The following outcomes were pursued for this step: (1) Selection of unique and meaningful measures of statistical features in the context of seating pressure map, (2) validation of pressure

map statistical features as complementary measures to common pressure measures, and (3) use and interpretation of selected statistical features of pressure map images in the context of humanseating interaction.

# **Image Registration and Similarity/Dissimilarity Coefficients**

A similarity (dissimilarity) measure between two sequences of measurements  $X =$  $\{x_i, i = 1, ..., n\}$  and  $Y = \{y_i, i = 1, ..., n\}$  quantifies the dependency (independency) between the sequences. If  $X$  and  $Y$  represent pixel intensities from resulting rasterized images of pressure mapping data, measures of the similarity (dissimilarity) between pressure maps can be obtained. In seating pressure maps, similarity measures can be useful when evaluating and comparing pressure maps between subjects (comparison of pressure readings and spatial distributions) or for within-subject assessments (evaluation of dynamic sitting or clinical intervention effects). Implementing similarity and dissimilarity measures, as global comparative measure for pressure mapping analysis, could potentially eliminate current requirements of using comparative visual feedback with a set of objective measures for undemanding assessment.

Similarity/dissimilarity measures have been studied and formulated for many years. Some measures use raw intensities from images, while other apply transformations to image intensities (e.g., normalization, ranking, or joint probability functions). Goshtasby (2012) evaluated the accuracies and speeds of 16 similarity measures and 11 dissimilarity measures using both synthetic and real images. Goshtasby also evaluated the sensitivity of the measures using combinations of intensity variations and noise. Goshtasby concluded that absolute superiority of one measure against others cannot be reached; however, better performances – using percent of correct matches between images – were found when using the following similarities and dissimilarities measures:

Eq. 17 - Pearson correlation coefficient

$$
r = \frac{\sum_{i=1}^{n} (x_i - \bar{x})(y_i - \bar{y})}{\{\sum_{i=1}^{n} (x_i - \bar{x})^2\}^{\frac{1}{2}} \{\sum_{i=1}^{n} (y_i - \bar{y})^2\}^{\frac{1}{2}}}
$$

Eq. 18 - Tanimoto measure

$$
S_T = \frac{X^T Y}{\|X - Y\|^2 + X^T Y}
$$

Eq. 19 - Minimum ratio

$$
m_r = \frac{1}{n} \sum_{i=1}^{n} r_i, \quad \text{where } r_i = \min\left\{\frac{x_i + \varepsilon}{y_i + \varepsilon}, \frac{y_i + \varepsilon}{x_i + \varepsilon}\right\}, \text{and}
$$

$$
\varepsilon = \text{small number } (e, g., 1).
$$

Dissimilarity Measures

Eq. 20 -  $L_1$  norm

$$
L_1 = \sum_{i=1}^n |x_i - y_i|
$$

Eq. 21 - Square  $L_2$  norm

$$
L_2^2 = \sum_{i=1}^n (x_i - y_i)^2
$$

Eq. 22 - Intensity-ratio variance

$$
R_V = \frac{1}{n} \sum_{i=1}^{n} (r_i - \bar{r})^2
$$
; where  $r_i = \frac{x_i + \varepsilon}{y_i + \varepsilon}$ ,  $\bar{r} = \frac{1}{n} \sum_{i=1}^{n} r_i$ , and  
 $\varepsilon = small number (e.g., 1).$ 

#### **Image Registration**

One major drawback of the similarity/dissimilarity measures is that, to accurately measure the relationship between images, images should be invariant to location and orientation. If the images to be compared are not generally located in the same x-y regions of space or the orientation and angular position of the images are significantly different, using similarity/dissimilarity coefficients without applying transformation functions to the images might not be appropriate.

Sitting is a dynamic activity. Subjects constantly shift the location and orientation of their pressure contact area with the purpose of relieving discomfort. Preferences in terms of sitting postures and sitting placement in the seat pan are common issues when comparing seating pressure maps. There is a need for implementing repositioning algorithms in pressure mapping analysis.

Various parametric and non-parametric spatial transformation techniques have been developed for image registration. Modersitzki (2004) evaluated several of these transformation techniques with mixed results. Landmark-based techniques require placements of "soft markers" in images (see Fig. [8\)](#page-66-0). The registration process in landmark-based techniques is governed by the placement and correspondence of these user-defined landmarks. These markers generally require expert knowledge for manual marking and/or sophisticated image analysis tools for automatic detection (Modersitzki, 2004, p. 27); one major drawback when using landmark-based techniques.

As the evaluation of continuous dynamic pressure maps or comparison of multiple-subject pressure maps is desired, the automatic detection of image features is a desired approach for repositioning and reorienting pressure maps. Registration techniques such as Principal Axes Transformations (PAT) and optimal parametric registrations work under this principle.



Figure 8. Examples of "soft markers" required for landmark-based techniques. (Modersitzki, 2004, p. 31). Reproduced with permission of the Licensor through PLSclear.

<span id="page-66-0"></span>PAT can have different approaches according to the distribution assumption; a standard approach – more sensitive to data perturbation – generally uses a Gaussian distribution, while a more robust approach is achieved by using a Cauchy distribution (Modersitzki, 2004). PAT works by initially calculating the center of mass and the eigen decomposition of the covariance matrix. These calculated measures are used as matching features between images.

PAT registration is accomplished by translating the center of mass and then rotating and scaling the resulting orthogonal axis to match the reference image (Alpert et al., 1990). An example of the application of this technique can be seen in Figure [9.](#page-67-0) The problem of using the center of mass of the images (i.e., center of pressure) for aligning pressure images is that it often results in misalignments and/or mismatches of the pressure distribution shapes between pressure maps. Figure [10](#page-67-1) shows an example where a PAT transformation would be not appropriate, as the translation and alignment of the center of pressures would results in an incorrect image registration.

Another issue of using PAT registration is that it applies scaling transformations for matching the orthogonal axis of the images. While scaling algorithms can be implemented for comparing pressure maps, it is not appropriate for research involving human subjects (e.g., seating research). Scaling algorithms will distort subject's anthropometry and cover the dissimilarities of true differences between subjects due to their size.



<span id="page-67-0"></span>Figure 9. PAT example. Reference (left). Template (center). PAT Transformation (right). (Modersitzki, 2004, p. 53). Reproduced with permission of the Licensor through PLSclear.



<span id="page-67-1"></span>Figure 10. CP locations for pressure maps samples 120-1-900 (left) vs 120-1-1050 (right).

In a different manner, optimal registration techniques use parameterized finite-dimensional optimization routines (e.g., Steepest descent, Gauss-Newton, or Levenberg-Marquardt) to minimize differentiability between images (Modersitzki, 2004). Selection of the

minimalization/maximization objective function defines the optimization approach used for image registration. A straightforward approach is the minimization of Sums of Squared Differences (SSD) or Mean Squared Error (MSE) of pixel intensities; while another approach, Mutual Information (MI), maximizes the entropy of the images' joint density. Using the same reference and template images shown in Figure [9,](#page-67-0) results of applying MI and MSE affine transformation to the template image can be seen in Figure [11.](#page-68-0)



Figure 11. Reference (left). Affine Linear MI (center). Affine Linear MSE (right) (Modersitzki, 2004, p. 71). Reproduced with permission of the Licensor through PLSclear.

<span id="page-68-0"></span>This study evaluated the performances of optimal parametric registrations techniques based on MSE and MI registrations in the context of seating pressure mapping images. Rigid transformations with rotational and translational capabilities were considered during registration. Affine linear transformation, like the ones used in Figure [11,](#page-68-0) are not considered in this study as shear and scaling transformations are not desired for contact pressure maps with human subjects. As explained earlier, scaling and shear transformations are not appropriate for research involving human subjects (e.g., seating research) as they distort the subject's anthropometry and cover dissimilarities due to true differences in size between pressure maps.

The following are the mathematical definitions of the MSE and MI image registration techniques given a reference image  $(X)$  and a template image  $(Y)$  with pixel intensities  $I_{Xk}$  and  $I_{Yk}$  respectively, a transformation function a, image density  $\rho$ , and image entropy  $\mathbb E$  (Modersitzki, 2004; Pataky et al., 2009):

Eq. 23 - Optimal Linear Registration (MSE)

Min (MSE); MSE = 
$$
\frac{1}{n} \sum_{k} (I_{Xk} - I_{Y_{ak}})^2
$$

Eq. 24 - Optimal Linear Registration (MI)

$$
Max (MI); \quad MI = -\mathbb{E}_{\rho_{X,Y_a}} \left[ \log \frac{\rho_{X,Y_a}}{\rho_X \rho_{Y_a}} \right]
$$

By applying random transformations to randomly selected seating pressure maps, the accuracies of the translational and rotational capabilities of each image registration method can be measured by using the similarity and dissimilarity measures described in the previous section. At optimality, the similarity (dissimilarity) measures should be relatively close to 100% (0) if a good registration or image match is made by the registration method.

The main objectives in this research step are to (1) introduce image registration as an alignment technique, and (2) use similarity and dissimilarity measures as way of comparing registered pressure maps. Image registration techniques of optimal linear registration based on minimization of the Mean Squared Errors (MSE) and optimal linear registration based on maximization of the Mutual Information (MI) were evaluated in this study.

# **Data Sampling**

To evaluate the translational and rotational capabilities of the image registration techniques, a subset of the dataset consisting of ten (10) samples of pressure maps was used. The selection criteria for these pressure map samples were based on different levels of contact area (i.e., number of contact cells). Two random transformations, each with a random translational and rotational shift, were then applied to each pressure map to create the synthetic transformed data subset. Selected samples with applied random transformations are shown in [Appendix L.](#page-303-0)

Conditional sampling was also used for extracting sets of images exhibiting significant pressure map shifts. These samples are used for evaluating the feasibility of using image registration techniques and similarity/dissimilarity measures for analyzing and comparing pressure maps during dynamic sitting movements. As the distance needed for the center of pressure to travel one pressure map cell is approximately one inch  $(\sqrt{19.37^2 + 16.56^2}) = 25.5$ mm), a significant location shift was considered as a distance greater than one inch between the pressure maps' centers of pressures ( $\Delta CP > 1$  in). Twenty (20) paired-samples were selected where potentially significant sitting movements were detected (named registration data subset), with each paired sample being selected from indexes within a continuous sitting interval (same subject). Distances between the center of pressure of selected paired-samples can be seen in [Appendix N,](#page-316-0) while the pressure maps for the selected paired-samples can be seen in [Appendix O.](#page-318-0)

### **Testing Procedures**

Using the transformed data subset, the accuracies of the translational and rotational capabilities of image registration techniques are evaluated using proposed similarity/dissimilarity coefficients ( $\varepsilon = 1$  is used when required). Because the transformed pressure maps included in this subset are in fact the same pressure maps as the reference maps (with very small differences due to the random transformation being applied), the resulting values of the similarity and dissimilarity coefficients can be used to benchmark registrations optimality. Visual feedback is also used to identify differences at optimality between image registration techniques.

When calculating similarities and dissimilarities coefficients between pressure maps, two scenarios were considered: (1) Only pairwise non-zero pressure cells between pressure maps are considered (referred to as masked), and (2) unbalanced pairwise pressure cells (i.e., a non-zero pressure cell and a zero pressure cell data pair) are accepted (referred to as non-masked).

The registration data subset was used to evaluate the performances of image registration techniques under dynamic sitting. Visual feedback was used to assess the image correspondence at optimality by using pressure map overlays and visual differences in pressure map images. Because pressure maps in this subset are inherently different, similarity and dissimilarity coefficients are only used as comparative measures post-registration. Improved values in measures of similarity/dissimilarity do not necessarily indicate a better registration, but if pressure maps images indeed share a number of commonalities and features, an increase (decrease) in similarity (dissimilarity) measures is usually obtained. Difference in applications of masked and non-masked variations of measures of similarity and dissimilarity coefficients were also evaluated.

To study the dynamic application of proposed comparative techniques, the case study includes a section where continuous and sequential pressure maps are registered and compared (using similarities and dissimilarities coefficients) to the initial pressure map frame. The objective is to evaluate the feasibility of using continuous similarities and dissimilarities coefficients as comparative dynamic pressure measures after image registration techniques are applied.

Due to the temporal nature of the (pre-processed) dynamic data subset, it is expected that the overall location and orientation of sequential pressure maps to not be significantly different over time, especially if significant in-chair movements do not occur. But if otherwise, any significant pressure redistribution, postural change, and/or positional shift made by the subject could potentially be captured by the continuous similarities and dissimilarities coefficients. Time
series plots were used to assess the changes in continuous values of similarities and dissimilarities coefficients during the 5-minute dynamic sitting interval sample.

For the dynamic case study, an additional dynamic pressure measure was also examined by comparing the distance traveled by the center of pressure (CP) of the template image (i.e. the one being transformed) at registration optimality. Comparing the distance of the locations of the centers of pressure between images is often not appropriate (see Fig. [10\)](#page-67-0), but tracking the distance traveled by the center of pressure of the template image after registration could be a good indicator of in-chair movement, particularly for positional shifts in the seat pan. Assessments of CPoriginal vs CPtransformed distances were done using time series plots. The objective was to evaluate significant registration translations of the CP during the dynamic sitting interval sample.

Visual feedback was also used during the case study to validate the image correspondence when significant changes in similarities coefficients, dissimilarities coefficients, or CP<sub>transformed</sub> translations were seen in their respective time series plots. Visual feedback assessment was made using pressure maps overlays to highlight differences in pressure between pressure map images at registration optimality.

Algorithms for applying random transformations to pressure map images, implementing MI and MSE image registration, calculating similarities and dissimilarities coefficients (masked and non-masked), and data visualization routines were coded and executed using the Python programming language. A condensed form of the Python script can be seen in [Appendix E.](#page-266-0)

## **Outcomes**

The following outcomes were pursued for this last step: (1) Recommendations of registration techniques for transforming and aligning pressure maps in the context of seating pressure maps, (2) use and interpretation of similarity and dissimilarity coefficients as global comparative measures in the context of seating pressure maps, and (3) examining the computational demands of using proposed comparative techniques for transforming and comparing pressure maps in both static (paired-samples) and dynamic (continuous pressure maps) environments.

### **Summary of Methods and Procedures**

Various subsets of the main dataset were used for the research steps in this study. The cluster data subset was used to evaluate density-based spatial clustering techniques as preprocessing methods for detecting and removing extrinsic pressure artifacts (i.e., outliers) in seating pressure maps. The static data subset and paired data subset were used to evaluate the uniqueness, feasibilities, and interpretations of seating pressure measures based on spatial autocorrelation, firstorder image statistical features, and second-order image statistical features. The transformed data subset and registration data subset were used to evaluate the application of image registration techniques for aligning and matching pressure maps, and also to evaluate the use of similarity and dissimilarity coefficients as global comparative measures between registered pressure map images.

The <u>dynamic data subset</u> was used as a case study for evaluating the dynamic applications of selected methods and measures. The subset was initially pre-processed using spatial clustering to remove extrinsic pressure artifacts (i.e. outliers). Measures of spatial autocorrelation and image statistical features were then calculated, and their dynamic behavior was assessed using time series plots. At the end, image registrations were performed between each pressure map frame and the initial frame, with assessments of similarity and dissimilarity coefficients using time series plots.

A summary table of the research objectives, along with the methodologies, research procedures, and outcome goals for each research step is shown in [Table 8.](#page-74-0)



<span id="page-74-1"></span><span id="page-74-0"></span>Table 8. Summary of research steps Table 8. Summary of research steps



Table 8 $-$ Continued

The following chapters [Chapter 5 (Results) and Chapter 6 (Case Study)] show the results obtained from completing the research steps in this study [\(Table 8\)](#page-74-0). The results of the applications of spatial clustering methods, measures of spatial autocorrelation, image statistical features, and image registration and similarity and dissimilarity coefficients are presented in Chapter 5. The feasibilities, uniqueness, and practicalities of the proposed methods are discussed within the following chapter subsection: (1) Spatial Clustering, (2) Spatial Autocorrelation and Image Statistical Features, and (3) Image Registration and Similarity/Dissimilarity Coefficients. Summaries of the findings obtained from applying proposed methodologies to each data subset are also included in their respective chapter subsection, along with research notes and recommendations.

Results of using selected methodologies in a 5-minute interval of sequential pressure map images (dynamic data subset) are presented in Chapter 6 as a case study. This case study initially evaluates the feasibility and practicality of using selected density-based spatial clustering techniques for detecting and removing extrinsic pressure artifacts (outliers) under a continuous setting (dynamic pressure map samples). Using the pre-processed dynamic data subset, the results of selected measures of spatial autocorrelation and image statistical features are also shown in this chapter, with discussions of their evaluations as potential dynamic pressure measures. The preprocessed dynamic data subset is also used to evaluate the applications of image registration and similarity/dissimilarity coefficients as comparative pressure mapping techniques under a dynamic sitting environment. Results and evaluations of the feasibility and practicality of using continuous dynamic registration and the use of similarity/dissimilarity coefficients as potential dynamic pressure measures are also presented and discussed in the chapter.

### CHAPTER V

### RESULTS

Python, a high-level, general-purpose, scripting programming language, was used to obtain the results presented in this chapter . The scripts shown i[n Appendix C,](#page-251-0) [Appendix D](#page-259-0) , an[d Appendix](#page-266-0)  [E](#page-266-0) were executed with Python 3.7 under the Spyder 3.3.4 Integrated Development Environment (IDE), using a desktop computer with a quadcore Intel i7-4770K CPU clocked at 3.90 Ghz, 16 GB of DD3 RAM at 1600 Mhz, and running the Windows 10 operating system. These same algorithms were also used to obtain the results presented in the following chapter (Chapter 6).

In this study, the numerical naming convention used for the pressure maps samples are in the format "Subject-Trial-Index". The dataset used in this study contains continuous seating pressure readings collected from eighty-two different subjects. Three different trials, each up to 2 hours of collection time, are included for each subject, with a number of sequential indexes constituting a trial. As indexes are recorded sequentially, these have a direct relation to time. In this dataset, the pressure map readings were captured at approximately one-second intervals, each being recorded as an Index. As a naming convention example, the sample "109-2-1" represents the first pressure map captured (Index 1) during the second recording session (Trial 2) for Subject 109. The eighty-two subjects are labeled sequentially from Subject 109 to Subject 190 as originally named in the dataset.

The results in this chapter are presented in three sections, each following the main objectives of this study: (1) Spatial Clustering, where methods for detecting and removing extrinsic

pressure artifacts are evaluated, (2) Spatial Autocorrelation and Image Statistical Features, where new potential pressure measures are studied, and (3) Image Registration and Similarity and Dissimilarity Coefficients, where methods for aligning and comparing pressure maps are examined.

# **Spatial Clustering**

To evaluate the outlier-detection accuracies of the studied clustering methods, a subset of the dataset (cluster data subset) was created using stratified sampling of subjects' pressure maps based on the distribution of contact areas (i.e., contact cells) (see Fig. [12\)](#page-78-0). The cluster data subset consists of twenty-eight samples (28) of pressure maps with unwanted pressure artifacts and twenty-eight samples without pressure artifacts (see [Appendix F](#page-274-0) and [Appendix G\)](#page-282-0). Expert knowledge was used for selecting and marking the extrinsic pressure artifacts (i.e. outliers), if any, in each seating pressure map sampled.



<span id="page-78-0"></span>Figure 12. Histogram of subjects' average contact cells.

Two variations of the OPTICS clustering algorithm were considered: (1) OPTICS\_DBSCAN where clusters are extracted using a DBSCAN-like method with an epsilon parameter (eps), and (2) OPTICS\_XI where clusters are extracted using automatic technique, as specified by Ankerst et al. (1999), with a Xi parameter.

A sensitivity analysis for the parameters of each clustering algorithm [\(Table 4\)](#page-47-0) was carried out to find possible ranges of values (minimum to maximum) where clustering algorithms where able to detect outliers while retaining the non-outliers as true pressure readings. Ten random samples with outliers where chosen from the cluster data subset to carry out the sensitivity analysis. Eight different combinations or sets of parameter settings were chosen to be evaluated for the DBSCAN, OPTICS\_DBSCAN, OPTICS\_XI, and HDBSCAN clustering methods, using possible values of Epsilon (*eps*), Minimum samples (*min\_samples*), Xi (*xi*), Minimum size (*min\_size*), and Leaf size (*leaf size*) from the ranges of values found during the sensitivity analysis (see [Table 9\)](#page-80-0).

In a similar manner, five different combinations or sets of parameter settings were evaluated for DENCLUE and DBCLASD clustering methods, using possible values of Epsilon (*eps*), Minimum density (*min\_density*), and Nearest Neighbors (as a % of pressure map *Area*) from the ranges of values found during the sensitivity analysis (see [Table 10\)](#page-81-0).

Note that combinations or sets of parameter settings are chosen according to the input data used for the clustering method. Findings during the sensitivity analysis typically resulted in different ranges of values (minimum to maximum) for each clustering method's parameters when using either the location input data or location-pressure input data.



<span id="page-80-0"></span>Table 9. Clustering methods parameters sets 1-8, location and location-pressure input data Table 9. Clustering methods parameters sets 1-8, location and location-pressure input data

<b>Set</b>	<b>DENCLUE</b>	<b>DENCLUE</b> (NP)	<b>DBCLASD</b>	<b>DBCLASD</b> (NP)
9	$eps:1.0e-06$ min_density:5.0e-04	$eps:1.0e-01$ $min\_density:1.0e-03$	Area: 28.5%	Area: $50\%$
10	eps:1.0e-03 min_density:5.0e-04	$eps:1.0e-01$ min_density:2.0e-03	Area:33%	Area: $67%$
11	eps:2.0 $min\_density:4.0e-04$	eps:2.0 min_density:1.5e-03	Area: $40\%$	Area:80%
12	eps:2.0 min_density:3.0e-04	eps:2.0 min_density:1.8e-03	Area: $20%$	Area: $33\%$
13	eps:1.0 min_density:2.0e-04	eps:1.0 min_density:1.3e-03	Area: $12\%$	Area: $20%$

<span id="page-81-0"></span>Table 10. Clustering methods parameters sets 9-13, location and location-pressure input data

*Note: NP = No Pressure*  $\rightarrow$  *Location input data* 

The following subsections show the results for each clustering method when using these defined sets of parameters. The best combinations of input data plus parameter settings are chosen for each method in terms of outlier and non-outlier accuracies, that is, their abilities to detect extrinsic pressure artifacts (outliers) and true contact pressure readings (non-outliers). Measure of "Outliers accuracy" calculate the proportion of pre-identified outliers being detected as outliers, while measure of "Non-Outliers accuracy" calculate the proportion of true contact pressure readings being detected as non-outliers. "Overall accuracy" is the calculated weighted average of both Outliers and Non-Outliers accuracies. A set of clustering method's parameters are considered for further evaluation if both average Outliers and Non-Outliers accuracies results are above 0.90.

## **DBSCAN**

DBSCAN algorithms were implemented from the Python module Scikit-learn (v0.20.3) (Pedregosa et al., 2011). A graphical summary of the average accuracies obtained when using DBSCAN, with both location and location-pressure data input, is presented in Figure [13.](#page-82-0) The topleft panel show overall average accuracies for each set of parameters and input data. The bottomleft panel shows average non-outlier accuracies when using seating pressure map samples without outliers. Right panels show average outliers (top-right) and non-outliers (bottom-right) accuracies when using seating pressure map samples with pre-identified outliers. Results indicate that DBSCAN algorithms generally show higher average accuracies for detecting outliers when the pressure reading locations are used as input data as compared to using the location-pressure information as input data.



<span id="page-82-0"></span>Figure 13. DBSCAN – Overall, Outliers, Non-Outliers average accuracy by set

[Table 11](#page-83-0) and [Table 12](#page-84-0) show descriptive statistics of accuracies results for all sets of parameters used in DBSCAN algorithms when using both location and location-pressure input data respectively, with sets of parameter chosen for further evaluation in bold. DBSCAN parameters sets 2 and 4, using location input data, yielded the same accuracy results in each sample; similarly, sets 5 and 8 also yielded the same accuracy results for each sample (see [Table](#page-83-0)  [11\)](#page-83-0). A good combination of high outlier and non-outlier average accuracies were also obtained by

<b>Variable</b>	<b>Set</b>	<b>Mean</b>	<b>StDev</b>	<b>Minimum</b>	<b>Maximum</b>
<b>Overall Accuracy</b>	7	0.997	0.008	0.953	1.000
	3	0.996	0.010	0.953	1.000
	1	0.995	0.011	0.941	1.000
	5/8	0.994	0.009	0.964	1.000
	2/4	0.988	0.010	0.961	1.000
	6	0.011	0.014	0.000	0.059
<b>Outliers Accuracy</b>	6	1.000	0.000	1.000	1.000
	2/4	0.949	0.194	0.111	1.000
	5/8	0.925	0.179	0.333	1.000
	7	0.817	0.262	0.000	1.000
	3	0.815	0.284	0.000	1.000
	1	0.772	0.334	0.000	1.000
Non-Outliers Accuracy	1	0.999	0.003	0.985	1.000
	3	0.999	0.004	0.975	1.000
	$\overline{7}$	0.999	0.004	0.975	1.000
	5/8	0.995	0.008	0.964	1.000
	2/4	0.989	0.010	0.959	1.000
	6	0.000	0.000	0.000	0.000

<span id="page-83-0"></span>Table 11. DBSCAN – Accuracies results by set (location input data)

*Note: Sets in bold are chosen for further evaluation (accuracies > 0.90)*

[Table 12](#page-84-0) shows that, when using the location-pressure information as input data, higher average outlier accuracies were obtained by sets of parameters 6 and 7. Unfortunately, these high average outlier accuracies were obtained at the expense of lower average non-outlier accuracies when compared to results using location input data [\(Table 11\)](#page-83-0). By comparing the average outliers and non-outlier accuracy results obtained when using parameters set 5 (or 8) with location input data (0.925 and 0.995 respectively) to the average accuracy results obtained when using parameters set 6 with location-pressure data (0.920 and 0.977 respectively), we see that higher outlier and

<b>Variable</b>	<b>Set</b>	<b>Mean</b>	<b>StDev</b>	<b>Minimum</b>	<b>Maximum</b>
<b>Overall Accuracy</b>	8	0.994	0.010	0.941	1.000
	$\overline{2}$	0.991	0.013	0.941	1.000
	5	0.990	0.012	0.941	1.000
	$\mathbf{1}$	0.989	0.014	0.941	1.000
	3	0.989	0.013	0.941	1.000
	7	0.986	0.012	0.950	1.000
	$\overline{4}$	0.983	0.016	0.924	1.000
	6	0.976	0.018	0.918	1.000
<b>Outliers Accuracy</b>	6	0.920	0.227	0.000	1.000
	7	0.907	0.233	0.000	1.000
	$\overline{4}$	0.787	0.315	0.000	1.000
	5	0.782	0.318	0.000	1.000
	8	0.706	0.335	0.000	1.000
	3	0.349	0.329	0.000	1.000
	$\overline{2}$	0.230	0.276	0.000	1.000
	$\ddagger$	0.000	0.000	0.000	0.000
Non-Outliers Accuracy	$\ddagger$	1.000	0.000	1.000	4.000
	$\overline{c}$	1.000	0.001	0.994	1.000
	3	0.998	0.003	0.986	1.000
	8	0.998	0.003	0.985	1.000
	5	0.993	0.006	0.976	1.000
	7	0.988	0.009	0.970	1.000
	$\overline{4}$	0.987	0.011	0.942	1.000
	6	0.977	0.016	0.928	1.000

<span id="page-84-0"></span>Table 12. DBSCAN – Accuracy results by set (location-pressure input data)

*Note: Sets in bold are chosen for further evaluation (accuracies > 0.90)*

Out of all the combinations of parameter settings and input data, DBSCAN parameters used in sets 2/4 and 5/8 with location input data resulted in high average outlier accuracies (0.949 and 0.925 respectively) and high average non-outlier accuracies (0.989 and 0.995 respectively). Figure [14](#page-85-0) shows boxplots for DBSCAN outlier accuracies for all parameter sets when using location input data. Results from sets 2 and 5 are highlighted to show points of individual pressure

maps where Outliers accuracies were not 1 (100%). Figure [15](#page-86-0) shows examples of the outlier reference maps where Outliers accuracies below 0.80 were found in any of these sets (2/4 and 5/8). The figure also shows cross-referenced clustering results between sets 2/4 and 5/8 for these outlier reference maps. DBSCAN failed to detect a significant number of outliers in pressure map samples 172-2-1047 and 144-1-779 when using parameter sets 2/4; but it was otherwise successful in detecting outliers in all other maps at the expense of marking some non-outlier readings as outliers. In contrast, DBSCAN successfully detected the group of outliers in sample 172-2-1047 when using parameter sets 5/8, but it was more conservative in marking outliers in all other maps presented in the figure. All DBSCAN sets (location or pressure-location) failed to mark the group of outliers referenced in sample 144-1-779 (see Fig. [15,](#page-86-0)  $2<sup>nd</sup> row$ ).



<span id="page-85-0"></span>Figure 14. DBSCAN – Outliers accuracy boxplots by set (location input data)



<span id="page-86-0"></span>Figure 15. DBSCAN – Low outlier accuracy samples in sets 2/4 and 5/8 (location input data)

Figur[e 16](#page-87-0) shows boxplots for DBSCAN Non-Outlier accuracies for all parameter sets when using location input data. Results from sets 2 and 5 are highlighted to show points of individual pressure maps where Non-Outliers accuracies were not 1 (100%). Non-Outliers accuracies results when using parameters sets 5/8 where generally higher compared to results when using parameters sets 2/4. It is important to note that the Non-Outliers accuracies results obtained from these sets (2, 4, 5, or 8) were above 0.95 for all samples. Figure [17](#page-88-0) show examples where Non-Outliers accuracies between 0.95 and 0.98 were found in any of these sets (2/4 and 5/8). Here we see that DBSCAN algorithms, when using parameters settings from either of these sets, mostly marked pressure readings as outliers when a significant departure from the main contiguous pressure cluster is found (e.g., samples 175-3-1142 and 175-2-1208).



<span id="page-87-0"></span>Figure 16. DBSCAN – Non-outliers accuracy boxplots by set (location input data)

In summary, using the location information as input data, parameters of epsilon between 1.60 - 1.8 with minimum samples at 8 (sets 2/4), or epsilon parameters between 2.00 - 2.20 with minimum samples at 10 (sets 5/8) were found as adequate when using DBSCAN algorithms for detecting outlier/non-outliers seating pressure readings in a 32x32 pressure map. If preservation of all true pressure readings is of utmost importance, using DBSCAN with the epsilon parameter at 2.5 with minimum samples at 10 (set 7) resulted in an acceptable average Outliers accuracy (0.817), while maintaining a very high average Non-Outliers accuracy (0.999); only four out of the fifty-six pressure map samples did not show a perfect Non-Outliers accuracy score, all were at least 0.9751 when using location input data and DBSCAN parameters from set 7 (see Fig. [16\)](#page-87-0).



<span id="page-88-0"></span>Figure 17. DBSCAN – Sets 2/4 and 5/8 samples, non-outlier accuracy <0.98 (location input data)

## **OPTICS\_XI**

OPTICS\_XI algorithms were also implemented from the Python module Scikit-learn (v0.20.3) (Pedregosa et al., 2011). A graphical summary of OPTICS\_XI average accuracies, with both location and location-pressure data input, is presented in Figure [18.](#page-89-0) As with similar figures, the top-left panel show average overall accuracies for each set of parameters and input data. Right panels show average outliers (top-right) and non-outliers (bottom-right) accuracies for each set of parameters when using seating pressure map samples with pre-identified outliers. The bottom-left panel shows average non-outlier when using seating pressure map samples without outliers. Results indicate that OPTICS\_XI algorithms generally show higher average accuracies for detecting outliers when using both pressure readings and location information as input data. When using only pressure readings location as input data, lower average outlier accuracies (<0.9) but higher average non-outlier accuracies (>0.9) were obtained, indicating a more conservative approach when marking outliers.



<span id="page-89-0"></span>Figure 18. OPTICS\_XI – Overall, Outliers, Non-Outliers average accuracy by set

[Table 13](#page-90-0) show descriptive statistics of accuracies results for all sets of parameters used in OPTICS\_XI algorithms when using both pressure readings and location information as input data. Results from using parameters settings in set 3 resulted in high average Outliers accuracy (0.905) and high average Non-Outlier accuracy (0.915).

Variable	<b>Set</b>	<b>Mean</b>	<b>StDev</b>	<b>Minimum</b>	<b>Maximum</b>
<b>Overall Accuracy</b>	8	0.981	0.074	0.446	1.000
	$\overline{4}$	0.968	0.124	0.241	1.000
	$\overline{c}$	0.920	0.193	0.241	1.000
	3	0.916	0.197	0.241	1.000
	$\mathbf{1}$	0.873	0.239	0.241	1.000
	5	0.818	0.308	0.207	1.000
	$\tau$	0.782	0.299	0.051	1.000
	6	0.661	0.380	0.101	1.000
<b>Outliers Accuracy</b>	7	0.907	0.260	0.000	1.000
	3	0.905	0.233	0.000	1.000
	$\mathbf{1}$	0.863	0.320	0.000	1.000
	$\overline{2}$	0.844	0.319	0.000	1.000
	$\overline{4}$	0.799	0.353	0.000	1.000
	8	0.799	0.353	0.000	1.000
	6	0.650	0.462	0.000	1.000
	5	0.602	0.465	0.000	1.000
Non-Outliers Accuracy	8	0.983	0.076	0.435	1.000
	$\overline{4}$	0.969	0.126	0.227	1.000
	$\overline{c}$	0.920	0.195	0.227	1.000
	3	0.915	0.199	0.227	1.000
	$\mathbf{1}$	0.873	0.242	0.227	1.000
	5	0.819	0.313	0.207	1.000
	7	0.781	0.302	0.051	1.000
	6	0.660	0.387	0.101	1.000

<span id="page-90-0"></span>Table 13. OPTICS\_XI – Accuracy results by set (location-pressure input data)

*Note: Sets in bold are chosen for further evaluation (accuracies > 0.90)*

Figures [19](#page-91-0) and [20](#page-91-1) show boxplots for OPTICS\_XI Outliers and Non-Outliers accuracies, respectively, for all parameter sets when using the location-pressure input data. Set 3 is highlighted to show points of individual pressure maps where Outliers and Non-Outliers accuracies were not 1 (100%). Note that non-outlier accuracies were very low on many samples



<span id="page-91-0"></span>Figure 19. OPTICS\_XI – Outliers accuracy boxplots by set (location-pressure input data)



<span id="page-91-1"></span>Figure 20. OPTICS\_XI – Non-outliers accuracy boxplots by set (location-pressure input data)

Figure [21](#page-92-0) shows examples of outlier reference maps where Outlier accuracies below 0.50 were found when using parameter settings in set 3 (location-pressure input data). Similarly, Figure [22](#page-93-0) shows examples of seating pressure maps where Non-Outliers accuracies were below 0.50 for the same set (3). OPTICS\_XI is shown to be somewhat inconsistent when detecting outliers; in some instances it was conservative in marking pressure readings as outliers (see Fig. [21\)](#page-92-0), while in other cases, the majority of true contact pressure readings were being marked as outliers (see Fig. [22\)](#page-93-0). This inconsistency in the accuracies results makes the use of OPTICS\_XI an unreliable technique for detecting outlier and non-outliers seating pressure readings in a 32x32 pressure map.



<span id="page-92-0"></span>Figure 21. OPTICS\_XI – Low outlier accuracy samples in set 3 (location-pressure input data)



<span id="page-93-0"></span>Figure 22. OPTICS XI – Low non-outliers accuracy samples in set 3 (location-pressure input)

#### **OPTICS\_DBSCAN**

OPTICS\_DBSCAN algorithms were also implemented from the Python module Scikitlearn (v0.20.3) (Pedregosa et al., 2011). A graphical summary of the average accuracies obtained when using OPTICS DBSCAN, with both location and location-pressure data input, is presented in Figure [23.](#page-94-0) As with similar figures, the top-left panel show average overall accuracies for each set of parameters and input data. Right panels show average outliers (top-right) and non-outliers (bottom-right) accuracies for each set of parameters when using seating pressure map samples with pre-identified outliers. The bottom-left panel shows average non-outlier when using seating pressure map samples without outliers. Results indicate that OPTICS\_DBSCAN algorithms generally show acceptable outlier and non-outlier accuracies either when using only the location information as input data or both pressure readings and location information as input data.



<span id="page-94-0"></span>Figure 23. OPTICS\_DBSCAN – Overall, Outliers, Non-Outliers average accuracy by set

[Table 14](#page-95-0) show descriptive statistics of accuracies results for all sets of parameters used in OPTICS\_XI algorithms when using the location information as input data. OPTICS\_DBSCAN parameters from sets 2 and 4, using location input data, yielded the same accuracy results in each sample (see [Table 14\)](#page-95-0). A good combination of high outlier and non-outlier average accuracies were obtained by sets 2, 4 and 8. Other sets either marked all readings as outliers (e.g., set 6) or were more conservative in marking outliers (e.g., sets 1, 3, 5, and 7). Using location input data and OPTICS\_DBSCAN with parameters in sets 2/4 and 8, resulted in high average outlier accuracies (0.968 and 0.933 respectively) and high average non-outlier accuracies (0.964 and 0.97 respectively). Figure [24](#page-95-1) shows boxplots for OPTICS\_DBSCAN outlier accuracies for all parameter sets when using location input data. Results from sets 2 and 8 are highlighted to show points of individual pressure maps where Outliers accuracies were not 1 (100%). Some of these individual pressure maps are presented in Figure [25.](#page-96-0)

<b>Variable</b>	<b>Set</b>	<b>Mean</b>	<b>StDev</b>	<b>Minimum</b>	<b>Maximum</b>
Overall Accuracy	7	0.994	0.012	0.941	1.000
	$\mathbf{1}$	0.993	0.011	0.941	1.000
	3	0.993	0.012	0.941	1.000
	5	0.991	0.010	0.943	0.998
	8	0.970	0.012	0.941	0.992
	2/4	0.964	0.012	0.939	0.989
	6	0.011	0.014	0.000	0.059
<b>Outliers Accuracy</b>	6	1.000	0.000	1.000	1.000
	2/4	0.968	0.122	0.444	1.000
	8	0.933	0.160	0.333	1.000
	5	0.853	0.223	0.333	1.000
	$\mathbf{1}$	0.786	0.320	0.000	1.000
	$\tau$	0.734	0.349	0.000	1.000
	3	0.560	0.381	0.000	1.000
Non-Outliers Accuracy	3	0.999	0.002	0.985	1.000
	7	0.998	0.003	0.982	1.000
	$\mathbf{1}$	0.996	0.004	0.982	1.000
	5	0.993	0.008	0.965	0.998
	8	0.970	0.011	0.943	0.991
	2/4	0.964	0.012	0.937	0.989
	6	0.000	0.000	0.000	0.000

<span id="page-95-0"></span>Table 14. OPTICS\_DBSCAN – Accuracy results by set (location input data)

*Note: Sets in bold are chosen for further evaluation (accuracies > 0.90)*



<span id="page-95-1"></span>Figure 24. OPTICS\_DBSCAN – Outliers accuracy boxplots by set (location input data)



<span id="page-96-0"></span>Figure 25. OPTICS\_DBSCAN – Low outlier accuracy samples in sets 2 and 8 (location input)

Using the location information as input data, Figure [25](#page-96-0) shows examples of outlier reference maps where outlier accuracies below 0.80 were found when using OPTICS DBSCAN with set 2 or set 8 parameters. While results obtained from set 2 generally show higher accuracies in detecting outliers, set 8 correctly detected the group of outliers present in sample 172-2-1047 (Fig. [25,](#page-96-0) 1<sup>st</sup> row), whereas set 2 did not. In both sets (2 and 8), many true contact pressure readings (nonoutliers) are being marked as outliers, particularly in the first rows of pressure readings under the legs. Figure [26](#page-97-0) confirms that using OPTICS\_DBSCAN with parameters from either set (2 or 8) always resulted in a number of non-outlier pressure readings being marked as outliers, as none of the individual map results showed a 100% Non-Outliers accuracy within these sets (see [Table 14\)](#page-95-0).



<span id="page-97-0"></span>Figure 26. OPTICS\_DBSCAN – Non-outliers accuracy boxplots by set (location input data)

[Table 15](#page-98-0) show descriptive statistics of accuracies results for all sets of parameters used in OPTICS\_DBSCAN algorithms when using the location-pressure data input. In this scenario, OPTICS\_DBSCAN parameters used in set 2 resulted in high average outlier accuracy (0.925) and high average non-outlier accuracy (0.982). Figure [27](#page-99-0) and Figure [28](#page-99-1) show boxplots for OPTICS\_DBSCAN outlier and non-outlier accuracies, respectively, for all parameter sets when using location-pressure input data. Set 2 is again highlighted to show results of individual pressure maps where low outlier and non-outlier accuracies were detected.

<b>Variable</b>	<b>Set</b>	<b>Mean</b>	<b>StDev</b>	<b>Minimum</b>	<b>Maximum</b>
<b>Overall Accuracy</b>	3	0.991	0.013	0.941	1.000
	$\mathbf{2}$	0.981	0.014	0.940	0.998
	8	0.981	0.013	0.950	0.998
	$\mathbf{1}$	0.980	0.017	0.924	1.000
	6	0.968	0.021	0.903	1.000
	4	0.964	0.023	0.895	1.000
	$\tau$	0.879	0.042	0.756	0.952
	5	0.019	0.018	0.000	0.074
<b>Outliers Accuracy</b>	5	1.000	0.000	1.000	4.000
	7	0.968	0.122	0.444	1.000
	$\overline{2}$	0.925	0.178	0.333	1.000
	8	0.891	0.195	0.333	1.000
	$\overline{4}$	0.830	0.264	0.111	1.000
	$\mathbf{1}$	0.804	0.300	0.000	1.000
	6	0.774	0.312	0.000	1.000
	3	0.245	0.282	0.000	1.000
Non-Outliers Accuracy	3	1.000	0.001	0.994	1.000
	$\mathbf{1}$	0.983	0.013	0.939	1.000
	$\overline{2}$	0.982	0.012	0.942	0.998
	8	0.982	0.012	0.949	0.998
	6	0.971	0.018	0.918	1.000
	$\overline{4}$	0.966	0.021	0.895	1.000
	7	0.878	0.043	0.751	0.951
	$\overline{5}$	0.008	0.013	0.000	0.042

<span id="page-98-0"></span>Table 15. OPTICS\_DBSCAN – Accuracy results by set (location-pressure input data)

*Note: Sets in bold are chosen for further evaluation (accuracies > 0.90)*

When introducing pressure information, OPTICS\_DBSCAN results from using parameter settings in set 2 showed a higher average Non-Outlier accuracy (0.982) than results from the best location-only sets (0.964 or 0.98, from sets 2 and 8 respectively). Unfortunately, a lower average outlier accuracy (0.925) was seen when using the location-pressure input data with this set (2) when compared to the best location-only sets (0.933 or 0.968, from sets 2 and 8 respectively), indicating a more conservative approach when marking outliers. However, there were only five instances (out of twenty-eight) where outlier accuracies were below 0.80, with all other samples having outlier accuracies at 100% (see Fig. [27\)](#page-99-0).



<span id="page-99-0"></span>Figure 27. OPTICS\_DBSCAN – Outliers accuracy by set (location-pressure input data)



<span id="page-99-1"></span>Figure 28. OPTICS\_DBSCAN – Non-outliers accuracy by set (location-pressure input data)

Figure [29](#page-100-0) shows examples of outlier reference maps where outlier accuracies below 0.80 were found when using OPTICS\_DBSCAN with location-pressure input data and set 2 parameters. The results shown in this figure indicate that OPTICS\_DBSCAN (set 2) was unable to properly mark outliers when a cluster of outliers separate from the main group of true contact pressure readings is present in the pressure map. Additionally, a number of true pressure readings are also being marked as outliers in these samples. Results indicate that the use of OPTICS\_DBSCAN as outlier dectection method comes at the expense of marking true pressure readings as outliers when either using location-only or location-pressure input data (see Figs. [25,](#page-96-0) [29\)](#page-100-0).



<span id="page-100-0"></span>Figure 29. OPTICS DBSCAN – Low outlier accuracy samples in set 2 (location-pressure input)

## **HDBSCAN**

HDBSCAN algorithms were implemented from the Python module *hdbscan* (v0.8.20) (McInnes et al., 2017). A graphical summary of the average accuracies obtained when using HDDBSCAN, with both location and location-pressure data input, is presented in Figure [30.](#page-101-0) As with similar figures, the top-left panel show average overall accuracies for each set of parameters and input data. Right panels show average outliers (top-right) and non-outliers (bottom-right) accuracies for each set of parameters when using seating pressure map samples with pre-identified outliers. The bottom-left panel shows average non-outlier when using seating pressure map samples without outliers. Results indicate that HDBSCAN algorithms behave somewhat similar in terms of average outlier and non-outlier accuracies when either using the location information as input data or both pressure and location information as input data.



<span id="page-101-0"></span>Figure 30. HDBSCAN – Overall, Outliers, Non-Outliers average accuracy by set

[Table 16](#page-102-0) show descriptive statistics of accuracies results for all sets of parameters used in HDBSCAN algorithms when using the location information as input data. Only results obtained <span id="page-102-0"></span>when using set 4 show average Outlier and Non-Outlier accuracies above 0.90. When using the location-pressure input data, none of the sets showed paired accuracies above 0.90 (see [Table 17\)](#page-103-0).

<b>Variable</b>	<b>Set</b>	<b>Mean</b>	<b>StDev</b>	<b>Minimum</b>	<b>Maximum</b>
Overall Accuracy	$\mathbf{1}$	0.992	0.013	0.941	1.000
	6	0.990	0.014	0.941	1.000
	$\overline{7}$	0.985	0.014	0.941	1.000
	3	0.981	0.018	0.929	1.000
	5	0.979	0.021	0.929	1.000
	$\overline{c}$	0.920	0.034	0.845	0.997
	$\overline{\mathbf{4}}$	0.907	0.033	0.833	1.000
	8	0.905	0.034	0.816	0.996
<b>Outliers Accuracy</b>	4	0.904	0.285	0.000	1.000
	8	0.895	0.296	0.000	1.000
	5	0.843	0.323	0.000	1.000
	3	0.776	0.379	0.000	1.000
	$\mathbf{1}$	0.746	0.366	0.000	1.000
	$\overline{c}$	0.674	0.452	0.000	1.000
	$\overline{7}$	0.631	0.468	0.000	1.000
	6	0.247	0.364	0.000	1.000
Non-Outliers Accuracy	6	0.999	0.002	0.988	1.000
	$\mathbf{1}$	0.996	0.009	0.968	1.000
	$\overline{7}$	0.990	0.011	0.957	1.000
	3	0.985	0.017	0.929	1.000
	5	0.982	0.021	0.929	1.000
	$\overline{2}$	0.925	0.043	0.842	1.000
	$\overline{\mathbf{4}}$	0.909	0.038	0.831	1.000
	8	0.907	0.039	0.816	1.000

Table 16. HDBSCAN – Accuracy results by set (location input data)

*Note: Sets in bold are chosen for further evaluation (accuracies > 0.90)*

Figure [31](#page-103-1) show boxplots for HDBSCAN outlier accuracies for all parameter sets when using the location input data. Set 4 is highlighted to show points of individual pressure maps where Outliers accuracies were not 1 (100%). This figure shows only three instances (out of twentyeight) where outlier accuracies were below 0.4. These instances are shown in Figure [32,](#page-104-0) where it can be seen that HDBSCAN, when using set 4 parameters and location input data, had issues

detecting outliers when in the presence of large group of outliers. Instead, the clustering algorithm marked them as a secondary pressure cluster group. In all other cases, the clustering algorithm detected the outliers in all other pressure maps successfully (see Fig. [31\)](#page-103-1).

<b>Variable</b>	<b>Set</b>	<b>Mean</b>	<b>StDev</b>	Minimum	<b>Maximum</b>
<b>Outliers Accuracy</b>	8	0.929	0.254	0.000	1.000
	5	0.879	0.301	0.000	1.000
	$\overline{4}$	0.826	0.347	0.000	1.000
	1	0.812	0.363	0.000	1.000
	3	0.792	0.382	0.000	1.000
	$\overline{2}$	0.693	0.439	0.000	1.000
	7	0.651	0.444	0.000	1.000
	6	0.217	0.347	0.000	1.000
Non-Outliers Accuracy	6	0.988	0.020	0.896	1.000
	1	0.960	0.040	0.834	1.000
	7	0.952	0.052	0.813	1.000
	3	0.947	0.050	0.822	1.000
	5	0.933	0.059	0.789	1.000
	4	0.921	0.063	0.755	1.000
	2	0.833	0.127	0.549	1.000
	8	0.821	0.116	0.527	1.000

<span id="page-103-0"></span>Table 17. HDBSCAN – Accuracy results by set (location-pressure input data)



<span id="page-103-1"></span>Figure 31. HDBSCAN – Outliers' accuracy boxplots (location input data)



<span id="page-104-0"></span>Figure 32. HDBSCAN – Samples with low outlier accuracy in set 4 (location input data)

Figure [33](#page-105-0) show non-outlier accuracies boxplots for all HDBSCAN parameter sets when using the location input data. Set 4 (highlighted in figure) show many instances where non-outlier accuracies are low  $( $0.9$ ). Examples of these instances can be seen in Figure [34,](#page-105-1) where outlier$ reference maps and cluster results are shown. When using set 4 parameters with location input data, HDBSCAN appears to be somewhat sensitive to pressure readings outlining the main pressure cluster (marking them as outliers). The algorithm also marks a number of internal nonoutlier pressure readings as outliers. Due to these low non-outlier accuracies, HDBSCAN appears to be unreliable for detecting outlier/non-outliers pressure readings in a 32x32 pressure map.



<span id="page-105-0"></span>Figure 33. HDBSCAN – Non-outliers' accuracy boxplots (location input data)



<span id="page-105-1"></span>Figure 34. HDBSCAN – Samples with low non-outlier accuracy in set 4 (location input data)

# **DENCLUE**

DENCLUE algorithms were implemented from the Python module *denclue* (v2.0) (Mgarrett, 2017). A graphical summary of the average accuracies obtained when using DENCLUE, with both location and location-pressure data input, is presented in Figure [35.](#page-106-0) As with similar figures, the top-left panel show average overall accuracies for each set of parameters and input data. Right panels show average outliers (top-right) and non-outliers (bottom-right) accuracies for each set of parameters when using seating pressure map samples with pre-identified outliers. The bottom-left panel shows average non-outlier when using seating pressure map samples without outliers. Unbalanced Outliers and Non-Outliers average accuracies are seen in some sets using the location-pressure input data, indicating that one accuracy increases at the expense of the other. DENCLUE algorithms generally show higher average accuracies for detecting outliers when using only the location information of pressure readings as input data. [Table 18](#page-107-0) show descriptive statistics of accuracy results for all sets of parameters used in DENCLUE algorithms when using the location information as input data.



<span id="page-106-0"></span>Figure 35. DENCLUE – Overall, Outliers, Non-Outliers average accuracy by set

<span id="page-107-0"></span>

Variable	<b>Set</b>	<b>Mean</b>	<b>StDev</b>	<b>Minimum</b>	<b>Maximum</b>
<b>Overall Accuracy</b>	11	0.996	0.009	0.953	1.000
	13	0.996	0.010	0.941	1.000
	9	0.993	0.012	0.941	1.000
	12	0.972	0.088	0.494	1.000
	10	0.874	0.287	0.000	1.000
<b>Outliers Accuracy</b>	10	0.962	0.154	0.200	1.000
	12	0.952	0.155	0.200	1.000
	11	0.850	0.282	0.000	1.000
	13	0.806	0.306	0.000	1.000
	9	0.443	0.383	0.000	1.000
Non-Outliers Accuracy	9	1.000	0.000	1.000	1.000
	13	0.999	0.004	0.975	1.000
	11	0.998	0.005	0.975	1.000
	12	0.973	0.090	0.476	1.000
	10	0.874	0.291	0.000	1.000

Table 18. DENCLUE – Accuracy results by set (location input data)

*Note: Sets in bold are chosen for further evaluation (accuracies > 0.90)*

Results in [Table 18](#page-107-0) show that, when using DENCLUE algorithms with the location information as input data, parameters settings from set 12 resulted in high average outlier accuracies (0.952) and high average non-outlier accuracies (0.973). Figure [36](#page-108-0) shows boxplots for DENCLUE outlier accuracies for all parameter sets when using location input data. Set 12 is highlighted to show points of individual pressure maps where Outliers accuracies were not 1  $(100\%)$ .

Figure [37](#page-108-1) shows examples of outlier reference maps where Outlier accuracies were 0.20 (Fig. [37,](#page-108-1) top) and 0.83 (Fig. [37,](#page-108-1) bottom) when using location input data with DENCLUE and set 12 parameters. While DENCLUE algorithms generally create multiple clusters from the pressure readings within a pressure map, it is still favorable for detecting outliers (marked as noise); only one sample (out of twenty-eight) had an outlier accuracy less than 0.80 due to the presence of a large group of outliers (see Fig. [37,](#page-108-1) top).


Figure 36. DENCLUE – Outliers accuracy boxplots by set (location input data)



<span id="page-108-0"></span>Figure 37. DENCLUE – Samples with low outlier accuracy in set 12 (location input data)

High non-outlier accuracies (average of 0.973) were also obtained when using the parameters settings from set 12 with the location information as data input. Figure [38](#page-109-0) shows boxplots for DENCLUE non-outlier accuracies for all parameter sets when using the location input data. Set 12 is highlighted to show points of individual pressure maps where Non-Outliers accuracies were not 1 (100%). Out of the twenty-eight samples with pre-identified outliers, only three showed Non-Outliers accuracies less than 0.90 when using this DENCLUE set (2) and the location data input. Figure [39](#page-110-0) shows outlier reference maps of all instances where non-outlier accuracies were less than 0.90 when using DENCLUE with set 12 parameters and location data input. This figure shows how using the DENCLUE algorithm with set 12 parameters and location data input create instances where true contact pressure readings outlining the main pressure cluster are being identified as outliers (noise). While this outlier detection behavior is only seen in three samples, the number of true contact pressure readings being marked as outliers is significant in these samples.



<span id="page-109-0"></span>Figure 38. DENCLUE – Non-outliers accuracy boxplots by set (location input data)



<span id="page-110-0"></span>Figure 39. DENCLUE – Samples with low non-outlier accuracy in set 12 (location input data)

To maximize the non-outlier accuracies found in set 12 [\(Table 18\)](#page-107-0), additional runs were performed using the DENCLUE clustering algorithm with the location information as input data. The DENCLUE parameter for minimum density (*min\_density*) was found to be influential in marking pressure readings as outliers, and it was fine-tuned to reduce instances such as the ones depicted in Figure [39.](#page-110-0) The additional sets of DENCLUE parameters evaluated in this study are shown in [Table 19,](#page-111-0) these are again used with the location input data.

Non-outlier accuracies increased by reducing the minimum density value (from the value of 1.8e-03 used in set 12). Unfortunately, this increasing in non-outlier accuracies were at the expense of lower outlier accuracies. However, acceptable tradeoffs were found where increased non-outlier accuracies were obtained while still maintaining a high average outlier accuracy (>0.90). [Table 20](#page-111-1) shows accuracies results for the additional DENCLUE sets. Results from sets 14 and 15 show an increase in average non-outliers accuracies when compared to the results obtained from set 12; also, the minimum non-outliers accuracies are also significantly higher.

<b>DENCLUE</b> (NP)
eps:2 $min\_density:1.7e-03$
eps: 0.01 $min\_density:1.65e-03$

<span id="page-111-0"></span>Table 19. DENCLUE additional parameter sets for location input data

*Note:*  $NP = No$  *Pressure*  $\rightarrow$  *Location input data* 

<span id="page-111-1"></span>Table 20. DENCLUE – Accuracy results for additional sets (location input data)

<b>Variable</b>	<b>Set</b>	Mean	<b>StDev</b>	<b>Minimum</b>	<b>Maximum</b>
<b>Overall Accuracy</b>	15	0.995	0.010	0.953	1.000
	14	0.992	0.020	0.868	1.000
	12	0.972	0.088	0.494	1.000
<b>Outliers Accuracy</b>	12	0.952	0.155	0.200	1.000
	14	0.926	0.175	0.200	1.000
	15	0.907	0.187	0.200	1.000
Non-Outliers Accuracy	15	0.997	0.008	0.952	1.000
	14	0.993	0.020	0.864	1.000
	12	0.973	0.090	0.476	1.000

Figure [40](#page-112-0) shows outlier accuracy boxplots for these additional DENCLUE sets (14 and 15). Even if lower outlier accuracies are seen when compared to set 12, high outlier accuracies

(i.e., greater than 0.90) are still obtained in most of the samples, notably for results obtained from set 14. Figure [41](#page-112-1) shows non-outlier accuracy boxplots for these additional sets. A signicant increase in non-outlier accuracies were obtained when using parameters from sets 14 and 15, when compared to results from set 12.



<span id="page-112-0"></span>Figure 40. DENCLUE – Additional outliers accuracy boxplots (location input data)



<span id="page-112-1"></span>Figure 41. DENCLUE – Additional non-outliers accuracy boxplots (location input data)

Figure [42](#page-114-0) shows a comparative visual analysis between the results from sets 12, 14 and 15 in instances where low outlier accuracies (Fig. [37\)](#page-108-0) or low non-outlier accuracies (Fig. [39\)](#page-110-0) were found in set 12. Examples of low outlier accuracies among these sets (12, 14, and 15) are shown in Figure [42](#page-114-0) (first and second row in the figure). Generally, using parameter settings from set 12 result in detecting and marking outlier with higher accuracy by correcly detecting more scattered outliers than results when using parameter settings from sets 14 or set 15 (e.g.,  $2<sup>nd</sup>$  row in [Figure](#page-114-0) [42\)](#page-114-0). But in other instances, results obtained from all sets were similar in their inability to detect a distinct cluster group of outliers as extrinsic pressure artifacts (e.g., 1<sup>st</sup> row in [Figure](#page-114-0) 42).

The benefits of running the additional sets (14 and 15) are seen in their improvement of non-outlier accuriaces when compared to set 12 results. Instances where low non-outlier accuracies were seen when using parameter settings in set 12 are now greatly improved when using parameter settings from either set 14 or set 15 (e.g., see rows 3-5 in [Figure](#page-114-0) 42). While the DENCLUE algorithm is more relaxed when using parameter settings from set 14 or 15 (in terms of detecting and marking outliers), it still offers high outlier accuracies  $(0.90)$  in most of the pressure map samples (see Fig. [40\)](#page-112-0) with greatly improved non-outlier accuracies (see Fig. [41\)](#page-112-1).

In summary, using the location information as input data, parameters of minimum density between 1.65e-03 to 1.7e-03, and epsilon parameters between 0.01 to 2, as used in sets 14 and 15, were shown to be adequate when using DENCLUE algorithms for detecting outlier/non-outliers sitting pressure readings in a 32x32 pressure map.



<span id="page-114-0"></span>Figure 42. DENCLUE – Samples with low accuracies in sets 12, 14 and 15 (location input data)

## **DBCLASD**

DBCLASD algorithms were implemented from the Python module *py-dbclasd* (Palacio, 2015). A graphical summary of the average accuracies obtained when using DBCLASD, with both location and location-pressure data input, is presented in Figure [43.](#page-115-0) As with similar figures, the top-left panel show average overall accuracies for each set of parameters and input data. Right panels show average outliers (top-right) and non-outliers (bottom-right) accuracies for each set of parameters when using seating pressure map samples with pre-identified outliers. The bottom-left panel shows average non-outlier when using seating pressure map samples without outliers.

Results indicate that DBCLASD algorithms generally show higher average outlier and non-outlier accuracies when using the pressure readings' location as input data, as compared to using location-pressure as input data.



<span id="page-115-0"></span>Figure 43. DBCLASD – Overall, Outliers, Non-Outliers average accuracy by set

[Table 21](#page-116-0) show descriptive statistics of accuracy results for all sets of parameters used in DBCLASD algorithms when using location information as input data. Unfortunately, none of these sets show both average outlier and non-outlier accuracies above 0.90. The highest Outliers accuracy is seen when using the parameter settings in set 13 with a 0.819 accuracy in detecting pre-defined outlier pressure readings (i.e., extrinsic pressure artifacts).

Variable	<b>Set</b>	<b>Mean</b>	<b>StDev</b>	<b>Minimum</b>	<b>Maximum</b>
<b>Overall Accuracy</b>	12	0.987	0.036	0.826	1.000
	13	0.987	0.030	0.838	1.000
	9	0.985	0.051	0.650	1.000
	11	0.979	0.039	0.851	1.000
	10	0.974	0.065	0.755	1.000
<b>Outliers Accuracy</b>	13	0.819	0.236	0.167	1.000
	12	0.764	0.294	0.000	1.000
	9	0.725	0.342	0.000	1.000
	10	0.716	0.353	0.000	1.000
	11	0.685	0.366	0.000	1.000
Non-Outliers Accuracy	12	0.989	0.036	0.826	1.000
	13	0.989	0.030	0.842	1.000
	9	0.988	0.051	0.650	1.000
	11	0.982	0.039	0.851	1.000
	10	0.976	0.066	0.755	1.000

<span id="page-116-0"></span>Table 21. DBCLASD – Accuracy results by set (location input data)

Figure [44](#page-117-0) shows boxplots for DBCLASD outlier accuracies for all parameter sets when using the location input data. Set 13 is highlighted to show points of individual pressure maps where Outliers accuracies were not 1 (100%). While results of using parameter setting described in set 13 show many samples with high outlier accuracy (median  $= 0.944$ ), there are many instances where the detection of outliers was poor. Figure [45](#page-117-1) show examples where low outlier accuracies were obtained. In some instances, the DBCLASD algorithm appears to have issues in detecting scattered outliers points within seating pressure maps (see Fig. [45,](#page-117-1) top).



<span id="page-117-0"></span>Figure 44. DBCLASD – Outliers accuracy boxplots by set (location input data)



<span id="page-117-1"></span>Figure 45. DBCLASD – Samples with low outlier accuracy in set 13 (location input data)

Some of the results obtained while using DBCLASD algorithms with location input data and parameter settings in set 13 were unusual. Figure [46](#page-118-0) show some examples were low nonoutlier accuracies were obtained. This figure shows a number of true contact pressure readings (i.e., non-outliers) being incorrectly marked as outliers in an unusual manner. Due to algorithms' inability to detect outliers and non-outliers with high accuracies, DBCLASD appears to be an inadequate technique for detecting unwanted pressure readings in a 32x32 pressure map.



<span id="page-118-0"></span>Figure 46. DBCLASD – Samples with low non-outlier accuracy in set 13 (location input data)

#### **Spatial Clustering Summary**

Many spatial clustering methods were shown to be adequate for detecting outlier/nonoutliers seating pressure readings in a 32x32 pressure map. DBSCAN and DENCLUE algorithms, in particular, showed superior average outlier and non-outlier accuracies among the various clustering methods evaluated. Given the results obtained from these clustering algorithms, recommended parameters for DBSCAN and DENCLUE algorithms are shown in [Table 22.](#page-119-0)

An absolute superiority of a particular combination of clustering method/parameter settings against others cannot be reached. Irrespective of the clustering method used, a tradeoff between outlier and non-outlier accuracies is usually seen when trying to increase one or the other. While a particular method/parameter combination cannot be chosen as the best, results indicate that better outlier/non-outlier accuracies are typically obtained when only using location information of the pressure readings as input data in most of the evaluated clustering algorithms.

<span id="page-119-0"></span>

Method	Parameters	Input	<b>Average Accuracy</b>	Avg.		
			Outliers	Non-Outliers	Overall	Proc Time
<b>DBSCAN</b>	eps: 1.60, 1.80 min_samples: 8	Location	0.949	0.989	0.988	5.8 <sub>ms</sub>
<b>DENCLUE</b>	eps: 2 $min$ density: 1.7e-03	Location	0.926	0.993	0.992	11.1s
<b>DBSCAN</b>	eps: 2.00, 2.20 min_samples: 10	Location	0.925	0.995	0.994	5.8 <sub>ms</sub>
<b>DENCLUE</b>	eps: 0.01 $min\_density: 1.65e-03$	Location	0.907	0.997	0.995	11.5s
<b>DBSCAN</b>	eps: $2.5$ min_samples: 10	Location	0.817	0.999	0.997	5.7 <sub>ms</sub>

Table 22. Summary of analysis results for recommended clustering methods

Among the recommended methods [\(Table 22\)](#page-119-0), the highest average outlier accuracy was achieved by DBSCAN when using parameters of epsilon between 1.6-1.8 and setting minimum samples at 8. This combination produced a 94.9% average outlier accuracy rating while maintaining an average non-outlier accuracy close to 99% (0.989). The highest average non-outlier accuracy, while maintaining an average outlier accuracy greater than 90%, is achieved by DENCLUE when using a minimum density of 1.65e-03, with a 99.7% average non-outlier

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accuracy rating. A good balance between average outlier and non-outlier accuracies were achieved by DENCLUE when using a minimum density of 1.7e-03, with 92.6% and 99.3% respectively.

If preservation of all true contact pressure readings is of utmost importance, a DBSCAN algorithm with parameters epsilon parameter minimum samples set at 2.5 and 10, respectively, showed very high non-outlier accuracies when using the location input data (see [Table 22\)](#page-119-0). This particular combination produced 52 out of 56 samples with 100% non-outlier accuracy scores, and the remaining samples with non-outlier accuracy scores greater than 97.51%. Considering its high non-outlier accuracies, an acceptable average outlier accuracy score of 81.7% was also achieved by these DBSCAN settings. Another alternative for preserving most of the true contact pressure readings is to use a DENCLUE algorithm with minimum density set at 1.65e-0.3 and use the location information as input data. This DENCLUE combination showed very high average nonoutlier accuracies (0.997), and an improved average outlier accuracy (0.907) when compared to the previously discussed DBSCAN combination (epsilon at 2.5 and minimum samples at 10).

The processing times for each clustering method were also recorded. [Table 22](#page-119-0) show DBSCAN algorithms with average processing times of around 5.8ms when detecting outliers/nonoutliers in 32x32 pressure maps, while DENCLUE showed average processing times of around 11s. DBSCAN algorithms implemented in this research come from the module scikit-learn (Pedregosa et al., 2011), a well-known fully-optimized machine learning python package. On the other hand, the DENCLUE module available for python and used in this research is non-optimized. This DENCLUE module has also been used in other research studies (L. Liao et al., 2017). The need for a fully optimized DENCLUE python package (introducing multiprocessing optimization during hill climb algorithms) will be beneficial for future pressure mapping analyses using the python programming language.

### **Spatial Autocorrelation and Image Statistical Features**

The following subsections show results of the analysis of spatial autocorrelation measures and image statistical features for the following datasets: (1) static data subset, and (2) paired data subset. Results of correlation and regression analysis are discussed with the aim of finding meaningful differences between highly correlated variables, and eliminating correlated variables via dimension reduction techniques (e.g., high correlation filters). Computation demands for calculating various measures are also discussed.

## **Static Data Subset**

An average coefficient of variation was calculated for each subject using seating pressure maps collected during their sitting session trials. Stratified sampling of subjects' pressure maps was used following the distribution of the average coefficient of variation by subject (see Fig. [47\)](#page-121-0). Twenty (20) samples of seating pressure maps were selected to create the static data subset (see [Appendix H\)](#page-287-0).



<span id="page-121-0"></span>Figure 47. Histogram of subjects' average coefficient of variation

**Spatial Autocorrelation.** Measures of Moran's I and Geary's C were calculated using modules from the Python Spatial Analysis Library (PySAL v1.14.4) (Rey & Anselin, 2007). The results showed that the measures are inversely identical to each other within the context of seating pressure mapping (using the static data subset). Regardless of the weight matrix used, both measures showed a very strong correlation between each other with correlation values of  $r = -1$ ,  $r = -0.998$ , and  $r = -0.999$  for the queen, constant-distance, and inverse-distance weight matrices respectively. By having very similar behavior to Gearys' C and easier interpretability (with a defined autocorrelation range from -1 to 1), Moran's I spatial correlation measure appears to be a better candidate as a new pressure measure.

On the other hand, computational demands using the PySAL python package were very different between these measures, even if formulas have a similar degree of complexity (see [Eq. 1](#page-52-0) and [Eq. 2\)](#page-52-1). Figure [48](#page-122-0) shows the average processing times when calculating the spatial autocorrelation measures in the static data subset samples.



<span id="page-122-0"></span>Figure 48. Spatial autocorrelation measures average processing time (static data subset)

Average processing time for calculating Moran's I was under 25ms in all weight matrices; Geary's C, on the other hand, showed an average processing time of around 150ms when using the queen matrix  $(3x3)$ , and around 400ms when using other larger weight matrices  $(5x5)$  (see Fig. [48\)](#page-122-0). The effect of choosing different weight matrices not only affected the computing time, but also the magnitude of the spatial autocorrelation measure. Figure [49](#page-123-0) shows Moran's I spatial autocorrelation measures using different weight matrices for all samples in the static data subset. Moran's I results show moderate to very strong positive spatial autocorrelation within all pressure map samples, with consistently higher measures when using the queen weight matrix (Q). Using weight matrices with a larger area (5x5 instead of 3x3) affected the Moran's I values. When using the Inverse-Distance weight matrix (ID) and Constant-Distance weight matrix (CD), both using a 5x5 matrix, Moran's I values are reduced by approximately 10.6% and 15.1% respectively, compared to results obtained when using the Queen weight matrix  $(Q)(3x3)$  (see Fig. [49\)](#page-123-0).



<span id="page-123-0"></span>Figure 49. Moran's I spatial autocorrelation by weight matrix (static data subset)

<span id="page-124-0"></span>



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A correlation analysis using Pearson product-moment was used to assess the relationship between all known and proposed pressure map measures using the samples in the static data subset. Figure [50](#page-124-0) shows the results of the correlation matrix presented as a hierarchical clustered correlogram.

Focusing on the correlated clusters where spatial autocorrelation measures are included (Fig. [50,](#page-124-0) top left), other meaningful correlations besides the ones between themselves (Moran's I and Geary's C) are also seen. The correlation measures obtained from Gray-Level Spatial-Dependence (GLSD) statistical features in the Y direction (GLSD – Correlation Y) and Moran's I (Q) (queen matrix) show a strong positive correlation ( $R^2 = 0.891$ ). Figures [51](#page-125-0) and [52](#page-126-0) show the regression model, fitted line plot, and standardized residual plots between these measures. An unusual observation ( $std. residual > |2|$ ) detected while fitting the regression model can also be seen in these figures. Figure [53](#page-126-1) shows the pressure map of this unusual observation (Fig. [53a](#page-126-1)), along with calculated Moran's I and GLSD Correlation Y measures.



<span id="page-125-0"></span>Figure 51. Moran's I vs GLSD Correlation Y regression (static data subset)



Figure 52. Moran's I vs GLSD Correlation Y residuals (static data subset)

<span id="page-126-0"></span>



(c) 117-1-1193 Second Gradient Map (d) 161-1-1833 Second Gradient Map



\*Unusual Observation

<span id="page-126-1"></span>Figure 53. Moran's I vs GLSD Correlation Y unusual observation (static data subset)

For comparative purposes, Figure [53](#page-126-1) also shows a secondary pressure map (Fig. [53b](#page-126-1)) with a similar Moran's I measure, but with a GLSD Correlation Y result close to the expected value  $(stat. residual = -0.01)$ . Second gradient maps along the Y-axis (90°) are also presented in this figure for each one of the pressure maps; these are calculated by using second order accurate central differences in the interior points of the images, and first order accurate one-sides (forward or backwards) differences at the image boundaries at a given direction. By comparing the second gradient maps between these samples, more scaterring of positive/negative gradients are seen in [Figure](#page-126-1) 53c, while [Figure](#page-126-1) 53d has more defined gradient clusters. GLSD Correlation measures appear to be sensitive to these pressure gradient variations at a given direction (e.g.,  $90^{\circ}$ ), while measures of Moran's I appear to give more emphasis in measuring presence of correlated pressure cluster with more robustness to these pressure gradient variations.

It is also important to highlight that measures of correlation using GLSD do not require any weight matrix. The magnitude of Moran's I spatial autocorrelation measure was significantly affected by defining weight matrices with different areas of interest (i.e., moving window) (see Fig. [49\)](#page-123-0). For the seating pressure maps evaluated in this study, the use of a queen weight matrix appears to be a more conservative approach when calculating Moran's I spatial autocorrelation measures. As the max-min size of autocorrelated high pressure clusters (e.g., ischial tuberosities) are usually within a 3 x 3 region of pressure cells (see [Appendix H\)](#page-287-0), higher Moran's I spatial autocorrelations values are obtained due to matching the size of these high-pressure clusters to the size of the queen weight matrix. Therefore, there appears to be a relationship between the expected max-min size of pressure correlated regions and selecting the size of the regions of interest in a weight matrix. A weight matrix with a region of interest greater than the max-min size of autocorrelated high-pressure clusters could potentially weaken the spatial autocorrelation values.

While Moran's I and GLSD Correlation measures showed similar behaviors  $(R^2 =$ 0.891), they were found to be unique pressure map descriptors, and are adequate measures of spatial autocorrelation of pressure maps. In the context of seating pressure maps, high spatial autocorrelation values indicate presence of distinct pressure clusters of various levels formed by contiguous pressure readings, while low values indicate scattered low/high pressure readings or distinct low-area high-pressure points (e.g., acute pressure points). [Appendix I](#page-291-0) include results of measures of spatial autocorrelation (Moran's I and GLSD Correlation) for all samples in the static data subset [\(Appendix H\)](#page-287-0).

Researchers have the option to measure spatial autocorrelation within pressure maps using Moran's I, which allows them to choose the size/weight of the area of interest (i.e., moving window) and is more robust to gradient variations, or use GLSD Correlation, which does not require a described weight matrix and is more sensitive to localized pressure gradient variations.

**Image Statistical Features.** Results from the correlation matrix and clustered correlogram also show instances where many image statistical features and known pressure measures are grouped into highly positive or negative correlated clusters (see Fig. [50\)](#page-124-0). Measures of Gradient Contrast (GLD) and Contrast (GLSD) behave almost identically ( $R^2 \approx 100\%$ ) regardless of the measure's direction  $[0^{\circ}(X)$  or  $90^{\circ}(Y)$ ]. Other measures, such as Gradient Contrast (GLD) and Gradient Mean (GLD), also behave similarly at either direction with  $R^2 \approx 84.5\%$  at 90°, and  $R^2 \approx$ 90.3% at 0°. Despite this, there were some instances where unusual observations were observed during regression analyses in both directions  $[0^{\circ}(X)$  and  $90^{\circ}(Y)$ , these are shown in Figures [54](#page-129-0) to [57.](#page-130-0)



<span id="page-129-0"></span>Figure 54. GLD Gradient Contrast Y vs GLD Gradient Meant Y regression (static data subset)



Figure 55. GLD Gradient Contrast Y vs GLD Gradient Meant Y residuals (static data subset)



Figure 56. GLD Gradient Contrast X vs GLD Gradient Meant X regression (static data subset)



<span id="page-130-0"></span>Figure 57. GLD Gradient Contrast X vs GLD Gradient Meant X residuals (static data subset)

Figure [58](#page-131-0) shows pressure maps of the samples where measures of GLD Gradient Contrast [in  $0^{\circ}(X)$  or  $90^{\circ}(Y)$ ] were unusual and higher than predicted. The figure shows that Gradient Contrast values are significantly higher, considering values of Gradient Mean, when pressure maps have either a single or small group(s) of acute high-pressure cells. These instances are captured better by measures of GLD Gradient Contrast due their sensitivities for high gradients (see [Eq. 6](#page-57-0) and [Eq. 9\)](#page-57-1). These two measures (GLS Gradient Contrast and GLD Gradient Mean) are considered adequate as global measures of pressure gradients within a pressure map due to their uniqueness as pressure map descriptors.









\*Unusual Observation

<span id="page-131-0"></span>Figure 58. GLD Gradient Contrast vs Gradient Mean unusual observations (static data subset)

Results from the correlation matrix and clustered correlogram presented in Figure [50](#page-124-0) also show other sets of statistical features that are grouped in strongly positive or negative correlated clusters. Measures of Homogeneity (GLSD), Inverse-Difference Moment (GLD), and Gradient Second Moment (GLD) are shown as positively correlated, and are measures commonly used to

quantify an image texture. An image texture measures the variations of the surface intensity and quantifies properties of smoothness, coarseness and regularity (Kurani et al., 2004, p. 1). Measures of Homogeneity (GLSD) and Inverse-Difference Moment (GLD) behave similarly when measured at 90° ( $R^2 \approx 94.5\%$ ) or 0° ( $R^2 \approx 94.2\%$ ) with no unusual observations in the regression models.

A strong negative correlation was found between Gradient Second Moment (GLD) and Gradient Entropy (GLD) in both 90° ( $R^2 \approx 96.5\%$ ) and 0° ( $R^2 \approx 92.2\%$ ) directions. GLD measures of Gradient Mean and Gradient Entropy also behave similarly when measured either at 90<sup>o</sup> ( $R^2 \approx 95\%$ ) or 0<sup>o</sup> ( $R^2 \approx 90\%$ ). The Gradient Second Moment (GLD) measure looks for lack of noise (or disorder) in pixel intensities, whereas Gradient Entropy (GLD) increases with noise/disorder; both of these measures are being affected, in opposite directions, by an overall increase in pressure gradients (i.e., an increase in pressure gradients [Gradient Mean (GLD)] is usually associated with an increase in image noise [Gradient Entropy (GLD)] and, thus, a decrease in surface smoothness [Gradient Second Moment (GLD)] within a pressure map image).

Statistical features of Gradient Second Moment (GLD) and Homogeneity (GLSD) do not show a very strong correlation between themselves ( $R^2 \approx 61\%$  at 90°, and  $R^2 \approx 50\%$  at 0°), even when both are measures of a pressure map texture and/or smoothness. Figure [59](#page-133-0) shows line plots for values of both of these measure at 90° (Y) for all samples in the static data subset. Two samples are highlighted to indicate where significant differences or unusual observations were seen during regression analyses (std. residuals  $>$  [2.29]). Figure [60](#page-134-0) shows pressure maps, gradient maps, and values of Gradient Second Moment (GLD) and Homogeneity (GLSD) for these unusual observations. First-order gradient maps are calculated as absolute differences in pressure in a given direction.

First-order gradient map from sample 122-2-2954 (Fig. [60c](#page-134-0)) shows low variations in the magnitudes of absolute gradients (low texture), reflected as a high Gradient Second Moment (GLD) value due to this. On the other hand, a higher texture is seen in gradient map from sample 145-1-1601 (Fig. [60d](#page-134-0)), resulting in a lower Gradient Second Moment (GLD) value. In contrast, the measure of Homogeneity (GLSD) in sample 122-2-2954 is higher than expected due to the presence of pressure clusters with identical high-pressure readings (300 mmHg), a consequence of the pressure interface mat limits (max. pressure response). Results indicate that Homogeneity (GLSD) measures are sensitive when a number of contiguous equal-value pressure readings are present in the pressure maps (i.e., homogeneity within various pressure cluster levels), while measures of Gradient Second Moment (GLD) are more sensitive to gradient transitions.

Both Gradient Second Moment (GLD) and Homogeneity (GLSD) measures are adequate, and complementary, measures of pressure map texture and homogeneity. Higher values on these measures will generally indicate a pressure map with smoother transitions between pressure levels, with less coarseness within the pressure map, and more homogeneous pressure cluster levels.



<span id="page-133-0"></span>Figure 59. GLD Gradient Second Moment Y vs GLSD Homogeneity Y (static data subset)





\*Unusual Observation

<span id="page-134-0"></span>Figure 60. GLD Gradient Second Moment vs GLSD Homogeneity unusual observations

(static data subset)

Other sets of statistical features that also show strong correlations are Energy (GLSD), Entropy (GLSD), and Contact Cells (see Fig. [50\)](#page-124-0). An initial assessment found that the direction of measurement does not significantly affect the behavior of Entropy (GLSD)  $\left[R^2 \approx 96.1\% \text{ between }\right]$  $90^{\circ}(Y)$  and  $0^{\circ}(X)$ ]. Similarly, measures of Energy (GLSD) are also generally not affected by the

direction of measurement ( $R^2 \approx 92\%$  between  $90^{\circ}(Y)$  and  $0^{\circ}(X)$ ). Measures of Energy (GLSD) and Entropy (GLSD) are almost inversely identical to each other with  $R^2 > 97.7\%$  in either  $90^{\circ}(Y)$  or  $0^{\circ}(X)$ . Regression results for measures of Energy (GLSD) and Entropy (GLSD) were obtained by excluding sample 145-1-1601 (see Fig. [60b](#page-134-0)). Figur[e 61](#page-135-0) showsthe relationship between these image statistical features while highlighting measures' discrepancies found in sample 145- 1-1601. Note that the measure scale for Energy (GLSD) is in inverse proportion. Energy (GLSD) and Entropy (GLSD) are significantly affected when a pressure map shows pressure clusters at max pressure response readings (300 mmHg) (see Fig. [60b](#page-134-0)). A higher entropy (e.g. ~9.25), and much lower energy (e.g. ~1/582.67), is to be expected for this sample if the max pressure response of the pressure mat interface was higher than subject's true maximum exerted pressure in a given cell. For this reason, sample 145-1-1601 was excluded during regression analysis. With the use of a proper pressure mapping interface with no capped-pressure readings and clusters, single measure such as Entropy (GLSD) at  $0^{\circ}(X)$  is representative of the second-order map texture.



<span id="page-135-0"></span>Figure 61. GLSD Energy X vs GLSD Entropy X (static data subset)

Measures of Entropy (GLSD) [at  $0^{\circ}(X)$ ] and Contact Cells also show a strong positive correlation ( $R^2 \approx 89.3\%$ ) when considering all samples included in the static data subset. Two unusual observations were found during regression analyses where the observed entropy values were lower than expected (see Figs. [62,](#page-136-0) [63\)](#page-136-1).



<span id="page-136-0"></span>Figure 62. GLDS Entropy X vs Contact Cells regression (static data subset)



<span id="page-136-1"></span>Figure 63. GLDS Entropy X vs Contact Cells residuals (static data subset)

By considering localized pressure changes to identify randomness (noise) in the pairwise pressure distribution at a given direction, GLSD Entropy values are expected to increase when the number of contact cells increase as a higher diversity of pressure readings is expected. But presence of homogeneous regions within a pressure map, relative to the contact pressure area, are also affecting the entropy value. Figure [64](#page-137-0) shows pressure maps where measures of Entropy (GLSD) were unusual and lower than expected considering the size of the pressure maps.



(b) 111-2-2878 Second Gradient Map (d) 189-3-3818 Second Gradient Map







\*Unusual Observation

<span id="page-137-0"></span>Figure 64. Contact Cells vs GLSD Entropy unusual observations (static data subset)

Common pressure measures, such as Sum of Pressure or Coefficient of Variation, do not show high correlations with proposed pressure measures; with measures of Skewness and Kurtosis only relating to each other ( $R^2 \approx 79.7\%$ ). On the other hand, Standard Deviation shows high correlations with various contrast measures, being the highest with the measure of Gradient Contrast X (GLD) ( $R^2 \approx 86.5\%$ ). But while the relationship between these measures is high, their approach for measuring contrast and variability is fundamentally different. Measures of Gradient Contrast are dependent on the spatial relationship of pressure readings, whereas Standard Deviation do not take this spatial relationship into consideration. Illustrative examples can be seen in Figure [65.](#page-138-0) The measure of Gradient Contrast in sample 186-1-3161 is high due to the presence of a spatially-related high-pressure region located among low pressure readings (see Fig. [65b](#page-138-1)), while measures of Standard Deviation are very similar for both of the pressure maps shown in this figure (i.e., no spatial relationships are considered).



<b>Sample</b>	161-1-1833	186-1-3161	
<b>Sum of Pressure</b>	19,865.39	19,567.5	
<b>Contact Cells</b>	386	393	
<b>Standard Deviation</b>	41.44064	40.77126	
GLD - Gradient Contrast X	1278.728863	1562.537572	

<span id="page-138-1"></span><span id="page-138-0"></span>Figure 65. Standard Deviation vs GLD Gradient Contrast X example (static data subset)

250

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100

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**Static Data Subset Summary.** In terms of spatial correlation measures, Morans' I appears to be more convenient to use than Geary's C. While they both behave similarly, Moran's I is easier to interpret. Analysis of the selection of the weight matrix for spatial autocorrelation measures indicate that higher spatial autocorrelations are obtained if area of interest (matrix moving window) is similar to the max-min size of expected autocorrelated high-pressure clusters. GLSD Correlation is also an acceptable measure of spatial autocorrelation; it does not require a described weight matrix and is more sensitive to localized pressure gradient variations. Higher GLSD Correlation values are usually obtained when measured in the anterior-posterior sitting direction  $[90^{\circ}(Y)]$ .

Many of the introduced image statistical features were also strongly correlated. In terms of measures of variability and gradients, Gradient Contrast (GLD) and Contrast (GLSD) are relatively the same measure, but the former is easier to compute and interpret. The same can be stated for Gradient Mean (GLD) and Gradient Entropy (GLD), being the former easier to compute and interpret. Measures of Gradient Contrast (GLD) and Gradient Mean (GLD) are both acceptable global measures of pressure map gradients. While they share many similarities, the Gradient Contrast (GLD) is more sensitive to pressure maps exhibiting a single or small group(s) of acute pressure points, while the Gradient Mean (GLD) is more robust to these high-pressure points. For these contrast measures, higher contrast values are usually obtained when measured in the lateral sitting direction  $[0^{\circ}(X)]$ . Compared to common measures of pressure variability such as Standard Deviation or Coefficient of Variation, Gradient Contrast (GLD) and Gradient Mean (GLD) also consider the spatial relationship of the pressure readings when assessing pressure map's variability.

Measures of Gradient Second Moment (GLD) and Homogeneity (GLSD) are unique and complementary measures for evaluating pressure maps' texture, smoothness and pressure regularity. Their differences lie in that Gradient Second Moment (GLD) is more sensible to changes in pressure gradients, while Homogeneity (GLSD) emphasizes more in measuring the transition and similarities within various pressure levels. Higher values in both measures are usually obtained when measured in the anterior-posterior sitting direction  $[90^{\circ}(Y)]$ .

Measures of Entropy (GLSD) and Energy (GLS) were found to be relatively the same. These measures are also correlated with Contact Cells (i.e., number of non-zero pressure readings), but they react differently if pressure maps exhibit high or low homogeneity given the size of the contact area. Using measures of Entropy (GLSD) or Energy (GLS) as global pressure descriptors is somewhat redundant if information on the number of contact cells and measures of homogeneity, such as Gradient Second Moment (GLD), are available. The information provided by contact cells and homogeneity can predict entropy/energy values with high accuracy ( $R^2 \approx 95\%$ ).

A dimensional reduction process focused on feature selection was followed by using high correlation filters ( $R^2 \geq 0.8$ ) in combination with analyses of regression models an evaluation of unusual observations. The goal was to select a set of measures where each selected feature is able to explain a unique user-chair interaction phenomenon. The selected pressure measures resulting from this analysis can be seen in [Table 23.](#page-141-0) Important common pressure measures are also included in this set. Each proposed measure has been categorized according to its potential use in pressure mapping analysis, along with important notes and recommendations for their applications.

In the following section, this reduced set of meaningful pressure measures are evaluated using paired-samples of static pressure maps from different subjects. As a result of information loss, these paired samples show no significant differences among common pressure measures (e.g. Contact Cells, Sum of Pressure, and Coefficient of Variation). These new measures are analyzed in their ability to discriminate and find differences (if any) among these paired samples, with the goal of effectively recovering the information loss.

<span id="page-141-0"></span>

Type	Measure	<b>Notes</b>	
General	<b>Contact Cells</b>	Indicates size of pressure area. A small high-pass pressure filter (e.g. 5 mmHg) is recommended to remove low pressure artifacts	
	<b>Sum of Pressure</b>	Measures the total amount of exerted pressure in contact area	
	<b>Skewness</b>	Measures high-low distribution of pressure readings	
Spatial Relation	Moran's I	Recommended area of weight matrix similar to max- min size of expected correlated high-pressure clusters	
	Correlation (GLSD)	Sensitive to localized pressure gradient variations. Higher values obtained along sitting direction axis (Y).	
	Coefficient of Variation	Non-spatial global measure of pressure variability	
Pressure Variability and Contrast	<b>Gradient Contrast</b> (GLD)	Sensitive when pressure maps have either a single or small group(s) of acute pressure points	
	<b>Gradient Mean</b> (GLD)	Robust to high-pressure points.	
<b>Smoothness</b> and Texture	Gradient Second Moment (GLD)	Sensitive to changes in pressure gradients	
	Homogeneity (GLSD)	Emphasizes in measuring the similarities within various pressure levels	

Table 23. Set of meaningful pressure measures

# **Paired Data Subset**

Similar to the sampling strategy used for creating the static data subset, stratified sampling of subjects' pressure maps was used following the distribution of the average coefficient of variation by subject (see Fig[. 47\)](#page-121-0). For each level of coefficient of variation, random paired samples were chosen if no significant differences ( $\Delta$  < 5%) were found across the following common pressure measures: Contact Cells, Sum of Pressure, and Coefficient of Variation. Ten (10) pairedsamples of pressure maps with various degrees of coefficient of variations were selected to create the paired data subset (see [Appendix J\)](#page-293-0).

**Paired-Samples Analysis.** To evaluate the discriminant power of newly proposed pressure measures, a meaningful difference between paired-samples is considered when a relative difference of at least ten percent is found between values of the proposed pressure measures  $(\Delta \ge 10\%)$ . For calculating Moran's I, an appropriate weight matrix (i.e., Queen, Constant-Distance, or Inverse-Distance) is selected for each paired-sample according to max-min size of the correlated high-pressure clusters in the samples. GLD and GLSD measures are also considered at both direction [90°(Y) and  $0^{\circ}(X)$ ]. Results of common pressure measures are presented along with any significant finding from the new pressure measures in each paired-sample.

As global descriptors of pressure distributions, the set of meaningful pressure measures in [Table 23](#page-141-0) are unable to find differences in terms of shape, orientation, or position between pressure maps; their emphasis is in describing pressure distribution patterns and spatial relationships within pressure maps. Their results are useful in identifying differences and similarities of the within-map intra-relationships of the pressure readings. Figures [66](#page-143-0) and [67](#page-144-0) are good examples of these restrictions; where differences in terms of shape, location, and spatial position of pressure clusters can be seen between paired samples. But focusing on the pressure distribution patterns and the overall relationship of the pressure readings and clusters, some similarities can be seen between these paired maps.

Figure [66](#page-143-0) shows a number of small high-pressure clusters in both maps, along with similarities in the spatial relationship between pressure levels. The main difference between these maps is seen in the pressure transitions between the legs and buttocks, where Figure [66b](#page-143-0) shows a more homogeneous transition than Figure [66a](#page-143-0). These small differences are being successfully detected by differences in the measures of pressure texture in the  $90^{\circ}(Y)$  direction.







(a) 150-2-1968 Pressure Map (b) 144-3-1841 Pressure Map

	<b>Pressure Measure</b>	Sample	Relative	∆ Plot		
<b>Type</b>			150-2-1968 144-3-1841	%		
	<b>Contact Cells</b>	288	293	1.74%		
General	<b>Sum of Pressure</b>	17411.35	17503.15	0.53%		
Variability	<b>Coefficient of Variation</b>	0.7959	0.7978	0.25%		
	<b>GLD - Gradient Second Moment Y</b>	0.0276	0.0320	16.00%		
Texture	GLSD - Homogeneity Y	0.0615	0.0709	15.19%		
			in the second contract of the second second to the second second the second second that the second second second the second			

\*Red highlight: No meaningful differences are found ( $\Delta \leq 10\%$ )

<span id="page-143-0"></span>Figure 66. Pressure measures for samples 150-2-1968 vs 144-3-1841 (paired data subset)

With respect to Figure [67,](#page-144-0) many similarities are also seen between the paired maps. These maps show similar pressure distribution patterns and similar high-pressure clusters in terms of size and magnitude (albeit in different locations). Minor differences can be seen in terms of pressure scattering as Figure [67b](#page-144-0) shows more texture and roughness in the right leg regions and Figure [67a](#page-144-0) shows more delineated acute pressure points close to the right ischial tuberosity. These minor differences are being successfully detected by differences in the values of gradient contrast (detecting acute points) and homogeneity (detecting texture differences).




(a) 120-2-1719 Pressure Map (b) 128-3-1298 Pressure Map

<b>Type</b>	<b>Pressure Measure</b>	Sample		<b>Relative</b>	∆ Plot	
			120-2-1719 128-3-1298	%		
	<b>Contact Cells</b>	388	386	$-0.52%$		
General	<b>Sum of Pressure</b>	16877.71	16871.47	$-0.04%$		
Variability	Coefficient of Variation	0.8247	0.8249	0.03%		
	<b>GLD</b> - Gradient Contrast Y	664.2320	592.9861	$-10.73%$		
Texture	GLSD - Homogeneity X	0.1026	0.0891	$-13.10%$		

\*Red highlight: No meaningful differences are found ( $\Delta \leq 10\%$ )

<span id="page-144-0"></span>Figure 67. Pressure measures for samples 120-2-1719 vs 128-3-1298 (paired data subset)

In general, paired-samples from Figures [66](#page-143-0) and [67](#page-144-0) are somewhat similar, with only minor differences seen in their pressure distributions. Only few of the reduced set of meaningful measures [\(Table 23\)](#page-141-0) were able to effectively capture these slight differences. The following selected examples show paired-samples where more significant differences were detected by the newly proposed pressure measures. A recurrent theme in these analyses is to also highlight the limitations of common pressure measures. All figures presented in this section show differences in measures of Contact Cells, Sum of Pressure, and Coefficient of Variation to be less than 5% (∆ < 5%), highlighting the information loss due to their inability to detect certain pressure distribution patterns. The full set of results for all paired-samples are shown in [Appendix K.](#page-297-0)

Figure [68](#page-145-0) shows paired-samples were significant differences are seen between maps' pressure distributions. The pressure map in Figure [68a](#page-145-0) shows better spatial relationship among pressure readings, with distinct presences of clusters of low- and high-pressure levels, smoother transitions between pressure levels, and greater homogeneity within the pressure levels. On the other hand, Figure [68b](#page-145-0) shows high-pressure readings being scattered throughout the map (e.g., upper legs and tuberosities), and higher variability among contiguous readings.







\*Red highlight: No meaningful differences are found ( $\Delta \le 10\%$ )

<span id="page-145-0"></span>Figure 68. Pressure measures for samples 122-3-51 vs 170-2-2787 (paired data subset)

The information loss while relying in common pressure measures is evident. Proposed pressure measures were able to effectively detect differences between the pressure maps shown in Figure [68.](#page-145-0) The scatteredness of high-pressure readings and the high-variability among contiguous readings in Figure [68b](#page-145-0) translate to lower spatial measures, higher gradient measures, and lower smoothness measures (i.e., increased texture) when compared to Figure [68a](#page-145-0). Figure [69](#page-146-0) shows another set of samples to further illustrate the discriminability of the new pressure measures.





(a) 118-2-61 Pressure Map (b) 188-2-2491 Pressure Map



\*Red highlight: No meaningful differences are found ( $\Delta \leq 10\%$ )

<span id="page-146-0"></span>Figure 69. Pressure measures for samples 118-2-61 vs 188-2-2491 (paired data subset)

By comparing the pressure maps shown in Figure [69,](#page-146-0) the scattered high-pressure clusters seen in Figure [69b](#page-146-0) significantly influence the measures of spatial relationship, pressure gradients, and map's texture when compared to Figure [69a](#page-146-0). Sample 188-2-2491 (Fig. [69b](#page-146-0)) also shows higher variability among contiguous readings and presence of acute pressure points in the upper legs. On the other hand, Figure [69a](#page-146-0) shows smoother transitions between pressure levels and more homogenous readings within clusters of various pressure levels. The coefficient of variation, commonly used to measure how evenly is the pressure distributed across the surface map, was unable to detect these differences in terms of the number of high-pressure clusters in Figure [69b](#page-146-0).

Figure [70](#page-148-0) shows another example with similar results to the ones shown in Figures 68 and [69.](#page-146-0) In this figure, the pressure map in Figure [70b](#page-148-0) shows higher texture and variability, and an increased number of disconnected high-pressure points/clusters. This leads to significant differences in measures of spatial relationship, gradients, and pressure homogeneity.

With the common pressure measures still showing similar values for the pressure maps in Figure [70,](#page-148-0) the measure of skewness is also indicating differences between the maps. Figure [70b](#page-148-0) is more positively skewed, that is, higher frequencies in the lower side of the pressure spectrum (0- 300 mmHg) is seen in the distribution of pressure readings. Seating pressure maps are expected to show positive skewness, as the number of relative low-pressure readings is usually significantly higher than the number of relative high-pressure readings. The skewness measure is able to quantify the degree of this relationship.

A visual representation of the distribution of the pressure readings for the pressure maps in Figure [70](#page-148-0) is shown in Figure [71.](#page-149-0) The presence of a higher frequency of low-mid pressure readings (50-110 mmHg) in sample 158-3-3717 (Fig. [70b](#page-148-0)) is traduced as a higher skewness value when compared to sample 137-2-922 (Fig. [70a](#page-148-0)). Sample 137-2-922 shows a higher frequency of mid-

pressure readings (110-180 mmHg), and lower frequency of low-mid pressure readings (50-110 mmHg) when compared to sample 158-3-3717, making the pressure distributions more negatively skewed. Note that measures of sum of pressure (i.e., the total exerted pressure in the pressure sensing area) and number of contact cells are relatively almost the same.





(a) 137-2-922 Pressure Map (b) 158-3-3717 Pressure Map



\*Red highlight: No meaningful differences are found ( $\Delta \le 10\%$ )

<span id="page-148-0"></span>Figure 70. Pressure measures for samples 137-2-922 vs 158-3-3717 (paired data subset)



<span id="page-149-0"></span>Figure 71. Pressure histograms for samples 137-2-922 vs 158-3-3717 (paired data subset)

**Paired Data Subset Summary.** Comparative results of the samples included in the paired data subset emphasize the importance of introducing new pressure measures to recover the information loss by current common pressure measures. The proposed measures of spatial relationship, variability, gradients, and smoothness and texture are useful complements to commonly used pressure measures; these new pressure measures are able to detect specific and unique pressure distribution patterns that commonly used pressure measures are unable to. The results in this section confirm that the set of meaningful pressure measures [\(Table 23](#page-141-0)**)** are valid and feasible to be used as global descriptors of pressure distribution within pressure maps. If used for comparative purposes, note that these measures are unable to identify differences in terms of shape, location and/or spatial position of pressure clusters. To overcome these limitations, image registration techniques are implemented and evaluated in the following section.

## **Image Registration and Similarity/Dissimilarity Coefficients**

The following subsections show the results of applying image registration techniques to compare pressure maps where significant changes are seen in terms of the shape, orientation, position and/or location of the pressure readings. Results from the following datasets are presented accordingly: (1) transformed data subset, used for evaluating performance and accuracy of registration techniques, and (2) registration data subset, used to analyze feasibility and practicality of proposed comparative techniques (image registration and similarity/dissimilarity coefficients) when significant movements occur (e.g., pressure map shifts, sitting reorientation or relocations).

While analyzing the transformed data subset, the similarity and dissimilarity coefficients are initially used as a supplementary benchmark to evaluate the accuracies and performances of the image registration techniques. Because the transformed pressure maps included in transformed data subset are in fact the same pressure maps as the reference maps (with very small differences due to the random transformation being applied), the resulting values of the similarity and dissimilarity coefficients at registration optimality can be used to benchmark the registrations procedure. A good registration procedure should result in approximately 1 in measures of similarity and 0 in measures of dissimilarity.

It is important to note that for pressure maps that are inherently different, such as the ones included in the registration data subset, the roles of the similarity and dissimilarity coefficients are changed to post-hoc comparative measures instead of benchmarking measures. In these instances, similarity and dissimilarity coefficients are only used to evaluate differences between registered maps at optimality. Higher (lower) values in measures of similarity (dissimilarity) do not necessarily indicate that a better registration was achieved by a particular registration method; but in cases where pressure map images share a number of commonalities and features, a proper correspondence between registered pressure map images generally results in an increase (decrease) of the similarities (dissimilarities) measures.

#### **Transformed Data Subset**

To evaluate the translational and rotational capabilities of the image registration techniques, a subset of the dataset consisting of ten (10) samples of pressure maps was used. Stratified sampling based on different levels of contact area was used to select the pressure map samples and create the transformed data subset (see Fig. [12\)](#page-78-0). Two random transformations, each with a random translational and rotational shift, were applied to each pressure map sampled; these were also included in the transformed data subset. Selected samples with applied random transformations are shown in [Appendix L.](#page-303-0)

Before running the optimal linear registration techniques [i.e., maximization of the Mutual Information (MI), or minimization of the Mean Square Errors (MSE)], the pressure map samples were upscaled to a factor of 10 (i.e., from a 32 x 32 map to a 320 x 320 map) to allow fine adjustments of the position and orientation of the pressure maps during image registration procedures.

Image registration algorithms were implemented from the SimpleITK  $(v1.2.0)$  python package, which was developed at the US National Institutes of Health (NIH) and also available in multiple programming languages (Yaniv et al., 2018). Before the registration process starts, an initial transformation is applied to center the images, and is defined by the geometric moments of gray level values computed from both images. This approach assumes that the moments of both pressure maps are similar, and hence the best initial guess for registering the images is to superimpose both mass centers (i.e., center of pressures).

After the initial centering, a number of transformations occur during the registration process. The transform used in this study applies a rigid transformation in 2D space with rotations represented by a Euler angle, and are specified as a rotation around an arbitrary center, followed by a translation. Linear interpolations are used to calculate resulting pressure map images during these transformations. Both registration method (MI and MSE) use the same acceleration settings, convergence settings, and optimality parameters during the registration process. Gradient descent is being used as the optimization algorithm during image registration.

Initial centering based on the geometric moments significantly reduced any translation and location differences between pressure maps. Unfortunately, significant rotational differences between pressure maps were found to have meaningful effects during registration procedures. After applying Mutual Information (MI) image registrations to the transformed data subset, results showed instances where large initial rotation differences between the maps significantly affected the registration performance and accuracy. An example is shown in Figure [72](#page-152-0) where pre-registered pressure maps for sample 126-2-2177 are shown. The template image shown is the resulting map after applying a random transformation (60° rotation, and horizontal and vertical translations).



MI Image Registration: 126-2-2177 vs 126-2-2177T, Scaling Factor: 10

<span id="page-152-0"></span>Figure 72. Sample 126-2-2177, original and transformed maps (transformed data subset)

Figure [73](#page-153-0) shows the results of registering the pressure maps presented in Figure [72](#page-152-0) with both registration methods (MI and MSE). Results of the Mutual Information (MI) registration were not appropriate at optimality (25 iterations), as additional rotation transformations are needed for better images' correspondence (see Fig. [73,](#page-153-0) top). Similarity and dissimilarity coefficients are also shown in the figure. Note that non-standardized metrics such as  $L_1$  Norm and Squared  $L_2$  Norm are in magnitude of  $10^2$  due to scaling factors. The registration error obtained at MI registration optimality led to a non-scaled  $L_1$  Norm measure (non-masked) of 10,983.49 mmHg, representing approximately a 90.45% pressure error in pressure maps' correspondence.



MI Image Registration: 126-2-2177 vs 126-2-2177T, Iteration 25 Metric: - 0.8112565578452797

MSE Image Registration: 126-2-2177 vs 126-2-2177T, Iteration 292 Metric: 5.818409527945756



<span id="page-153-0"></span>Figure 73. Sample 126-2-2177, optimal MI and MSE registration (transformed data subset)

Figure [73](#page-153-0) also shows the results of registering the pressure maps presented in Figure [72](#page-152-0) with the Mean Square Error (MSE) registration method (see Fig. [73,](#page-153-0) bottom). MSE results shows an improvement in the registration procedure by obtaining better images' correspondence when compared to MI results. MSE registration shows a non-scaled  $L_1$  Norm (non-masked) of 783.11 mmHg, representing approximately a 6.45% pressure error between images, with optimality being achieved after 292 iterations (3.2s processing time).

Figure [74](#page-154-0) shows pressure map differences at MSE optimality (see Fig. [73,](#page-153-0) bottom). These pressure map differences are calculated by subtracting the pressure readings of the transformed template pressure map (i.e. moving map) to the pressure readings in the reference pressure map (i.e. fixed map). This figure shows a low-pressure lattice pattern for the pressure differences across the pressure maps with some slight pressure differences around the left ischial tuberosity. This lattice pattern is expected if a proper and successful registration is made on equal pressure maps.



MSE Image Registration: 126-2-2177 vs 126-2-2177T, Iteration 292 [Reference - Transformed] (mmHg)

<span id="page-154-0"></span>Figure 74. Sample 126-2-2177, optimal MSE registration differences (transformed data subset)

Another example where the registration procedure was affected by the significant rotation difference between pre-registered pressure map is shown in Figure [75.](#page-155-0) This figure shows the reference pressure map for sample 175-3-1142 along the template image resulting after applying a random transformation (35° rotation, and horizontal and vertical translations).



MI Image Registration: 175-3-1142 vs 175-3-1142T, Scaling Factor: 10

<span id="page-155-0"></span>Figure 75. Sample 175-3-1142, original and transformed maps (transformed data subset)

Figure [76](#page-156-0) shows the results of registering the pressure maps presented in Figure [75](#page-155-0) with both registration methods (MI and MSE). Results of using MI registration were again unsuccessful between these pressure maps, with additional rotation transformations still needed for better images' correspondence (see Fig. [76,](#page-156-0) top). An 83.27% pressure error in images' correspondence is detected by the  $L_1$  Norm measure (non-masked) at MI optimality. On the other hand, a successful and proper registration was achieved when using MSE registration, with a 6.37% pressure error as per the  $L_1$  Norm measure (non-masked). Figure [77](#page-156-1) shows pressure map differences at MSE optimality. This figure shows the expected low-pressure lattice pattern of the pressure differences between the pressure maps, with slight pressure differences around the mid-ischial tuberosities region.



MI Image Registration: 175-3-1142 vs 175-3-1142T, Iteration 15 Metric: - 0.8457956617867095

MSE Image Registration: 175-3-1142 vs 175-3-1142T, Iteration 124 Metric: 18.426114469712083



<span id="page-156-0"></span>Figure 76. Sample 175-3-1142, optimal MI and MSE registration (transformed data subset)



MSE Image Registration: 175-3-1142 vs 175-3-1142T, Iteration 124 [Reference - Transformed] (mmHq)

<span id="page-156-1"></span>Figure 77. Sample 175-3-1142, optimal MSE registration differences (transformed data subset)

Previous examples demonstrate how significant differences in rotation between pressure map images can have adverse effects when performing MI registration procedures; however, this is not always the case. Figure [78](#page-157-0) shows pre-registered pressure maps for sample 109-2-265 along with the template image resulting from applying a random transformation (36° rotation, and vertical and horizontal translation). While this transformation is similar to the one applied in Figure [75,](#page-155-0) the registration results were successful when using both registration methods. Figure [79](#page-157-1) shows proper registrations when using MI or MSE, with better results being obtained when using the latter (10.55% and 5.59%  $L_1$  Norm (non-masked) pressure error for MI and MSE respectively).



MI Image Registration: 109-2-265 vs 109-2-265T, Scaling Factor: 10

<span id="page-157-0"></span>Figure 78. Sample 109-2-265, original and transformed pressure maps (transformed data subset)

MI Image Registration: 109-2-265 vs 109-2-265T, Iteration 31



MSE Image Registration: 109-2-265 vs 109-2-265T, Iteration 134

<span id="page-157-1"></span>Figure 79. Sample 109-2-265, optimal MI and MSE registration (transformed data subset)

Excluding unsuccessful registrations for samples 126-2-2177 (Fig. [73\)](#page-153-0) and 175-3-1142 (Fig. [76\)](#page-156-0), proper registrations where generally achieved by MI for all other samples, with an average  $L_1$  Norm (non-masked) pressure error of 8.92% and non-masked Pearson Correlation Coefficients of at least 0.9 ( $r \ge 0.9$ ). However, using optimal linear registration based on Mean Square Errors (MSE) minimization generally results in more accurate registration procedures.

Excluding unsuccessful registrations, Figure [80](#page-158-0) shows the non-masked similarity and nonmasked dissimilarity scores at registration method's optimality for all other samples in the transformed data subset. A total of twenty registrations (ten pressure map samples, each with two applied random transformations) were completed by each registration method. Individual points in the figure represents the similarity/dissimilarity score achieved by the registration method in each registered sample. Tanimoto similarity scores are not shown in the figure as their behavior was almost the same as the Pearson similarity scores ( $R^2 = 99.85\%$ ). As seen in the figure, higher similarities scores and lower dissimilarities scores are generally obtained with MSE registration.



<span id="page-158-0"></span>Figure 80. Non-masked similarity and dissimilarity scores plots (transformed data subset)

As explained earlier in this section, the similarity and dissimilarity coefficients are being used as a supplementary benchmark to evaluate the accuracies and performances of the image registration techniques while evaluating the transformed data subset. Due to the fact that registered pressure maps are almost identical to the reference maps, with differences being due to random applied transformations, a registration method achieving a high similarity and low dissimilarity is desired. The similarity and dissimilarity coefficient results obtained at MSE optimality generally outperform the ones obtained at MI optimality. Visual feedback of the registration process also confirms that MSE generally achieves optimal registrations with higher accuracies and better images' correspondences. [Table 24](#page-159-0) shows the results of one-sided Wilcoxon signed-rank tests, including results from all samples, of the similarity and dissimilarity metric scores between MI and MSE optimalities. These paired difference tests show that MSE registration achieves significantly better results than MI registration at  $\alpha = 0.05$ . The results of samples' similarity and dissimilarity coefficients obtained at MI and MSE optimalities are shown in [Appendix M.](#page-314-0)

<span id="page-159-0"></span>Table 24. MI vs MSE: Wilcoxon signed-rank tests for similarity and dissimilarity results



**Transformed Data Subset Summary.** Image registration methods based on optimal linear models of Mutual Information (MI maximization) or Mean Square Errors (MSE minimization) were, for most samples, suitable for aligning the pressure map images in the transformed data subset (i.e., mostly identical pressure maps). The pressure map resolutions obtained with these

samples (32x32) required upscaling (e.g., factor of 10) to allow fine rotation and translation adjustments during the registration process. Initial centering using image moments (i.e., center of pressures) and subsequent 2D rigid transformation were generally adequate to achieve good registration for both MI and MSE registration methods.

In some instances, Mutual Information exhibited registration issues when significant rotation differences are present among pressure map images. On the other hand, results using MSE provided proper and accurate registration for all samples included in the transformed data subset. While Mutual Information generally reached optimality at a faster rate (53 less iterations on average when compared to MSE registration), MSE provided significantly higher accuracy and better images' correspondence at optimality (see Fig. [80](#page-158-0) and [Table 24\)](#page-159-0).

Similarity and dissimilarity coefficients, which quantify the relationship between pressure images, generally confirmed good registrations at optimality, particularly for MSE. Use of MSE registration resulted in an average Pearson Correlation Coefficient of  $r = 0.9966$  and a 6.11% average pressure error from  $L_1$  Norm among all registered samples.

#### **Registration Data Subset**

This section shows the results and evaluations of using image registration techniques and similarity and dissimilarity measures for analyzing and comparing pressure maps during dynamic sitting. For this purpose, the registration data subset was created using twenty (20) samples of pairs of pressure maps selected by stratified sampling based on the different levels of contact area (Fig. [12\)](#page-78-0). Each sample pair was selected from indexes in a continuous sitting interval (within-subject) where a potential significant positional shift or movement is detected. A potential significant movement is considered as a translation of the center of pressure greater than one inch ( $\Delta CP >$ 1 *in*) within a twenty seconds time window. Sample pairs selection was done while screening the

dynamic movement to confirm that pressure maps selected are not within-movement, but rather to select pre-movement pressure maps (with relative pre-movement stability) and a post-movement pressure maps (with relative post-movement stability). [Appendix N](#page-316-0) shows the selected pressure map indexes from various sitting intervals (within-subjects) with the translation distances of the Center of Pressure (CP) and the time window in frames (1 index  $\sim$  1 second). Sampled pressure maps were again upscaled by a factor of 10 for registration purposes. Upscaled pressure maps of selected sample pairs are shown in [Appendix O.](#page-318-0)

Given that MI and MSE registrations have different optimality metrics, and that the use of similarity and dissimilarity coefficients as a registration benchmark is not appropriate for pressure maps that are inherently different, visual feedback was used to assess images' registrations and correspondences results for MI and MSE registration optimality in all pairs of pressure map samples. Subjective assessments of the seating pressure map alignments completed by each registration method was done using expert knowledge. Iterative pressure map overlays and maps with highlights of pressure differences during registrations were used for visual feedback assessments. The results of MI and MSE registration optimalities for all pairs of pressure map samples, along with notes from the subjective visual feedback assessments, can be seen in [Appendix Q.](#page-328-0)

Assessments via visual feedback found that in twelve out of the twenty registered samples, there were no visually noticeable differences between the optimality results of MI registration and MSE registration, with both registration methods producing proper and accurate alignments between the seating pressure maps. Visual assessments also showed that optimal results from MI and MSE were found to be visually distinguishable in six others of the registered samples (see notes in [Appendix Q\)](#page-328-0), with MSE producing better image correspondences in all of these samples.

Figures [81](#page-163-0) and [82](#page-164-0) show some of the examples where visually distinct registrations are found between image registrations (MI and MSE). In both of these examples, MSE registration was able to identify and correctly align the locations of the ischial tuberosities and legs regions during the registration, greatly improving the images' correspondence. The improvement in the images' correspondence achieved by MSE registration results in some measures showing higher (lower) similarities (dissimilarities) when compared to results from the MI registration (e.g., [Figure](#page-163-0) [81](#page-163-0) shows MSE results of 0.904 and 7,778.48 mmHg for non-masked variations of Pearson and non-scaled  $L_1$  Norm respectively, while MI shows results of 0.851 and 7,802.28 mmHg for these same measures). Note that not every similarity or dissimilarity coefficient improves when using MSE registration over MI registration (e.g., [Figure](#page-164-0) 82 shows higher non-masked Pearson values when using MSE over MI [0.819 vs 0.786], but lower non-masked non-scaled  $L_1$  Norm values are obtained when using MI [6,631.85 mmHg vs 7,778.48 mmHg]).

Visual feedback assessments also found two pairs of samples where misalignments of the pressure map images are present at optimality when using either registration (MI or MSE). Figures [83](#page-165-0) and [84](#page-166-0) show the pressure maps for these pairs of samples along with optimal registration results from MI and MSE, where evidence of incorrect alignments at registration optimalities are seen.

For the pressure map samples obtained from subject 169 (Fig. [83\)](#page-165-0), both MI and MSE registrations attempted to align the pressure clusters in the ischial tuberosities from the template image (moving image) with the pressure clusters in the mid-tights regions of the reference image (fixed image). In this instance, the lack of distinct high-pressure clusters around the ischial tuberosities in the reference image and the significant difference in the size between pressure maps greatly affected the images' correspondence during both MI and MSE registration procedures.



Image Registration: 114-2-1826 vs 114-2-1836, Scaling Factor: 10







MSE Image Registration: 114-2-1826 vs 114-2-1836, Iteration 26 Metric: 366.45105250150675





<span id="page-163-0"></span>Figure 81. Subject 114, optimal image registration: MI vs MSE (registration data subset)



Image Registration: 152-1-1986 vs 152-1-1990, Scaling Factor: 10







MSE Image Registration: 152-1-1986 vs 152-1-1990, Iteration 15 Metric: 317.74378949193886





<span id="page-164-0"></span>Figure 82. Subject 152, optimal image registration: MI vs MSE (registration data subset)



Image Registration: 169-2-1993 vs 169-2-2009, Scaling Factor: 10





MSE Image Registration: 169-2-1993 vs 169-2-2009, Iteration 7 Metric: 813.4337766317217





<span id="page-165-0"></span>Figure 83. Subject 169, optimal image registration: MI vs MSE (registration data subset)



Image Registration: 174-3-958 vs 174-3-970, Scaling Factor: 10







MSE Image Registration: 174-3-958 vs 174-3-970, Iteration 119 Metric: 856.9876533029358





<span id="page-166-0"></span>Figure 84. Subject 174, optimal image registration: MI vs MSE (registration data subset)

In samples obtained from subject 174 (Fig. [84\)](#page-166-0), the differences in the seating pressure maps from index 958 to 970 (approximately twelve seconds) shows a complete re-orientation of the legs. Image registration methods have to account for a rotational difference of around  $70^0$  to be able to provide an adequate registration with proper images' correspondence. Compared to MSE registration results, MI registration was able to detect the need for significant rotational transformations by showing registered pressure maps with better alignments, particularly in the legs regions, but more rotation transformations are still needed for a proper registration. On the other hand, MSE registration focused on aligning the mid- and high-level pressure clusters around the mid-regions of the pressure maps, where most of the pressure is located. The pressure readings under the leg regions were possibly not significantly considered by the MSE registration procedures due to having relatively low-pressure values, with the rotational transformations applied by the MSE registration actually being made in the opposite direction (not in alignment with the legs orientation).

Findings from the visual feedback assessments indicate that using image registration methods based on the minimization of the Mean Square Errors (MSE) results in alignments of seating pressure map images that are equal to or better than the ones obtained when using MI image registration. In twelve out of the twenty registered samples (60%), no visually noticeable differences were seen between the registration methods, but significantly improved alignments and images' correspondences where seen in six of out of the twenty registered samples (30%) when using MSE registration.

As explained earlier in this section, higher (lower) values in measures of similarity (dissimilarity) do not necessarily indicate that a better registration is achieved by a particular registration method. Nonetheless, an increase (decrease) in similarity (dissimilarity) measures is generally seen if proper correspondences are obtained at registration optimality between images that truly share a number of commonalities and features. In the pairs of samples where the MSE registration resulted in better pressure map alignments and images' correspondence, significant improvements in the measures of similarity such as Pearson and Tanimoto and dissimilarity measures such as  $L_1$  Norm and Squared  $L_2$  Norm were seen, possibly due to the better image correspondences achieved by MSE (see [Appendix P\)](#page-326-0). Measures of similarity and dissimilarity were not significantly different in instances where the registration results from MI and MSE were not visually distinguishable; but values of these coefficients where marginally better, in most cases, when using MSE registration due to slightly better images' correspondences (see [Appendix P\)](#page-326-0).

Different approaches for measuring similarities and dissimilarities (masked vs nonmasked) were used in this study. Differences of their use and application are now more evident when using the registration data subset; this is due to the pressure maps images included in this dataset being inherently different (as opposed to the ones used in the transformed dataset). When calculating similarities and dissimilarities coefficients using the masked approach, only non-zero pressure readings sharing the same locations in both pressure map images are considered, while the non-masked approach considers these unbalanced pressure readings (i.e., for a particular pressure map location, one pressure map has a non-zero pressure reading while the other pressure map does not).

When using the non-masked approach, a penalty while calculating the similarity and dissimilarity coefficients was expected due to unbalanced pressure readings being considered. Most of the similarity and dissimilarity measures concur with this logic, as measures such as Tanimoto, Minimum Ratio,  $L_1$  Norm, and Squared  $L_2$  Norm show lower (higher) similarities (dissimilarities) when using the non-masked approach. But a contrasting behavior is seen for the

Pearson Correlation Coefficient and Intensity-Ratio Variance measures, as these improve when considering unbalanced paired readings (see [Appendix P\)](#page-326-0).

The improvements obtained by the Pearson Correlation Coefficient and Intensity-Ratio Variance measures when considering a non-masked approach are possibly due to the fact that most pressure readings' location mismatches (i.e., non-overlapping pressure readings) occur around the outlines of the pressure maps, where readings with low-pressure values are mainly present. These mismatches in the outlines of the pressure maps (e.g., a low-pressure reading in a pressure map matched with a zero pressure readings in the other pressure map) can result to a higher Pearson Correlation Coefficient or lower Intensity-Ratio Variance due to their approach in calculating Sum of Squares Error (SSE) (see Equations [17](#page-64-0) and [22\)](#page-64-1).

The non-masked and masked approaches for measuring the similarities and dissimilarities between pressure map images have their unique purpose and use. A research study where the goal is measuring the similarity/dissimilarity of only shared features (i.e. overlaps) between pressure map images might be inclined on evaluating the masked variation of these coefficients. While a research study where the goal is measuring all true differences between pressure map images might be inclined to evaluate the non-masked variation of the similarity/dissimilarity coefficients.

Throughout this study, the non-masked variation was the favored approach as it considers all pressure readings differences between pressure map images. The following analysis evaluates the differences in the similarity and dissimilarity coefficient values obtained for each registration method when using the non-masked approach.

Figure [85](#page-170-0) shows the paired differences in the similarity and dissimilarity values between image registration optimalities. These paired differences are calculated by subtracting the results obtained when using MSE registration to the ones obtained when using MI registration. In this figure, similarity measures from Pearson and Tanimoto and dissimilarity measures from  $L_1$  Norm and Square  $L_2$  Norm indicate that higher (lower) similarities (dissimilarities) are seen between registered pressure map samples when using MSE registration, again, possibly due to better images correspondences' of pressure map samples. Ratio based measures (i.e., Minimum-Ratio and Intensity-Ratio Variance) indicate that similarities/dissimilarities seen between registered pressure map samples are very similar when using MI registration or MSE registration (see Fig. [85\)](#page-170-0).



<span id="page-170-0"></span>Figure 85. MI vs MSE non-masked similarity/dissimilarity differences (registration data subset)

[Table 25](#page-171-0) shows descriptive statistics for all similarity and dissimilarity coefficients along with one-way Wilcoxon signed-rank tests to compare results from the image registration methods (MI vs MSE). At  $\alpha = 0.05$ , significant differences are generally seen between the similarity and

dissimilarity values obtained by each registration method. These results indicate that significantly higher (lower) similarities (dissimilarities) are generally seen between registered pressure map when using MSE registration as compared to MI registration. Again, it is important to emphasize that higher similarities or lower dissimilarities do not necessarily indicate that a better registration or alignment between pressure maps was found by a particular registration method. These differences in values of similarity and dissimilarity coefficients between the registration methods are possibly due to the fact that pressure map alignments attained by MSE generally resulted in better registrations and correspondences of the pressure readings (as confirmed via visual feedback assessments). On the other hand, values for ratio-based measures indicate that the similarities (dissimilarities) seen between the registered pressure map samples are not significantly different when using MI or MSE registration. The ratio-based measures are somewhat unique compared to other coefficients, with them being particularly sensitive to pressure map shapes and/or scale differences; more details on their sensitivities are presented in the case study (Chapter 6).

<span id="page-171-0"></span>Table 25. Non-masked similarity/dissimilarity coefficients: descriptive statistics, one-sided

	Coefficient	<b>Method</b>	<b>Mean</b>	<b>StDev</b>	Min	<b>Median</b>	<b>Max</b>	p-value	
Similarity	Pearson	MI	0.8543	0.0764	0.6286	0.8522	0.9616	0.001	$\mu_{MSE}$
		<b>MSE</b>	0.8726	0.055	0.7416	0.8688	0.9675		
	Tanimoto	MI	0.7564	0.1183	0.495	0.773	0.9366	0.001	$\Lambda$
		<b>MSE</b>	0.7764	0.1022	0.5342	0.7815	0.9457		$\mu_{MI}$
	Min-Ratio	MI	0.5832	0.093	0.3793	0.5867	0.7472	0.743	$H_o$ :
		<b>MSE</b>	0.5805	0.1018	0.3201	0.5791	0.7463		
Dissimilarity	$L_1$ Norm	MI	854,234	298,948	547,894	730,774	1,498,689	0.032	
		<b>MSE</b>	833,580	271,001	538,889	713,017	1,357,217		$\mu_{MSE}$
	$Sq L_2$ Norm	MI	$4.2E + 07$	$2.9E+07$	$1.1E + 07$	$3.6E + 07$	$1.2E + 08$	0.001	VI
		<b>MSE</b>	$3.8E + 07$	$2.3E+07$	$1.1E+07$	$3.3E + 07$	$1.0E + 08$		
	Int-Ratio	MI	2.063	4.034	0.164	0.766	17.881	0.294	$H_{o}{:}\mu_{MI}$
	Var	<b>MSE</b>	1.48	1.848	0.165	0.536	6.525		

Wilcoxon signed-rank tests (registration data subset)

Information about the number of iterations and processing time for each pairs of registered samples are shown in [Appendix P.](#page-326-0) When using the SimpleITK  $(v1.2.0)$  python package, it is important to emphasize that the stopping criteria for the registration procedures do not necessarily trigger during the optimal iteration. Multiple points of interest are generally found during registration procedures, and a single optimal point is chosen by the algorithm among the points of interest. As an example, Figure [86](#page-172-0) shows a time series plot of the Mutual Information (MI) values during the registration process for paired-samples 110-2-1065 and 110-2-1073.



<span id="page-172-0"></span>Figure 86. MI iteration values, samples 110-2-1065 vs 110-2-1073 (registration data subset)

In addition to the initial transformation (iteration 0), two other preliminary transformations where used by the MI registration process of these paired-samples. These transformations occurred in iterations 11 and 15, and are represented as blue stars in the figure (see Fig. [86\)](#page-172-0). Transformations following each preliminary transformation attempted to increase the mutual information values between registered pressure map images, by using the minimization of the negative mutual information as the objective function during gradient descent optimization. This same principle is used for MSE transformations using the minimization of the mean squared errors as the objective function during gradient descent optimization. For the example shown in Figure [86,](#page-172-0) three points of interest were found in this registration process [10, 14, 21], with the tenth iteration (10) being chosen as the optimal iteration due its lower negative mutual information value.

Figure [87](#page-173-0) shows boxplots of the processing times when using MI and MSE registrations for the pressure map samples in the registration data subset. On average, MSE registration requires approximately 28 more iterations than MI registration, which translates to an additional time of 1.93 seconds. The highest processing time observed was 2.58 seconds (52 iterations) using MI registration and 15.59 seconds (171 iterations) using MSE registration. For the sample with the highest processing time using MSE registration (171 iterations), the registration process actually reached local optimality at iteration 17, with subsequent iterations trying different transformations to improve registration results (generally the case for MSE registrations). On average, MI required 1.14 seconds to complete the registration process while MSE required 3.07 seconds.



<span id="page-173-0"></span>Figure 87. MI vs MSE computing time (registration data subset)

**Registration Data Subset Summary.** Results of the implementation of image registration techniques and similarity and dissimilarity measures for analyzing and comparing pressure maps during dynamic sitting (e.g.,  $\Delta CP>1$  in) were generally successful. MI image registration methods were found to provide adequate alignments of pressure map images in most cases, but MSE image registration results were found to be equal to or better than the ones obtained by MI registrations. In twelve out of the twenty registered samples (60%), no visually noticeable differences were seen between the registration methods, but significantly improvements in alignments and images' correspondences where seen in six of out of the twenty registered samples (30%) when using MSE registration. Pearson and Tanimoto similarity measures, and  $L_1$  Norm and Square  $L_2$  Norm dissimilarity measures indicate that significantly higher (lower) similarities (dissimilarities) are observed between registered pressure map samples when using MSE image registration compared to MI image registration, possibly due to the better images correspondences' of pressure map samples achieved by the MSE registrations.

Evidence of incorrect alignments of the pressure map images at registration optimalities were found in two pairs of samples (10%) when using either MI or MSE image registration methods. Pressure maps commonalities, such as shared delineated shapes and similar locations of high- and low-pressure cluster, significantly improves the registration procedures; a significant lack of any of these could possibly result in inadequate optimal registrations (see Figs. [83,](#page-165-0) [84\)](#page-166-0). The lack of distinct high-pressure clusters (e.g., those normally found around the ischial tuberosities), significant differences in pressure map sizes, and/or significant re-orientations of relatively low-pressure readings (e.g., changes in facing of the legs) were possible factors that attributed to inaccurate registration for these misaligned samples.

Measures of similarity and dissimilarity using proposed coefficients were found to be adequate for measuring and comparing differences between pressure map images. Variations when calculating the similarity and dissimilarity coefficients (i.e., masked or non-masked approach) provided different comparison basis. The masked approach is aimed at research studies where the goal is to compare pressure map images while only considering common pressure regions (i.e. overlaps), while the non-masked approach is aimed at research studies where the goal is to measure all true differences between pressure map images.

In the context of seating pressure map images, similarity measures of Tanimoto and Minimum Ratio were found to be generally lower when using the non-masked approach, while dissimilarity measures of  $L_1$  Norm and Squared  $L_2$  Norm were generally higher. This is due to the non-masked approach taking into consideration all true differences between the pressure map images. But a contrasting behavior is seen for the Pearson Correlation Coefficient and Intensity-Ratio Variance measures, as these improve when using the non-masked approach. This is possibly due to the fact that most pressure readings' location mismatches (i.e., non-overlapping pressure readings) occur around the outlines of the pressure maps, where readings with low-pressure values are mainly present.

In regard to computational times, MSE image registrations, on average, required approximately 28 more iterations than MI image registrations, which translates in requiring and average time of 3.07 seconds to complete the registration process while MI image registrations only required 1.14 seconds on average. Both were implemented using the SimpleITK (v1.2.0) python package.

## CHAPTER VI

# CASE STUDY

Results from Chapter 5 show that a number of spatial data analytics and image processing techniques are useful and effective for cleansing, evaluating, aligning, and comparing pressure map images. In this case study, the applications of selected techniques are evaluated in terms of continuous sitting, where subjects' pressure maps are constantly captured within a given time interval. A 5-minute sitting interval sample (referred as to dynamic data subset) with a number of sequential spatio-temporal pressure images from one of the subjects in the dataset is used for this case study. As seating subject's frequently change their seating postures during prolonged sitting, changes in pressure distributions and location and orientation of the pressure readings are made constantly. The main goal in this case study is to evaluate the real-life applications of these methods and techniques under dynamic sitting.

The effectiveness of selected spatial clustering methods as pre-processing techniques for continuous pressure mapping are initially examined. Selected spatial clustering methods are evaluated by their performances in continuous data cleansing (i.e., removing unwanted pressure artifacts from continuous pressure maps). The density-based spatial clustering technique providing the highest overall accuracies in detecting extrinsic pressure artifacts (outliers) and true contact pressure readings (non-outliers) is selected as the pre-processing techniques applied to the dynamic data subset for subsequent analyses.

After the extraneous pressure maps artifacts are removed, the set of meaningful pressure measures featured in [Table 23](#page-141-0) were calculated and evaluated in terms of their practicality and feasibility as measures of dynamic pressure. The application of sequential image registration (using minimization of the Mean Squared Errors [MSE]) as a tool to align dynamic pressure map imagesis also evaluated. Similarity and dissimilarity coefficients are also evaluated as comparative dynamic measures for post-registered continuous pressure maps. Comparisons to the initial reference index (Index 1) are used as a way of measuring continuous pressure map changes over time. Computation demands for continuous pre-processing (data cleansing) and sequential image registrations (pressure map alignments) are also discussed in this chapter.

## **Data Sample**

To evaluate the applications of selected spatial data analytics and image processing techniques under continuous dynamic sitting, a single 5-minute sitting interval sample of continuous pressure maps was used (dynamic data subset). The sampled interval includes a number of within-subject sequential spatio-temporal pressure maps, and was selected from the first sitting interval during the second data collection session (Trial 2) of Subject 109. This 5-minute interval contains 281 individual frames with extrinsic pressure artifacts continuously present within the recorded pressure maps. Significant pressure redistributions and potential evidence of dynamic sitting are also present in the sampled interval.

#### **Pre-Processing: Spatial Clustering**

The results compiled in [Table 22](#page-119-0) (Chapter 5) show that algorithms based on DBSCAN and DENCLUE, when using only the pressure readings' location information as input data, were

suitable for pre-processing seating pressure maps. With proper parameter settings, these algorithms exhibited high accuracies when discriminating extrinsic pressure artifacts (outliers) and true contact pressure readings (non-outliers) in seating pressure maps. These density-based spatial clustering algorithms are evaluated in this case study for their abilities in detecting extrinsic pressure readings artifacts in continuous pressure map.

Unwanted pressure readings and extrinsic artifacts were defined and selected via expert knowledge for all 281 pressure maps withing the dynamic data subset. Selected density-based spatial clustering algorithms (see [Table 26\)](#page-178-0) were then executed while calculating measures of outliers and non-outlier accuracies for all continuous pressure maps. The aim is to select the bestperforming combination (i.e., clustering methods and parameter settings) from [Table 26](#page-178-0) by using the overall accuracy (i.e., calculated weighted average of both outliers and non-outliers accuracies) as the measuring criteria. The best-performing combination was used as the pre-processing techniques applied to the dynamic data subset for subsequent analyses.

Method	Parameters	Input Data
DBSCAN-1	eps: 1.60, 1.80 min_samples: 8	Location
<b>DENCLUE-1</b>	eps: 2 min_density: 1.7e-03	Location
DBSCAN-2	eps: 2.00, 2.20 min_samples: 10	Location
DENCLUE-2	eps: 0.01 $min\_density: 1.65e-03$	Location
DBSCAN-3	eps: 2.5 min_samples: 10	Location

<span id="page-178-0"></span>Table 26. Parameter settings and clustering methods evaluated (dynamic data subset)

The pressure map samples included in the dynamic data subset show high consistency in the locations of extrinsic pressure artifacts cluster and locations of scattered unwanted pressure readings. Figure [88](#page-180-0) shows original pressure maps (non-cleansed) of some of the samples where various extrinsic pressure artifacts (outliers) are present. This figure also shows the expert-created outliers references maps where these outliers are being pre-identified as noise (black dots); these served as basis for calculating clustering algorithms' accuracies.







(a) Original 109-2-1 Pressure Map (b) 109-2-1 pre-identified outliers (black)



(c) Original 109-2-115 Pressure Map (d) 109-2-115 pre-identified outliers (black)


<span id="page-180-0"></span>Figure 88. Examples of original pressure maps from interval sample 109-2 with marked outliers

The original pressure maps presented in Figure [88](#page-180-0) show clearly demarked regions of pressure outliers caused by extrinsic artifacts at the bottom of the pressure map images, with other pressure reading outliers being scattered throughout these pressure maps. Pre-processing techniques for continuous data cleansing are needed for eliminating these unwanted pressure readings and artifacts.

For most of the pressure maps in the dynamic data subset, the selected density-based spatial clustering algorithms [\(Table 26\)](#page-178-0) were able to correctly identify and classify pressure artifacts (outliers) and true contact pressure readings (non-outliers). However, the algorithms were not able to correctly discriminate these extrinsic artifacts from the true pressure readings in some of the pressure maps. Figure [89](#page-181-0) shows the pressure map sample (109-2-203) where the lowest overall accuracies were observed for the DBSCAN-1 and DBSCAN-2 clustering methods, both marking a number of non-outlier pressure readings as outliers. Clustering algorithms results from DBSCAN-3, DENCLUE-1, and DENCLUE-2 showed a 100% overall accuracy while classifying outlier and non-outliers for this specific sample.



(a) Original 109-2-203 Pressure Map (b) 109-2-203 Outlier Reference









(c) 109-2-203 Results (DBSCAN-1) (d) 109-2-203 Results (DBSCAN-2)



<span id="page-181-0"></span>Figure 89. Clustering results for sample 109-2-203 (location-only data)

The lowest overall accuracies observed for the DBSCAN-3, DENCLUE-1, and DENCLUE-2 clustering algorithms were seen in sample 102-2-208 (see Fig. [90\)](#page-183-0). While these clustering algorithms were able to identify the cluster of outliers at the bottom of the pressure map, Figure 90 shows their inefficacy in correctly identifying some of the pre-identified outliers in the leg regions, thus significantly affecting their outlier accuracy scores. DBSCAN-1 and DBSCAN-2 clustering algorithms were able to classify all the pre-identified outliers included in this pressure map sample. Unfortunately, their more aggressive approach in marking pressure readings as outliers resulted in a number of true contact pressure readings (non-outliers) being incorrectly classified as extrinsic pressure artifacts (outliers).



(a) Original 109-2-208 Pressure Map (b) 109-2-208 Outlier Reference







(c) 109-2-208 Results (DBSCAN-1) (d) 109-2-208 Results (DBSCAN-2)



Figure 90. Clustering results for sample 109-2-208 (location-only data)

<span id="page-183-0"></span>A summary of the results obtained by using the selected clustering methods to pre-process the dynamic data subset can be seen in [Table 27.](#page-183-1) Results of the performances and accuracies of these clustering method are generally high, with average Outliers and average Non-Outliers accuracies greater than 90% for any of methods. Results also show tradeoffs between these accuracies, with some methods being more aggressive in classifying pressure readings as outliers, while others exhibiting a more conservative approach when marking outliers.

Method		Input	Average (Min) Accuracy	Avg.		
	Parameters		<b>Outliers</b>	Non-Outliers	Overall	(Max) Proc Time
DBSCAN-1	eps: $1.60$ min_samples: 8	Location	100\% $(100\%)$	99.431% (96.918%)	99.440\% (96.959%)	3.285ms (15.991ms)
<b>DENCLUE-1</b>	eps: $2$ min_density: 1.7e-03	Location	95.035% (71.429%)	100\% $(100\%)$	99.914% $(99.379\%)$	8.597s (11.764s)
DBSCAN-2	eps: $2.00$ min_samples: 10	Location	100\% $(100\%)$	99.909% (99.315%)	99.910\% $(99.324\%)$	2.895 <sub>ms</sub> (7.995ms)
<b>DENCLUE-2</b>	eps: $0.01$ min density: $1.65e-03$	Location	92.900% (71.429%)	100\% $(100\%)$	99.879% (99.379%)	8.493s (10.370s)
DBSCAN-3	eps: $2.5$ min_samples: 10	Location	92.298% (71.429%)	99.999% (99.685%)	99.866% (99.379%)	2.870 <sub>ms</sub> (4.997ms)

<span id="page-183-1"></span>Table 27. Dynamic data subset clustering methods results of accuracies and processing times

Results from [Table 27](#page-183-1) show that only DBSCAN-1 and DBSCAN-2 were able to correctly classify all extrinsic pressure artifacts as outliers, however, they also show the lowest Non-Outlier average accuracies among the clustering methods' results. This indicate that these variations of DBSCAN favor a more aggressive approach when detecting outliers, by incorrectly classifying true contact pressure readings as outliers. It is important to note that, in spite of having the lowest non-outlier accuracies among the clustering methods, average non-outlier accuracies are above 99% for any of the selected methods. Results from the table also show that both clustering methods using DENCLUE algorithms were able classify all true contact pressure readings as non-outliers, indicating a more conservative approach when marking pressure readings as outliers.

A good balance between average Outliers and Non-Outliers accuracies were obtained by most of the clustering methods being evaluated, with two clustering methods excelling over the others. Clustering results [\(Table 27\)](#page-183-1) show DENCLUE-1 having an average Overall accuracy of 99.914% which resulted from a very high average Outliers accuracy score (95.04%) and a perfect Non-Outliers accuracy score (100%) in all pressure maps, and DBSCAN-2 having an average Overall accuracy of 99.910% which resulted from with a very high average Non-Outliers accuracy score (99.91%) and a perfect Outliers accuracy score (100%) in all pressure maps.

While all clustering methods were found to be adequate for pre-processing the pressure maps included in the dynamic data subset, this case study selected DENCLUE-1 due to having a slight edge in the Overall accuracy score and also for being able to keep all true contact pressure readings for subsequent analyses. Unfortunately, the non-optimized python package use in this study (Mgarrett, 2017, n. DENCLUE 2.0) resulted in very high computational demands while processing all samples in the dynamic data subset (see [Table 27\)](#page-183-1).

The average processing time when using DENCLUE-1 was around 8.6 seconds per frame on average, and the total processing time required to pre-process all 281 individual pressure maps was around 40 minutes. In contrast, the processing times obtained from any of the DBSCAN algorithms, implemented from a fully-optimized python package, were around 3 milliseconds per frame on average, with the total time required to pre-process all 281 individual pressure maps being less than 1 second. These drastic differences in the processing times between these clustering methods can be attributed to many factors (e.g., programming optimizations, multiprocessing capabilities, and/or clustering algorithm complexities), and need to be considered for real-life applications. Fully optimized DBSCAN algorithms are available in many commercially available packages and programming languages, and they generally achieve very good results when using seating pressure maps (see [Table 27\)](#page-183-1). As an example, DBSCAN-3 clustering was still able to achieve very high Non-Ouliers accuracies (average of 99.999%) and reasonable Outliers accuracies (average of 92.298%) while still required less than a second; this could be an alternative method to DENCLUE algorithms if preservation of the true contact pressure readings is of utmost importance.

For the purpose of this study, the algorithm's performance in classifying outliers and nonoutliers outweighs their required computation time, therefore, the density-based clustering algorithm DENCLUE-1 is used as the pre-processing technique applied to the dynamic data subset due to the high overall accuracies obtained while cleaning the pressure map images included in the dataset. The (pre-processed) dynamic data subset is now ready for subsequent analyses using measures of spatial autocorrelation, image statistical features, and comparative techniques using image registration and similarity/dissimilarity coefficients.

## **Dynamic Measures: Spatial Autocorrelation and Image Statistical Features**

Meaningful pressure measures featured in [Table 23](#page-141-0) (Chapter 5) were calculated and evaluated in terms of their practicality and feasibility as measures of dynamic pressure using the pre-processed dynamic data subset. Validation of their use as dynamic measures was done via visual feedback of time series plots. Emphasis is given in selecting and evaluating a sequence of indexes where significant changes in these measures occur in a short period of time. Comparative visual feedback between pressure maps within a sequence of indexes is used to confirm in-chairmovements (i.e., dynamic sitting), while evaluating measures' sensitivities and changes over time.

Figure [91](#page-186-0) shows the time series plots for the general pressure measures of Contact Cells, Sum of Pressure, and Skewness for the full 5-minute interval length of this sample (281 indexes).



<span id="page-186-0"></span>Figure 91. Pressure measures: general overview, dynamic data subset (sample 109-2)

Results in Figure [91](#page-186-0) show a consistent increase in Sum of Pressure during the first minutes of the sitting interval (approximately 2.5 min), indicating a possible pressure creep effect. It also shows that the number of contact cells increased slightly in the same period of time. The pressure creep effect was confirmed via visual feedback, where pressure readings in the ischial tuberosities were consistently increasing over time. This increase in pressure and somewhat stability in contact cells is also being detected by the skewness measure. The skewness is decreasing over time within the same time frame due the increase in the relative frequency of cells with high-pressure and midpressure values.

At around index 150, considerable changes in the values across all measures are also seen in the time series plots in Figure [91,](#page-186-0) possibly indicating an In-Chair-Movement (ICM). These measures are also identifying possible ICMs (i.e., dynamic sitting) occurring around indexes 200 and 250; with measures of skewness also identifying continuous changes in the pressure between indexes 180 and 200 that other measures are less sensitive to it.

Figure [92](#page-188-0) shows a sequence of pressure maps between indexes 148 and 156 (elapsed time of approximately 8 seconds) where the first considerable changes in the values of the general pressure measures are seen. The sequences of indexes presented in this case study generally show a pre-movement pressure map (with relative pre-movement stability) and a post-movement pressure map (with relative post-movement stability). The figure also show values and trendlines for all meaningful pressure measures featured in [Table 23](#page-141-0) (Chapter 5) along a comparison between the pre-movement index (148) and post-movement index (156) as relative changes in percentage (%) across these measures.

A significant reduction of the overall pressure can be seen in the sequence of indexes shown in Figure [92.](#page-188-0) The magnitudes and cluster sizes of the high-pressure regions exerted by the ischial



<span id="page-188-0"></span>Figure 92. Changes in pressure measures between indexes 148 and 156 (sample interval 109-2)

tuberosities, along with the pressure in the buttock regions, have decreased in the latter frames. A slight increase in the pressure map size is also seen post-movement, with the number of contact cells increasing by around 5%. This decrease in the overall pressure and increase in contact cells also affect the skewness measure considerably. A larger relative presence of low and low-mid pressure reading values are seen within the post-movement pressure map (109-2-156), this being indicated as a relative increase of the skewness value of around 50%.

Figure [92](#page-188-0) also shows a considerable higher contrast is pre-movement frames, mainly due to the presence of larger high-pressure clusters under the ischial tuberosities and increased pressure in buttocks region, with both Gradient Contrast and Gradient Means measures indicating so. Note that the Coefficient of Variation (CV) measure, while changing its values in the within-movement frames, does not show any significant difference between the pre-movement pressure map (Index 148) and post-movement pressure map (Index 156) with a 0.07% relative difference.

An increase in pressure homogeneity is also obtained after the ICM in Figure [92.](#page-188-0) Measures of Gradient Second Moment and Homogeneity (Y) show considerable increases in their values, generally indicating a seating pressure map with more congruent pressure readings and with smoother pressure transitions (e.g., less pronounced gradients) between pressure levels.

Time series plots shown in Figure [93](#page-190-0) are of measures of spatial relationship for the 5 minute interval length included in the dynamic data subset. The effect of pressure creep around the ischial tuberosities can also be seen for measures of spatial relationship, as they increase consistently over time until the first considerable ICM (Index 148) occurs. Spatial relationship measures, just like general pressure measures (Fig. [91\)](#page-186-0), are also able to capture dynamic sitting with considerable changes in their values occurring specially around indexes 150 and 200.

For the ICM around Index 150 (see Fig. [92\)](#page-188-0), decreases between five to ten percent are seen across the spatial relationship measures. While the pressure map obtained after the in-chairmovement is more homogeneous and with less pressure variability/contrast, the pre-movement pressure map actually exhibits pressure readings with higher spatial relationship. This premovement map (Fig. [92,](#page-188-0) top left) shows a higher number of distinct cluster of various pressure levels, with similar-value pressure readings usually found in contiguity among themselves; indicating a higher spatial relationship compared to latter frames.



(a) Moran's I: Queen Weight Matrix



<span id="page-190-0"></span>Figure 93. Pressure measures: spatial relationship, dynamic data subset (sample 109-2)

Figure [94](#page-192-0) shows the time series plots for measures of pressure variability and contrast for all indexes included in the dynamic data subset. In the indexes previous to the first considerable ICM (Index 148), measures of Gradient Contrast and Gradient Mean are also constantly increasing due to the pressure creep factor around the ischial tuberosities. It has already been established, as in the case with other meaningful pressure measures, that significant changes in pressure map contrast and variability also occurred between indexes 148 and 156 mainly due to the decrease in size of the large high-pressure clusters and decrease pressure in buttocks region in the latter frames (see Fig. [92\)](#page-188-0). Additionally, measures of variability and contrast, just as many other meaningful measures, are also reacting to potential in-chair-movement around Index 200.







(b) GLD – Gradient Contrast X ( $\theta = 0^{\circ}$ ) (c) GLD – Gradient Contrast Y ( $\theta = 90^{\circ}$ )



<span id="page-192-0"></span>Figure 94. Pressure measures: variability and contrast, dynamic data subset (sample 109-2)

Figure [95](#page-193-0) shows a sequence of pressure maps between indexes 186 and 209 (elapsed time of approximately 23 seconds) where the second considerable shifts in the values of meaningful pressure measures are seen. As with similar figures, the figure also show values and trendlines for all meaningful pressure measures featured in [Table 23](#page-141-0) (Chapter 5) along with a comparison between the pre-movement index (186) and post-movement index (209) as relative changes in percentage (%) across these measures.

The sequence of seating pressure maps presented in Figure [95](#page-193-0) indicate an occurrence of In-Chair-Movement (ICM). While the total pressure (Sum of Pressure) exerted into the pressure interface stayed relatively the same before and after the ICM, significant differences on how pressure is distributed are seen. Areas under the legs show overall reductions in exerted pressure after movement (Index 209), but gains are otherwise seen in areas around the ischial tuberosities and buttock regions. These differences in relative pressure distribution are being detected by the measures of skewness, being significantly lower in the latter frames. This increase in the exerted



	<b>Type</b> <b>Pressure Measure</b>						Relative %	A FIOL
			192	201	209	<b>Trends</b>	(186 vs 209)	$(186 \text{ vs } 209)$
General	<b>Contact Cells</b>	371	340	329	330		$-11.05%$	
	Sum of Pressure			15,484.79 14,513.51 13,591.37 15,460.33			$-0.16%$	
	Skewness	3.1429	0.9690	2.0989	2.4634		$-21.62%$	
Spatial	Moran's $I(Q)$	0.7772	0.8157	0.8105	0.8152		4.89%	
	<b>GLSD</b> - Correlation X	0.6949	0.6040	0.6984	0.7613		9.55%	
	<b>GLSD - Correlation Y</b>	0.7652	0.7353	0.7830	0.8181		6.91%	
Variability	Coefficient of Variation	1.0694	0.6956	0.9835	1.2253		14.58%	
	<b>GLD</b> - Gradient Contrast X	1,258.43	693.75	1,009.55	1,660.92		31.98%	
	<b>GLD</b> - Gradient Contrast Y	946.23	444.73	712.54	1,237.05		30.73%	
	<b>GLD - Gradient Mean X</b>	21.47	20.34	21.47	23.50		9.44%	
	<b>GLD</b> - Gradient Mean Y	16.45	15.04	16.42	18.79		14.20%	
Texture	<b>GLD - Gradient Second Moment X</b>	0.0282	0.0258	0.0266	0.0313		11.23%	
	<b>GLD - Gradient Second Moment Y</b>	0.0429	0.0345	0.0371	0.0441		3.02%	
	GLSD - Homogeneity X	0.0673	0.0432	0.0452	0.0972		44.47%	
	<b>GLSD - Homogeneity Y</b>	0.1238	0.0782	0.0867	0.1166		$-5.78%$	

<span id="page-193-0"></span>Figure 95. Changes in pressure measures between indexes 186 and 209 (sample interval 109-2)

pressure around the ischial tuberosities and buttock regions are also affecting the values of measures of contrast and variability during and after the in-chair-movement, with measures of Gradient Contrast, Gradient Mean, and Coefficient of Variation being considerably higher in the latter frames.

The changes in the pressure distributions between the pre-movement pressure map (Index 186) and post-movement pressure map (Index 209) in Figure [95](#page-193-0) have also significantly affected measures of texture and smoothness. There is a considerable increase in the uniformity of the pressure readings at the post-movement seating pressure map (Fig. [95,](#page-193-0) bottom right), which is translated as an increase in measures of Gradient Second Moment and Homogeneity (X). This increase in post-movement homogeneity is also strengthened by the higher spatial relationship seen among the pressure readings within various levels of pressure, with the late frame (Index 209) showing less variability within these clusters of pressure levels and increase contiguity between similar-value pressure readings. Moran's I and the GLSD Correlation measures are detecting this increase in the spatial relationships among similar-value pressure readings.

Figure [96](#page-195-0) shows the time series plots for the measures of texture, smoothness, and homogeneity for all indexes included in the dynamic data subset. The changes in smoothness (e.g., less texture) and homogeneity occurring during the in-chair-movement around Index 200 (Fig. [95\)](#page-193-0) were the highest relative changes among sequential indexes in the dynamic data subset.

In the indexes previous to the first considerable ICM (Index 148), measures of Gradient Second Moment (GLD) are decreasing over time due to the pressure creep factor in the ischial tuberosities and buttock regions. Gradient Second Moment measures are known to be sensitive to changes in pressure levels and gradients when measuring smoothness and texture, while measures of Homogeneity are somewhat more robust to these pressure variations and have more emphasis

in measuring the similarities of the pressure readings within various pressure levels. Measures of Homogeneity show more stability in their values for the indexes prior to the first considerable ICM (Index 148). This indicate that, while the total pressure exerted to the pressure interface is increasing over this period of time, the homogeneity within the pressure cluster levels is relatively stable, that is, the contiguity and grouping aspect of similar-value pressure readings are relatively similar across these indexes.



<span id="page-195-1"></span><span id="page-195-0"></span>Figure 96. Smoothness and texture pressure measures (sample interval 109-2)

Most meaningful measures are also detecting a possible in-chair-movement around Index 250 (see Figs. [91,](#page-186-0) [93,](#page-190-0) [94,](#page-192-0) [96\)](#page-195-0). In most of these time series plots, a defined spike in their values

(upward or downward) is generally seen, with most of the measures' values returning close to they were before the movement (spike) occurred.

Figure [97](#page-197-0) shows the sequence of pressure maps between indexes 246 and 252 (elapsed time of approximately 6 seconds) where the last considerable changes in the values of the meaningful pressure measures are seen. These measures are mostly reacting to a side-to-side inchair-movement as detected from the seating pressure maps presented in Figure [97.](#page-197-0) Pressure is seen tilting, particularly around the ischial tuberosities and buttock regions, from one side to the other within this time interval. Some changes in meaningful pressure measures' values are seen in the resulting post-movement seating pressure map (Index 252). While all meaningful pressure measures are changing and reacting to the in-chair-movement between these indexes accordingly, the post-movement seating pressure map (Index 252), contrary to previously detected in-chairmovements, does not show large differences to the pre-movement (Index 246) seating pressure map; this is in agreement to the spikes seen in the time series plots where values of the meaningful pressure measures are somewhat returning back to pre-movement values (see Figs. [91,](#page-186-0) [93,](#page-190-0) [94,](#page-192-0) [96\)](#page-195-0).

The post-movement seating pressure map in Figure [97](#page-197-0) (bottom, right) does show some slight differences when compared to the pre-movement seating pressure map (top, left). The total pressure exerted to the pressure interface is reduced, particularly around the buttocks area. This modifies the values of skewness (more positive due to higher frequency of relatively low- and midlow pressure readings) and variability/contrast measures (less pressure in the buttock regions and tuberosities). The spatial relationships are not significantly different between these maps (Index 246 vs Index 252), but a slightly higher homogeneity is obtained in the late frames due to a reduction of the gradients between pressure levels.

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	<b>Pressure Measure</b>	Index				<b>Trends</b>	<b>Relative %</b>	∆ Plot
<b>Type</b>		246	247	248	252			(246 vs 252)   (246 vs 252)
General	<b>Contact Cells</b>	341	323	318	328		$-3.81%$	
	Sum of Pressure		17,445.56 13,387.17		14, 153.42   14, 469.36		$-17.06%$	
	<b>Skewness</b>	2.2049	2.1037	2.3669	2.6441		19.92%	
Spatial	Moran's I (Q)	0.8278	0.8292	0.8099	0.8051		$-2.75%$	
	<b>GLSD</b> - Correlation X	0.7664	0.7161	0.7246	0.7578		$-1.11%$	
	<b>GLSD</b> - Correlation Y	0.8351	0.8053	0.8171	0.8124		$-2.72%$	
Variability	Coefficient of Variation	1.1955	1.0379	1.1863	1.2696		6.20%	
	<b>GLD</b> - Gradient Contrast X	1,817.41	1,073.85	1,591.88	1,597.69		$-12.09%$	
	<b>GLD - Gradient Contrast Y</b>	1,262.39	718.35	1,030.86	1,209.40		$-4.20%$	
	<b>GLD</b> - Gradient Mean X	25.47	21.44	25.35	22.78		$-10.55%$	
	<b>GLD</b> - Gradient Mean Y	19.81	16.34	19.11	17.71		$-10.62%$	
Texture	<b>GLD - Gradient Second Moment X</b>	0.0291	0.0269	0.0248	0.0321		10.34%	
	<b>GLD - Gradient Second Moment Y</b>	0.0412	0.0384	0.0350	0.0498		20.68%	
	<b>GLSD - Homogeneity X</b>	0.0902	0.0556	0.0547	0.0979		8.52%	
	GLSD - Homogeneity Y	0.1386	0.1035	0.0835	0.1473		6.28%	

<span id="page-197-0"></span>Figure 97. Changes in pressure measures between indexes 246 and 252 (sample interval 109-2)

When calculating measures of Gray-Level Differences (GLD) and Gray-Level Spatial-Dependence (GLSD), a significance effect in measures' values when considering a different axis direction is seen for the time series plots in Figures [93,](#page-190-0) [94,](#page-192-0) and [96.](#page-195-0) GLD measures of Gradient Contrast and Gradient Mean are identifying higher variabilities when measured in the horizontal or lateral direction ( $\theta = 0^{\circ}$ , X) (see Fig. [94\)](#page-192-0), while GLSD measures of Correlation, Gradient Second Moment, and Homogeneity show higher values when measured in the vertical or anteriorposterior direction ( $\theta = 90^{\circ}$ , Y) (see Figs. [93,](#page-190-0) [96\)](#page-195-1).

While the direction when calculating pressure map gradients have significant effects in GLD and GLSD measures, there is a strong dynamic relationship between both directions ( $\theta = 0^{\circ}$ ) and  $\theta = 90^{\circ}$ ) among the indexes included in the dynamic data subset. The dynamic behavior of GLD and GLSD measures are very similar in both directions with the most notable difference being in significant offsets in the measures' values between both directions ( $\theta = 0^{\circ}$  and  $\theta = 90^{\circ}$ ). Figure [98](#page-199-0) shows the pressure map for the first index of the 5-minute sitting interval (Sample 109- 2-1), along with the first-order and second-order gradient maps for the same sample. Seating pressure maps usually have an elongated shape towards the anterior-posterior direction ( $\theta = 90^{\circ}$ ) due to the fact that buttock-popliteal lengths are generally greater than hip breadths (see [Table 3\)](#page-45-0).

First-order and second-order gradient maps in Figure [98](#page-199-0) also show how seating pressure maps generally exhibit higher pressure gradients in the lateral direction ( $\theta = 0^{\circ}$ ) due to closeness of high-pressure clusters (e.g., ischial tuberosities) to lateral edges. When measured in the anteriorposterior direction ( $\theta = 90^{\circ}$ ), pressure transitions are smoother and with less gradients as pressure in the leg regions increase gradually when approximating to high-pressure clusters in the tuberosities. This is translated as an increase in homogeneity, smoothness, and spatial relationship when measured in the anterior-posterior direction ( $\theta = 90^{\circ}$ ) (see Fig. [98,](#page-199-0) bottom right).



DCLNP-1 | 109-2-1, Seatpan First Order Absolute Gradient Map (mmHg)



DCLNP-1 | 109-2-1, Seatpan Second Order Central Gradient Map (mmHg)



<span id="page-199-0"></span>Figure 98. First-order and second-order gradient maps, directions  $\theta = 0^{\circ}$ , 90° (sample 109-2-1)

In this section, many examples of the potential use of spatial relationship measures and image statistical features as dynamic pressure measures are shown. It has been shown that these meaningful pressure measures can be used as global pressure map descriptors in a static environment (within a single pressure map) and dynamic environments (continuous pressure maps) to measure distinct and unique phenomena within seating pressure maps.

While spatial relationship measures and image statistical features can help in identifying in-chair-movements, these measures are not able to track changes in terms of shape, location and/or spatial position of pressure readings. To evaluate these changes, continuous comparative techniques using image registration and dynamic similarity/dissimilarity coefficients are implemented and studied in the following section.

## **Sequential Image Registration and Similarity/Dissimilarity Coefficients**

In this case study, a sequential image registration technique (using minimization of the Mean Squared Errors [MSE]) is evaluated as a tool to align the dynamic pressure map images included in the dynamic data subset. Given the results of the image registration methods in the previous chapter (Chapter 5), MSE registration was chosen due to the higher accuracy and improved image correspondence achieved when aligning various seating pressure map images. Similarity and dissimilarity coefficients are also evaluated as comparative dynamic measures for post-registered continuous pressure maps. Comparisons to the initial reference index (Index 1) are used as a way of measuring continuous pressure map changes over time.

Figure [99](#page-201-0) shows the reference pressure map that will be used as a comparison basis (sample 109-2-1). A visual feedback assessment of the pressure maps following this first frame confirmed the use of sample 109-2-1 to be an appropriate basis for comparison. The pressure map images

following sample 109-2-1 showed relative stability in the pressure distributions and locations of pressure readings when compared to the first sampled index.



Image Registration: 109-2-1

Figure 99. Image registration reference map (Sample 109-2-1)

<span id="page-201-0"></span>MSE registrations were completed to align all indexes in the dynamic dataset to the reference index (Fig. [99\)](#page-201-0). Similarity and dissimilarity coefficients were calculated using a nonmasked approach (unbalanced pairwise pressure cells are allowed) with an epsilon parameter equal to one ( $\varepsilon = 1$ ) for ratio-based measures. The non-masked approach was used in this case study as the goal is to measure all true differences between the initial sitting pressure map and consecutive pressure map images. Results of the similarities and dissimilarities coefficients of the postregistration comparisons are shown in [Appendix R](#page-349-0)

As the indexes included in the dynamic data subset were sampled from an interval where the subject used a fixed sitting surface (i.e., same seat pan contour), similarities and dissimilarities coefficients were expected to indicate a high correspondence between the successive pressure map images and the initial pressure map image (Index 1). It was expected that the overall shapes and sizes of the continuous pressure maps to not be significantly different from one another unless significant In-Chair-Movements (ICM) occurred. Results in general show high correspondence between the pressure map images following the reference frame (Index 1). Figure [100](#page-202-0) shows time series plots of the similarity measures (compared to the reference pressure map) for all indexes in the dynamic data subset.



<span id="page-202-0"></span>Figure 100. Similarity coefficients (non-masked): MSE registration (sample interval 109-2)

Values of Pearson Correlation Coefficient (PCC) show relative stability in the similarities of images between Index 1 and Index 149 (see Fig. [100\)](#page-202-0), a behavior somewhat similar to measures of GSLD Homogeneity during this same interval (see Fig. [96\)](#page-195-1). Other similarity measures are indicating a decrease in the similarities of successive pressure maps when compared to the initial seating pressure map. Measures of Tanimoto and Minimum Ratio are more sensitive to the pressure differences in pair-wise pressure readings when comparing seating pressure map images. This decrease in similarities throughout Index 1 and Index 149 is due to the pressure creep phenomenon found when evaluating measures of Sum of Pressure (see Fig. [91\)](#page-186-0) and contrast measures (see Fig. [94\)](#page-192-0). The Minimum Ratio measure is more sensible to the increase in pressure seen in some of the pairwise readings (the ratio is lower when greater differences are found). Meanwhile, the Tanimoto measures consider these pressure differences as well, but also considers their relationships (similar to Pearson), making the values of Tanimoto similarities somewhere in between the PCC and Minimum Ratio values.

Measures of dissimilarity are also reacting to the pressure creep phenomenon occurring between indexes 1 and 149. Figure [101](#page-203-0) shows time series plots of the dissimilarity measures (compared to the reference pressure map) for all indexes in the dynamic data subset.



<span id="page-203-0"></span>Figure 101. Dissimilarity coefficients (non-masked): MSE registration (sample interval 109-2)

The results in Figure [101](#page-203-0) show measures of  $L_1$  Norm and Squared  $L_2$  Norm increasing in their dissimilarity values due to differences in pressure between the initial reference index (Index 1) and successive indexes before index 150. Similar to Tanimoto and Minimum Ratio measures, this behavior is due to the pressure creep phenomenon during this time frame. To evaluate the pressure creep effect, the registration results between the initial frame (Index 1) and Index 149 (before the first considerable in-chair-movement) are presented in Figur[e 102,](#page-204-0) along with measures of similarity/dissimilarity and a visual highlights of pressure differences between these images.



Image Registration: 109-2-1 vs 109-2-149, Scaling Factor: 10

MSE Image Registration: 109-2-1 vs 109-2-149, Iteration 13 Metric: 262.92266118599525





<span id="page-204-0"></span>Figure 102. Optimal MSE image registration: Index 1 vs Index 149 (sample interval 109-2)

MSE registration achieved appropriate alignments and image correspondence between the seating pressure maps presented in Figure [102.](#page-204-0) The pressure distributions in terms of location and spatial relationship of pressure readings are similar, but the magnitudes of the pressure readings at Index 149 are considerable increased (see Fig. [102](#page-204-0) bottom right). Larger high-pressure clusters are seen under the ischial tuberosities in the latter frame, with higher pressures also being exerted in the top buttock regions. Given these pressure differences, a decrease (increase) in pressure map similarities (dissimilarities) are seen by the Tanimoto, Minimum Ratio,  $L_1$  Norm and Squared  $L_2$ Norm measures; all being sensitive to those pairwise differences in pressure. Measures such as Pearson, not being sensitive to differences in pressure scale, finds the relationship among pressure maps somewhat similar (non-masked  $r = 0.977$ ) The Intensity Ratio Variance also show low dissimilarities between these maps due to the robustness of this measure to pressure scaling differences (non-masked  $R_V = 0.018$ ). Intensity Ratio Variance is more sensitive to overlapping differences in terms of shapes (when using the non-masked approach). The overall shapes of these pressure maps from Index 1 to Index 149 were very consistent and similar (see Fig. [102,](#page-204-0) top row).

Another important measure obtained when using sequential image registration procedures (i.e., alignment of continuous images) is the distance traveled by the center of mass [Center of Pressure (CP)] of the template image (i.e. moving image) to reach registration optimality. The template pressure maps (i.e. moving maps) were all registered according to the initial reference pressure map (i.e. fixed map). The translation required to align these pressure map images to the reference map can be calculated as the distance traveled by the center of pressure during registration. A CP to CP distance is calculated as the Euclidean distance between the CP locations of the of the pre-registered map and post-registered map. Note that this distance between CP locations are not calculating differences in the CP locations between the template map and

reference maps, but the translation of CP within the template map after registration. Figure [103](#page-206-0) shows the CP translation results of the registration process for aligning each subsequent pressure map to the reference map (Index 1).



<span id="page-206-0"></span>Figure 103. Original vs Transformed CP locations: Cells distances (sample interval 109-2)

The required translations to align the pressure maps from index 1 through 149 were minimum, with most registrations doing CP translations of less than 1 cell (see Fig. [103\)](#page-206-0). It is important to emphasize that pressure maps were scaled by a factor of ten to allow fine-tuning transformations during registrations. Therefore, the resulting CP to CP distances (in units of cells) presented in Figure [103](#page-206-0) are also in factor of ten. To obtain real distances (in units of cells) between the original and transformed CP locations, the cell distances need to be divided by 10. It is also important to highlight that meaningful differences in CP movement were considered when translations of CP were greater than one inch  $(CP > 1 \text{ in})$ ; one inch being the approximate

distance required to travel one unit of cell. Hence, a distance of 10 cells in the current scale of CP to CP distances roughly equates to a 1-inch movement in CP location. Figure [103](#page-206-0) only show one instance (Index 192) where a translation greater than 1 inch (10 upscaled cells) was needed to align the template pressure map to the reference pressure map, indicating that the subject was sitting in a relative stable location throughout the entire 5-minute sitting interval.

Time series plots in Figures [100,](#page-202-0) [101](#page-203-0) and [103](#page-206-0) also show highlights of index ranges where possible in-chair-movement is detected. The first region shows a considerable shift in values of similarities and dissimilarities between indexes 149 and 159. Figure [104](#page-207-0) shows a close examination of the similarity measures for this range of indexes. This figure shows that similarity measures had a considerable decrease in Index 152 during an in-chair-movement. This same inchair-movement was also detected using values of meaningful pressure measures as dynamic pressure measures (see Fig. [92\)](#page-188-0).

<span id="page-207-0"></span>

<span id="page-207-1"></span>Figure 104. Similarity coefficients highlights: MSE registration (sample interval 109-2)

To evaluate the pressure map differences during the first considerable in-chair-movement, the registration results between the initial frame (Index 1) and Index 152 are presented in Figure [105,](#page-208-0) with measures of similarity/dissimilarity and a visual highlights of pressure differences between these images also being presented.



Image Registration: 109-2-1 vs 109-2-152, Scaling Factor: 10







<span id="page-208-0"></span>Figure 105. Optimal MSE image registration: Index 1 vs Index 152 (sample interval 109-2)

Figure [105](#page-208-0) shows considerable changes in pressure distributions at index 152 when compared to the initial seating pressure map. The reference index (109-2-1) shows a distinct

presence of high-pressure clusters under the ischial tuberosities while the pressure map in index 152 shows higher pressure being exerted under the leg regions (see Fig. [105,](#page-208-0) bottom right). These pressure differences are still being accounted by the Tanimoto, Minimum Ratio,  $L_1$  Norm and Squared  $L_2$  Norm similarity and dissimilarity measures, but now measures of Pearson Correlation Coefficient (PCC) and Intensity Ratio Variance are also indicating considerable changes. A decrease in non-masked PCC similarity is now seen from 0.977 in the pre-movement index 149 to 0.884 during the in-chair-movement at index 152 (see Figs. [102,](#page-204-0) [105\)](#page-208-0). Likewise, the non-masked Intensity Ratio Variance dissimilarity measures increased from 0.018 in pre-movement index 149 to 0.147 during the in-chair-movement at index 152 (see Figs. [102,](#page-204-0) [105\)](#page-208-0). These changes in these two similarity/dissimilarity measures are due to significant differences in pressure distributions (e.g., pressure under ischial tuberosities) and differences in shape (e.g., no overlaps or intersections between pressure readings in the top left leg region).

Other possible in-chair-movements are detected within the highlighted regions of interest shown in Figures [100,](#page-202-0) [101](#page-203-0) and [103.](#page-206-0) The second region of interest show a number of possible inchair-movement between indexes 180 and 217. A close examination of the similarity measures for this range of indexes is also shown in Figure [104.](#page-207-0) The first index to be evaluated for this region is Index 192, where considerable decreases in similarities are seen during the in-chair-movements. This same in-chair-movement was also detected using values of meaningful pressure measures as dynamic pressure measures (see Fig. [95\)](#page-193-0).

Figure [106](#page-210-0) shows the registration results between the initial frame (Index 1) and Index 192, along with measures of similarity/dissimilarity and visual highlights of pressure differences between these images. Pronounced pressure differences are now seen between the reference map and Index 192 when compared to differences between the reference map and Index 152 (Fig. [105\)](#page-208-0).



Image Registration: 109-2-1 vs 109-2-192, Scaling Factor: 10

<span id="page-210-0"></span>Figure 106. Optimal MSE image registration: Index 1 vs Index 192 (sample interval 109-2)

100

 $\Omega$ 

200

300

300

200

100

0

Differences in the pressure distributions between Index 192 and the reference map (Index 1) are seen in the high-pressure cluster under the ischial tuberosities and higher-pressure values around the buttocks area in the reference map, while the pressure map in Index 192 shows more pressure in both leg regions (see Fig. [106,](#page-210-0) bottom right). According to similarity values, these pronounced differences are the highest seen among compared indexes (see Fig. [104\)](#page-207-1). A close examination of the dissimilarity measures for this range of indexes, seen in Figure [107,](#page-211-0) also shows that Index 192 is where the highest dissimilarities are obtained according to most of the measures.



<span id="page-211-0"></span>Figure 107. Dissimilarity coefficients highlights: MSE registration (sample interval 109-2)

Index 192 is also where the distance traveled by the Center of Pressure (CP) is the largest (13.24 cells) among the translations needed to reach registration optimality across all indexes (see Fig. [103\)](#page-206-0). The registered pressure map overlays in Figure [106](#page-210-0) (bottom left) shows how the template image (Index 192) had to be slightly moved down in the Y-axis (anterior-posterior direction) to have a better match of the pressure map shape and correspondence of the locations of high-pressure within each map.

In addition, a significant number of potentials in-chair-movements are also seen within the second region of interest (indexes 180 and 217). Figures [104](#page-207-0) and [107](#page-211-0) show close examination of the similarity and dissimilarity measures for this range of indexes respectively, where differences in the behavior or sensitivities between similarity/dissimilarity measures are seen between indexes 196 and 200. Measures such as Pearson, Tanimoto, and Squared  $L_2$  Norm show higher (lower) similarity (disimilarity) between Index 200 and the reference index, than the ones obtained when

comparing Index 196 to the reference index. Other measures such as  $L_1$  Norm and Minimum Ratio show opposite results, by detecting higher (lower) similarity (disimilarity) between Index 196 and the reference index than the ones obtained when comparing Index 200 to the reference index. To evaluate these discrepancies between similarity and dissimilarity measures, the registration results between the initial frame (Index 1) and Index 196, and between the initial frame (Index 1) and Index 200 are presented in Figures [108](#page-212-0) and [109](#page-213-0) respectively. Measures of similarity/dissimilarity and visual highlights of pressure differences between images are also presented in these figures.



Image Registration: 109-2-1 vs 109-2-196, Scaling Factor: 10

MSE Image Registration: 109-2-1 vs 109-2-196, Iteration 19 Metric: 412.77150687357937





<span id="page-212-0"></span>Figure 108. Optimal MSE image registration: Index 1 vs Index 196 (sample interval 109-2)



Image Registration: 109-2-1 vs 109-2-200, Scaling Factor: 10

<span id="page-213-0"></span>Figure 109. Optimal MSE image registration: Index 1 vs Index 200 (sample interval 109-2)

Differences between the reference index (Index 1) and Index 196 show lower differences in pairwise pressure readings than the ones between the reference index (Index 1) and Index 200 (see Figs. [108,](#page-212-0) [109,](#page-213-0) bottom right). The lower overall differences in pressure among the pairwise pressure readings seen when registering Index 196 (Fig. [108\)](#page-212-0), compared to the ones obtained when registering Index 200 (Fig. [109\)](#page-213-0), are being detected by measures of  $L_1$  Norm and Minimum Ratio. Values of non-masked  $L_1$  Norm and Minimum Ratio are at 6,788.77 mmHg and 0.613 respectively

when registering Index 196, compared to values of 8,190.81 mmHg and 0.544 respectively when registering Index 200.

While lower overall pressure differences  $(L_1)$  Norm values) are obtained when registering Index 196, compared to the ones obtained when registering Index 200, the differences in pressure in specific regions are greater when registering Index 196. The map of pressure differences seen in Figure [108](#page-212-0) (bottom right) shows higher pressure differences around the ischial tuberosities (differences between 200-250 mmHg between pairwise cells), compared to map of pressure differences seen in Figure [109](#page-213-0) (bottom right) where the pressure differences around the ischial tuberosities are lower (differences between 150-175 mmHg between pairwise cells). These large pairwise pressure differences seen when registering Index 196 (Fig. [108\)](#page-212-0) affects the measures of Pearson, Tanimoto, and Squared  $L_2$  Norm, with these measures agreeing that higher (lower) similarities (dissimilarities) are seen when registering Index 200, instead of 196. This is a good example of the differences and sensitivities of various similarity and dissimilarity coefficients.

Compared to other similarity and dissimilarity measures, the Intensity Ratio Variance has a unique behavior and sensitivity when comparing pressure map images. The Intensity Ratio Variances do not show major significant shifts when comparing all indexes to the reference map, but spikes in their values are seen in the time series plot in Figure [101,](#page-203-0) indicating a reaction to specific differences between pressure maps.

Figure [107](#page-211-0) shows particular instances where changes in Intensity Ratio Variance values are considerable higher when compared to other similarity and dissimilarity coefficients. Indexes 203, 208, and 258 are instances where unique spikes are seen in the values of Intensity Ratio Variance. Other similarity and dissimilarity coefficients do not react in a similar way when these indexes are compared, suggesting that Intensity Ratio Variance measures are sensitive to specific differences between pressure maps. To evaluate the uniqueness of the Intensity Ratio Variance measure, the registration results and similarity and dissimilarity coefficients obtained when comparing these indexes [203, 208, and 258] to the reference maps are presented in Figure [110.](#page-215-0)



300

(c) 109-2-1 vs 109-2-258

 $100$ 

 $\Omega$ 

<span id="page-215-0"></span>Figure 110. Optimal MSE image registration: Indexes 203, 208, and 258 (sample interval 109-2)

200

 $300$ 

Figure [110a](#page-215-0) shows the results when comparing Index 203 to the reference map. For this particular index, all similarity and dissimilarity coefficients detect considerable differences between the maps (e.g., non-masked Pearson Correlation Coefficient  $= 0.861$ ), but measures of Intensity Ratio Variance show a considerable change when compared to results from other indexes. As an indicator, 92.88% of compared indexes show values of non-masked Intensity Ratio Variance
less than 0.5, with the average value being 0.16; due to this, a non-masked Intensity Ratio Variance value greater than one is considered significant for this dynamic data subset sample.

In all three indexes, measures of Intensity Ratio Variance indicated considerable pressure map differences (see Fig. [107\)](#page-211-0). Index 203 (Fig. [110a](#page-215-0)) shows a significant non-masked Intensity Ratio Variance value of 1.929, while indexes 208 (Fig. [110b](#page-215-0)) and 258 (Fig. [110c](#page-215-0)) show nonmasked Intensity Ratio Variance values of 1.987 and 1.306 respectively. The high values of Intensity Ratio Variance are due to differences in the shapes between the pressure maps; considerable regions with non-overlapping pressure readings are found, particularly in the leg regions. Also note that similarity and dissimilarity coefficients other than Intensity Ratio Variance are indicating relatively high (low) similarities (dissimilarities), particularly when comparing indexes 208 and 258 (e.g., non-masked Pearson Correlation Coefficient are set at 0.980 and 0.981 respectively). The examples shown in Figure [110](#page-215-0) indicate that measures of Intensity Ratio Variance are particularly sensitive to these differences in shapes (i.e., non-overlapping pressure readings) when compared to sensitivities from other similarity and dissimilarity coefficients.

The last section in this case study is devoted to evaluating the computational demands for continuous dynamic image registration. To register all 281 indexes in the dynamic data subset, the total MSE registration process was executed in 676.33 seconds (approximately 11 minutes). Figure [111](#page-217-0) shows a histogram of the processing time for all indexes. Results show that alignment of pressure maps was done in one second or less for 66.5% of the indexes included in the dynamic data subset, with MSE registration taking longer than 5 seconds in just 10% of the indexes when aligning them to the reference map. The maximum recorded processing time for a particular index was 45 seconds (Index 256, with total of 235 iterations and optimality at iteration 13).



Figure 111. MSE image registration processing times (Sample 109-2)

<span id="page-217-0"></span>The results in this section show the potential of using similarity and dissimilarity coefficients as complementary dynamic pressure measures for identifying and evaluating in-chairmovements (ICM). Sequential image registration using MSE attained the intended results for the 5-minute sitting interval sample evaluated in this case study; proper alignments, centering, and correspondences in pressure maps' image features were achieved. While the method chosen for this case study is based on comparisons of all pressure maps to the initial reference map (Index 1), other comparison basis could have been chosen (e.g., other pressure maps index or an aggregate map) with different interpretable results.

Similarities and dissimilarities coefficients were suitable comparative techniques between post-registered pressure maps with potential uses for dynamic sitting applications. These coefficients can evaluate differences in the pressure distributions between pressure maps and be used as global comparative measures, each with a unique take, while the use of new proposed pressure measures in [Table 23](#page-141-0) (Chapter 5) can highlight the features that makes each map different.

## CHAPTER VII

## CONCLUSIONS

This work evaluated the applications of machine learning, spatial data analytics, digital image processing, and optimal image registration as new techniques for analyzing pressure maps. The applications, feasibilities, and practicalities of introduced techniques were made within the context of seating research. Results obtained in this study indicate that many of these techniques are suitable for analyzing pressure maps, with applications for pre-processing, analysis and evaluation, and comparisons of seating pressure map images. These techniques were found to also be cross-functional for applications in static (i.e., single map) and dynamic (i.e., sequential temporal maps) environments.

The research objectives were successfully fulfilled by achieving the following:

- (1) The study introduced appropriate methods for detecting and removing extrinsic pressure artifacts (i.e., pressure reading outliers), with overall accuracies over ninetynine percent (99%), by using density-based spatial clustering techniques. The feasibility and practicality of applying these techniques for cleansing continuous pressure maps (e.g., dynamic sitting) was also demonstrated.
- (2) Various pressure measures based on spatial autocorrelation and image statistical features were introduced and validated as new pressure measures. These new measures were found to be appropriate and suitable for measuring certain aspects of the pressure maps, such as specific pressure distribution patterns (e.g., homogeneity, acute points,

and low-high distributions), overall spatial relationships, and pressure contrasts that commonly used pressure measures were not able to describe due to information loss. Their values and usefulness as dynamic pressure measures were also demonstrated.

(3) A toolset for aligning and comparing pressure maps is introduced by using optimal image registration methods and similarity and dissimilarity coefficients. Accurate and appropriate alignments were obtained via image registration, particularly by using the MSE metric. The uniqueness of each similarity/dissimilarity coefficient was explained when comparing pressure patterns between pressure maps, along with demonstrating the feasibility and practicality of applying these techniques for aligning and comparing continuous pressure maps (e.g., dynamic sitting).

A summary of the results obtained in the study is presented in [Table 28.](#page-220-0) This table presents concise findings for each introduced methodology along with their applications and interpretations in the context of seating pressure mapping analysis. One major benefit in introducing these techniques is the increase in objectivity through quantitative evaluation, with no dependence of visual feedback assessments for understanding seating pressure map characteristics, features, and, particularly, dynamic behavior. The human information-processing system is overloaded by sensorial information, with constraints placed in cognitive processes such as attention, perception, recognition, judging, reasoning, and problem solving (Payne, 2003; Smith & Kelly, 2015). Such constraints make the human information-processing system prone to errors and misjudgments.

By assessing values of meaningful pressure measures and similarity/dissimilarity coefficients, particularly during dynamic evaluation of time series plots, a general idea of the seating activity and behavior of the seating pressure distributions is generally obtained without recurring to constant visual feedback – a more-demanding cognitive activity.



<span id="page-220-1"></span><span id="page-220-0"></span>Table 28. Summary of study findings, comments and conclusions Table 28. Summary of study findings, comments and conclusions

Table 28-Continued [Table 28 ̶](#page-220-1) Continued





 $\mathbf l$ 





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201

While the introduced techniques for pressure mapping analysis were evaluated in a task seating environment (i.e. mousing and typing), the applications of these methodologies, along with their use and interpretation, should be transferable to other seating research environments. For example, research in automobile seating could be enhanced by the analytical capabilities of the introduced methodologies. The automobile seating environment provides certain restrictions in terms of seating postures and movements, thus making seating pressure behavior to be generally stable. Therefore, pressure redistributions during driving activities are important indicators of sitting discomfort, and enhancements in monitoring, tracking, and analysis of seating pressure maps can help in a better understanding of these movement-discomfort relationships (Sammonds et al., 2017).

Other implementations of the introduced methodologies can be in the ergonomic evaluation of aircraft pilot seats, where factors such as inappropriate seat dimensions and improper sitting postures are possible contributors to discomfort. Pilot discomfort due to sitting conditions can lead to distractions and reduction in pilot performance during an air flight, causing concerns in flight safety (Andrade, 2013). By use of pressure mapping interfaces, the introduced techniques could help in evaluating pilot seat designs and seating postures, while helping in further understanding their relation to seating comfort-discomfort.

Another example where introduced methodologies can help expand the analytical capabilities is in paraplegic seating research, where the monitoring of pressures between the soft tissues of the body and the support surface is important in assessing tissue viability (Aissaoui et al., 2001). While body tissues can generally tolerate high pressures for short periods of time, the lack of sitting movement or pressure redistribution is of concern. Blood supply and lymphatic drainage are impaired if high seating pressures are maintained (Aissaoui et al., 2001). The

additional information provided by the introduced methodologies can help in identifying unfavorable pressure distribution patterns or stagnant sitting behavior.

In all aforementioned examples, the analysis of the relationships between user-chair interactions and seating comfort-discomfort could be expanded by the introduced pressure mapping techniques; these can help in objectively identifying the seating conditions that can lead to discomfort. While many of the findings in this study are in the context of seating pressure mapping evaluation, the applications of these techniques can also be tailored and employed in nonseating research using pressure map images (e.g., gait analysis, industrial applications, and sports fields), or for research studies using spatially related three-dimensional datasets (e.g., surface topography, contour data, and heat maps).

## **Limitations**

Some of the limitations in this study are in terms of the pressure mapping interface used to collect the pressure maps included in the studied dataset. There were instances where many pressure sensor cells in the pressure mat were maxed out (i.e., 300 mmHg), usually around highpressure regions such as the ischial tuberosities. Some of the introduced pressure measures, such as homogeneity and spatial relationships measures, were sensitive to clusters of maxed out readings. To obtained more accurate results with introduced measures, the use of pressure mapping interfaces with pressure limits higher than the expected max pressure reading is required.

Introduced methodologies were validated for a grid-base pressure mat interface with 1024 (32 x 32) contiguous pressure elements (sensors). While the applications of many of the introduced measures, techniques, and methodologies should scale well with grid-base pressure mat interfaces with different configurations (e.g., 16 x 16, or 32 x 80 [used in mattress research]), proposed techniques for data cleansing (using density-based spatial clustering) might not be adequate for other pressure mapping applications. This study implemented density-based spatial clustering on the assumption that seating pressure maps generally exhibit a single-body (or a number of large bodies) of contiguous pressure readings. This assumption could be violated in other human-subject pressure mapping applications (e.g., gait analysis, mattress mapping, or dental mapping). In controlled pressure mapping environments, particularly in industrial applications (e.g., sealing packaging, robotic assembly, and ultrasonic welding), extrinsic pressure artifacts might not even be present; making the pre-processing (data cleansing) of collected pressure maps not a requirement.

For the dynamic evaluation of continuous pressure maps, the 5-minute interval sample used in this study provided sufficient dynamic pressure redistributions to evaluate the feasibility of introduced dynamic pressure measures. Unfortunately, significant seat pan repositions did not occur during this sitting time interval. More seating repositions could potentially be observed in longer sitting sessions, where the potential use of measures of registered CP translation distances could be better evaluated. The dynamic evaluation conclusions presented in this study assume that all introduced methodologies and measures are scalable (different pressure map resolutions) and extendable (longer collection of continuous pressure maps).

Evaluations of introduced comparative techniques were limited to comparisons of pressure maps with no significant orientation differences (e.g., rotational differences of more than 90°), or significant scaling differences (e.g., differences in number of contact cells more than 20%). Significant scaling differences can occur when comparing pressure maps between subjects due to differences in subjects' anthropometry, or when comparing within-subject pressure maps where different seating surfaces are examined (e.g., different seating area and/or contour). These scaling differences can have meaningful effects during image registration procedures. While scaling algorithms can be also implemented for comparing pressure maps, it is generally not appropriate for research involving human subjects (e.g., seating research). Scaling algorithms will distort subject's anthropometry and cover dissimilarities due to true differences in size between subjects, and therefore not considered in this study. But other potential pressure mapping research applications where objects are naturally scalable (e.g., tire footprint analysis) might benefit from scaling algorithms during image registrations.

Another major limitation is that seating pressure maps were used as the testing and validation platform for introducing new methods and techniques for pressure mapping analysis. While other pressure mapping applications could benefit from many of the proposed methodologies, their applications and interpretations could possibly change according to what is being researched (human or object) and which contact interaction (surface) is being studied.

## **Future Research**

Possible avenues for future research are in terms of pre-processing (data cleansing) techniques. Additional input data can be provided to density-based clustering algorithms with the purpose of enhancing detection and classification accuracies of extrinsic pressure artifacts (outliers). One possibility could be incorporating pressure distances between individual pressure reading and the map's center of pressure (with appropriate weights) as a way to identify closeness to the main pressure body. Other techniques could include forward or backwards propagation analysis in continuous pressure maps to detect common areas and locations where outliers are detected across sequential pressure maps, or use of multi-phase algorithms (e.g., using combinations of clustering methods, pressure magnitudes, locations, and distances information) to provide outlier scores to pressure readings within a pressure map.

With the introduction of new pressure measures and comparative techniques, future studies in seating research can implement these to further study human-chair interactions. Research can be aimed at determining appropriate ranges of values for the proposed pressure measures in relation to sitting comfort-discomfort. These measures can also be used to understand subjects' anthropometry influences during extended sitting bouts, and further help in understanding the relationships to comfort-discomfort during dynamic sitting.

As one of the limitations in this study is the use of seating pressure maps as the testing and validation platform for introduced methodologies, is also of importance that applications, evaluations, feasibilities, and practicalities of proposed methodologies are studied in other pressure mapping application fields.

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Appendix A

Institutional Review Board Approval Letters

## ESTERN MICHIGAN UNIVERSI

Human Subjects Institutional Review Board

Date: May 14, 2013

Tycho Fredericks, Principal Investigator To: Steven Butt, Co-Principal Investigator James Burns, Student Investigator

From: Amy Naugle, Ph.D., Chair

Re: HSIRB Project Number 13-05-21

This letter will serve as confirmation that your research project titled "Determining Seat Pan Requirements and Interface Pressures for Self-selected Seating Comfort" has been approved under the expedited category of review by the Human Subjects Institutional Review Board. The conditions and duration of this approval are specified in the Policies of Western Michigan University. You may now begin to implement the research as described in the application.

Please note: This research may only be conducted exactly in the form it was approved. You must seek specific board approval for any changes in this project (e.g., you must request a post approval change to enroll subjects beyond the number stated in your application under "Number of subjects you want to complete the study)." Failure to obtain approval for changes will result in a protocol deviation. In addition, if there are any unanticipated adverse reactions or unanticipated events associated with the conduct of this research, you should immediately suspend the project and contact the Chair of the HSIRB for consultation.

Reapproval of the project is required if it extends beyond the termination date stated below.

The Board wishes you success in the pursuit of your research goals.

May 14, 2014 **Approval Termination:** 

> Walwood Hall, Kalamazoo, MI 49008-5456 PHONE: (269) 387-8293 FAX: (269) 387-8276

# WESTERN MICHIGAN UNIVERS



**Institutional Review Board** FWA00007042 IRB00000254

Date: July 16, 2019

To: Tycho Fredericks, Principal Investigator Steven Butt, Co-Principal Investigator Joan Martinez, Student Investigator for dissertation Student Investigators: James Burns, Megan Hammond, David Haruza, Anna Konstant, Persefoni Lauhon, Katelyn McComb, Michelle Valente

MyNaug From: Amy Naugle, Ph.D., Chair

Re: HSIRB Project Number 13-05-21

This letter will serve as confirmation that the change to your research project titled "Determining" Seat Pan Requirements and Interface Pressures for Self-selected Seating Comfort" requested in your memo received July 15, 2019 (to expand dissemination to allow data to be used for Joan Martinez's dissertation) has been approved by the Human Subjects Institutional Review Board.

The conditions and the duration of this approval are specified in the Policies of Western Michigan University.

Please note that you may only conduct this research exactly in the form it was approved. You must seek specific board approval for any changes in this project. You must also seek reapproval if the project extends beyond the termination date noted below. In addition, if there are any unanticipated adverse reactions or unanticipated events associated with the conduct of this research, you should immediately suspend the project and contact the Chair of the HSIRB for consultation.

The Board wishes you success in the pursuit of your research goals.

Approval Termination:

May 13, 2020

Office of the Vice President for Research Research Compliance Office 1903 W. Michigan Ave., Kalamazoo, MI 49008-5456 PHONE: (269) 387-8293 FAX: (269) 387-8276 WEBSITE: wmich.edu/research/compliance/hsirb

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Appendix B

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Appendix C

Python Code: Spatial Clustering Algorithms
```
\frac{1}{2}.
2^{\circ}3. Created on Thu Mar 7 09:13:08 2019
4.
5. @author: Joan Martinez
6.7. 
8. import numpy as np 
9. import pandas as pd 
10. from sklearn.cluster import DBSCAN, OPTICS 
11. from hdbscan import HDBSCAN 
12. from sklearn import metrics 
13. from sklearn.preprocessing import StandardScaler 
14. import matplotlib.pyplot as plt 
15. import sys, time, glob, os 
16. import matplotlib as mpl 
17. from skimage.external import tifffile 
18. 
19. sys.path.append(os.getcwd()+'\\DENCLUE-master') 
20. from denclue import DENCLUE # mgarrett, 2017 (github.com/mgarrett57/DENCLUE) 
21. 
22. sys.path.append(os.getcwd()+'\\py-dbclasd-master') 
23. from dbclasd2 import dbclasd # Sebastian Palacio, 2015 (github.com/spalaciob/py-dbclasd) 
24. 
25. # create colormap 
26. upper = mpl.cm.jet(np.arange(int(256/4.5),256)) 
27. cmap = mpl.colors.ListedColormap(upper, name='myColorMap', N=upper.shape[0]) 
28. 
29. ########################### LOAD DATA ############################################## 
30. 
31. sheet = 'Seatpan' 
32. 
33. # Pressure Mat Info 
34. res1 = 32 
35. res2 = 32 
36. pmax = 300 
37. 
38. Y1 = pd.read_excel('Data\\Cluster data subset.xlsx', sheet_name=sheet) 
39. Ylab = pd.read_excel('Data\\Cluster data subset.xlsx', sheet_name=sheet + ' Outliers') 
40. 
41. nindex = np.size(Y1u10c[1,:])42. 
43. Y = np.float32(Y1.values.reshape(res1,res2,nindex)) 
44. Ym = np.ma.masked where(Y == 0, Y) ## Inactive cells = 0 mmHg
45. 
46. indexlist = list(range(56)) 
47. 
48. #Setting up column/rows/pressure array 
49. X1 = np.array(np.meshgrid(np.arange(1,res1+1),np.arange(1,res2+1))).T.reshape(-1,2) 
50. X1 = pd.DataFrame(np.hstack((X1,np.zeros(res1*res2).reshape(1,1))),columns=['Row','Column'
   ,'Pressure']) 
51. 
52. #Setting up cluster label variables 
53. cluvarlist = ['db', 'dbnp', 'op', 'opnp', 'opdb', 'opdbnp', 'hdb', 'hdbnp' 
54. ,'dcl', 'dclnp', 'dbcl', 'dbclnp']
```
# -\*- coding: utf-8 -\*-

```
55. labvarlist = ['DBSCAN', 'DBSCAN (NP)', 'OPTICS_XI','OPTICS_XI (NP)', 'OPTICS_DBSCAN', 
    'OPTICS_DBSCAN (NP)', 'HDBSCAN', 'HDBSCAN (NP)', 'DENCLUE', 'DENCLUE (NP)', 'DBCLASD', 'DB
   CLASD (NP)'] 
56. props = dict(boxstyle='round', facecolor='wheat', alpha=0.3) 
57. 
58. Results = pd.DataFrame(columns=['File','Sheet','Method','Parameters','Clusters',
    'Noise Pts','Cluster Accuracy','Overall Accuracy','Outliers Accuracy',
    'Non-Outliers Accuracy', 'Homogeneity','Completeness','V-measure','Adj RI', 'Adj MI',
    'Silhouette Coefficient', 'Proc Time']) 
59.
60.
61. start = time.time()
62. ############################## START INDEXING ################################# 
63. for i in indexlist: 
64. 
65. filename = Y1.columns[i]66. os.makedirs('Data\\Cluster data subset\\' + filename, exist_ok=True) 
67. 
68. #Plot pressure map 
69. plt.figure(figsize=(5, 4), dpi=200) 
70. plt.imshow(Ym[:,:,i], cmap=cmap);
71. plt.clim(0,pmax) 
72. plt.colorbar() 
73. plt.title(f'{filename} - Pressure Map (mmHg)') 
74. plt.savefig(f'Data\Cluster data subset\{filename}\Pressure Map - {filename}.tif',
       bbox_inches='tight') 
75. plt.clf() 
76. 
77. 
78. X=X1 
79. X['Pressure'] = np.array(Y1.iloc[:, i]).reshape(-1, 1)80. labels_true = np.array(Ylab.iloc[:,i]) 
81. 
82. #Eliminating non-pressure elements 
83. X = X.drop(X[X.Pressure == 0].index)84. labels_true = np.array([labels_true[j] for j in X.index]) 
85. X = X \cdot \text{reset index}(drop=True)86. 
87. # Standardization (Z) 
88. X['Pressure'] = StandardScaler().fit_transform(X['Pressure'].values.reshape(-1,1)) 
89. 
90. ###### NO PRESSURE DATA ####### 
91. Xnp = X.drop('Pressure', axis=1)
92. Xnpreord=X[['Column','Row']]
93. 
94. #Marking all as non-outliers 
95. core_samples_mask = np.zeros(len(X.iloc[:,0]), dtype=bool)<br>96. core samples mask[:] = True
       core samples mask[:] = True
97. 
98. #Plotting Reference Outlier Map 
99. real_n_noise = list(labels_true).count(-1) 
100. real_non_outliers = list(labels_true).count(0) 
101. 
102. unique_labels = set(labels_true) 
103. colors = [plt.cm.Set3(each) 
104. for each in np.linspace(0, 1, len(unique_labels))] 
105. 
106. fig, ax = plt.subplots() 
107. pstr = ('Outliers: %i' %real_n_noise + '\nNon-Outliers: %i' %real_non_outliers)
```

```
108. ax.text(res1 + 1.5, 1, pstr, fontsize=7, verticalalignment='top', bbox=props)
109.<br>110.
          # Black removed and is used for noise instead.
111. for k, col in zip(unique_labels, colors): 
112. if k == -1: 
113. # Black used for noise.
114. col = [0, 0, 0, 1] 
115. 
116. class member mask = (labels true == k)
117. 
118. xy = X[class member mask & core samples mask]119. ax.plot(xy['Column'], xy['Row'], 'o', markerfacecolor=tuple(col), 
120. markeredgecolor='k', markersize=7) 
121. 
122. xy = X[class_member_mask & ~core_samples_mask] 
123. ax.plot(xy['Column'], xy['Row'], 'o', markerfacecolor=tuple(col),
124. markeredgecolor='k', markersize=5) 
125. 
126. plt.xticks(np.arange(0, res1+1, res1/8))<br>127. plt.vticks(np.arange(0, res1+1, res1/8))
          plt.yticks(np.arange(0, res1+1, res1/8))
128. plt.title(f'{filename} - Outliers Reference [Noise: {real_n_noise}]') 
129. ax.axis([-0.5, res1+0.5, -0.5, res2+0.5]) 
130. ax.set aspect(1)
131. ax.invert yaxis()
132. 
133. plt.savefig(f'Data\Cluster data subset\{filename}\Reference - {filename}.tif',
          dpi=200, bbox_inches='tight') 
134. plt.clf() 
135. 
136. # Compute DBSCAN
137. proctime = time.time() 
138. db = DBSCAN(eps=2.5, min_samples=8, metric='euclidean', algorithm='brute').fit(X) 
139. dbtime = time.time() - proctime 
140. 
141. proctime = time.time() 
142. dbnp = DBSCAN(eps=2.2, min samples=10, metric='euclidean',
           algorithm='brute').fit(Xnp) 
143. dbnptime = time.time() - proctime 
144. 
145. # Compute OPTICS XI
146. proctime = time.time() 
147. op = OPTICS(min_samples= 3 , metric='euclidean', cluster_method='xi', xi= 0.1,
          min_{\text{cluster\_size}} = 0.4, algorithm='brute').fit(X)
148. optime = time.time() - proctime 
149. 
150. proctime = time.time() 
151. opnp = OPTICS(min samples= 3 , metric='euclidean', cluster method='xi', xi= 0.03,
          min cluster size = 0.4, algorithm='brute').fit(Xnp)
152. opnptime = time.time() - proctime 
153. 
154. # Compute OPTICS DBSCAN
155. proctime = time.time() 
156. opdb = OPTICS(min_samples= 8, max_eps= 2.2, metric='euclidean',
           cluster_method='dbscan', algorithm='brute').fit(X) 
157. opdbtime = time.time() - proctime 
158. 
159. proctime = time.time() 
160. opdbnp = OPTICS(min_samples= 10, max_eps= 2, metric='euclidean',
           cluster_method='dbscan', algorithm='brute').fit(Xnp)
```

```
161. opdbnptime = time.time() - proctime 
\frac{162}{163}.
163. # Compute HDBSCAN 
          proctime = time.time()165. hdb = HDBSCAN(min cluster size=12, min samples=3, metric='euclidean', alpha=1.0,
          algorithm='best', leaf size=5,
166. Example 20 genus constructs and the entity cluster selection method='eom',
          allow single cluster=False).fit(X)
167. hdbtime = time.time() - proctime 
168. 
169. proctime = time.time() 
170. hdbnp = HDBSCAN(min_cluster_size=12, min_samples=3, metric='euclidean', alpha=1.0,
          algorithm='best', leaf_size=5, gen_min_span_tree=True,
          cluster_selection_method='eom', allow_single_cluster=False).fit(Xnp) 
171. hdbnptime = time.time() - proctime 
172. 
173. # Compute DENCLUE
174. proctime = time.time() 
175. dcl = DENCLUE(h=None, eps=1, min_density=2e-04, metric='euclidean').fit(X.values) 
          dcltime = time.time() - protein177. 
178. proctime = time.time() 
179. dclnp = DENCLUE(h=None, eps=1, min_density=1.3e-03,
180. metric='euclidean').fit(Xnp.values)
181. dclnptime = time.time() - proctime 
182. 
183. # Compute DBCLASD
184. proctime = time.time() 
185. dbcldiv = 8 
186. dbcl = dbclasd(n neighbors = int(len(X)/dbcldiv)).fit(X.values)
187. dbcltime = time.time() - proctime 
188. 
189. proctime = time.time() 
190. dbclnpdiv = 5 
191. dbclnp = dbclasd(n neighbors = int(len(X)/dbclnpdiv)).fit(Xnp.values)
192. dbclnptime = time.time() - proctime 
193. 
194. for var, lab in zip(cluvarlist,labvarlist): 
195. 
196. # Number of clusters in labels, ignoring noise if present. 
197. labels = eval(var).labels_ 
198. n_clusters_ = len(set(labels)) - (1 if -1 in labels else 0) 
199. n_noise_ = list(labels).count(-1) 
200. cmatrix = metrics.confusion_matrix(labels_true, labels) 
201. 
202. if real n noise + n noise == 0:
203. outacc = 1 
204. noutacc = 1 
205. ovacc = 1 
206. else: 
207. correct_n_noise = cmatrix[0][0] 
208. incorrect_non_outliers = cmatrix[1][0] 
209. outacc = (correct_n_noise/real_n_noise) 
210. noutacc = ((real_non_outliers-incorrect_non_outliers)/real_non_outliers) 
211. ovacc = (correct_n_noise+(real_non_outliers-
                 incorrect_non_outliers))/(real_n_noise + real_non_outliers) 
212. 
213. if n clusters + n noise == 1:
214. silhouette=1
```


```
258. if (var == 'dcl' or var == 'dclnp'): 
                259. pstr = ('eps:%.1e' %eval(var).eps + '\nmin_density:%.1e'
                  %eval(var).min_density) 
260. 
261. if (var == 'dbcl'): 
                pstr = ('n neighbors:%i' %eval(var).n neighbors + '\nArea%%:%.2f'
                   %(1/dbcldiv)263. 
264. if (var == 'dbclnp'): 
265. pstr = ('n neighbors:%i' %eval(var).n neighbors + '\nArea%%:%.2f'
                   %(1/dbclnpdiv)) 
266. 
267. 
268. Results.loc[len(Results)] = np.array([filename, sheet, lab, pstr, n clusters,
              n_noise_,metrics.accuracy_score(labels_true, labels),ovacc, outacc,noutacc, 
              metrics.homogeneity_score(labels_true, labels),
              metrics.completeness_score(labels_true, labels),
              metrics.v_measure_score(labels_true, labels),
              metrics.adjusted_rand_score(labels_true, labels),
              metrics.adjusted_mutual_info_score(labels_true, labels,
              average_method='arithmetic'), silhouette, proctime])
269. 
270. unique_labels = set(labels) 
271. colors = [plt.cm.Set3(each) 
272. for each in np.linspace(0, 1, len(unique_labels))] 
273. 
274. fig, ax = plt.subplots() 
275. ax.text(res1 + 1.5, 1, pstr, fontsize=7,verticalalignment='top', bbox=props) 
276. 
277. # ############### RESULTS PLOT ######################################## 
278. # Black removed and is used for noise instead. 
279. for k, col in zip(unique_labels, colors): 
280. if k == -1: 
281. # Black used for noise.
282. col = [0, 0, 0, 1] 
283. 
284. class member mask = (labels == k)
285. 
286. xy = X[class_member_mask & core_samples_mask] 
287. ax.plot(xy['Column'], xy['Row'], 'o', markerfacecolor=tuple(col), 
288. markeredgecolor='k', markersize=7) 
289. 
290. xy = X[class member mask 8 ~-core samples mask]291. ax.plot(xy['Column'], xy['Row'], 'o', markerfacecolor=tuple(col), 
292. markeredgecolor='k', markersize=5) 
293. 
294. plt.xticks(np.arange(0, res1+1, res1/8)) 
295. plt.yticks(np.arange(0, res1+1, res1/8)) 
296. plt.title(f'{filename} - {lab} [Clusters: {n_clusters_}, Noise: {n_noise_}]') 
297. ax.axis([-0.5, res1+0.5, -0.5, res2+0.5]) 
298. ax.set_aspect(1) 
299. ax.invert_yaxis() 
300. 
301. plt.savefig(f'Data\Cluster data subset\{filename}\{lab} - {filename}.tif',
                  dpi=200, bbox_inches='tight') 
302. plt.clf() 
303. 
304. #### Create TIF files
```


Appendix D

Python Code: Spatial Autocorrelation and Statistical Features

```
1. # -*- coding: utf-8 -*- 
2. """
3. Created on Thu Apr 4 13:22:31 2019
4.
5. @author: Joan Martinez
6. """ 
7. 
8. import numpy as np 
9. import pandas as pd 
10. import scipy as sp 
11. import pysal 
12. import matplotlib.pyplot as plt 
13. import matplotlib as mpl 
14. import skimage.feature as sf 
15. import sys 
16. import time 
17. import glob 
18. import os 
19. from skimage.external import tifffile 
20. 
21. sys.path.append(os.getcwd()+'\\biokit\\viz') 
22. import corrplot 
23. 
24. # create colormap 
25. upper = mpl.cm. jet(np.arange(int(256/4.5), 256))26. cmap = mpl.colors.ListedColormap(upper, name='myColorMap', N=upper.shape[0]) 
27. 
28. 
29. # ############################################################################# 
30. # Load data 
31. 
32. sheet = 'Seatpan' 
33. Dataset = 'Static' 
34. #Dataset = 'Paired' 
35. 
36. Y1 = pd.read_excel('Data\\{Dataset} data subset.xlsx', sheet_name=sheet) 
37. 
38. os.makedirs('Data\\{Dataset} data subset\\' + sheet + '\\Results' , exist_ok=True) 
39. os.makedirs('Data\\{Dataset} data subset\\' + sheet + '\\Plots', exist_ok=True) 
40. 
41. nindex = np.size(Y1u10c[1,:])42. 
43. res1 = 32 
44. res2 = 32 
45. pmax = 300 
46. 
47. Y = np.float32(Y1.values.reshape(res1,res2,nindex)) 
48. Ym = np.ma.masked where(Y == 0, Y) ## unactive cells = 0 mmHg
49. Y1m = np.ma.masked where(Y1 == \theta, Y1) ## unactive cells = \theta mmHg
50. 
51. ############################################################################## 
52. ############################################################################## 
53. 
54. #Spatial Autocorrelation Variales 
55. miarrq, gcarrq, miarrc, gcarrc, miarrid, gcarrid = (np.zeros(nindex) for _ in range(6))
56. 
57. # Weight Matrix for Autocorrelation 
58. wq = pysal.lat2W(res1,res2, rook = False) 
59. X = np.array(np.meshgrid(np.arange(1,res1+1),np.arange(1,res2+1))).T.reshape(-1,2)
```

```
60. wid = pysal.threshold continuousW from array(X,2*2**0.5)61. wc = pysal.threshold_continuousW_from_array(X,2*2**0.5, alpha = 0)
62. 
63. #First Order Statistics Variables 
64. ctarr, sumarr, meanarr,sdarr,cvarr, skewarr,kurtarr = (np.zeros(nindex) for _ in range(7))
65. histarr = np.zeros(shape=(pmax+1, nindex)) 
66. 
67. #Gradient Variables 
68. diffx = np.ma.array(np.zeros(shape = (res1,res2-1,nindex)))
69. diffy = np.ma.array(np.zeros(shape = (res1-1,res2,nindex))) 
70. gradx,grady = (np.ma.array(np.zeros(shape = (res1,res2,nindex))) for _ in range(2)) 
71. histdiffxarr, histdiffyarr = (np.zeros(shape=(pmax+1, nindex)) for _ in range(2)) 
72. 
73. #GLD Variables 
74. gradprobdistrx,gradprobdistry = (np.zeros(shape=(pmax+1, nindex)) for _ in range(2)) 
75. [gradcontrastx,gradcontrasty,gradsecmomentx,gradsecmomenty, 
76. gradentropyx,gradentropyy,gradmeanx,gradmeany, 
77. invdiffmomx,invdiffmomy] = (np.zeros(nindex) for _ in range(10)) 
78. 
79. #GLSD Variables 
80. [glsd_energyx,glsd_energyy,glsd_contrastx,glsd_contrasty, 
81. glsd_correlationx,glsd_correlationy,glsd_homogeneityx,glsd_homogeneityy, 
82. glsd_entropyx,glsd_entropyy] = (np.zeros(nindex) for _ in range(10)) 
83. 
84. 
85. start = time.time()
86. #INDEX LOOP 
87. i = 088. for i in range(nindex): 
89. 
90. miarrq[i] = "%.5f" %pysal.Moran(Y[:, :, i], wq, permutations=2).I
91. gcarrq[i] = "%.5f" %pysal.Geary(Y[:,:,i], wq, permutations=2).C 
92. 
93. miarrc[i] = "%.5f" %pysal.Moran(Y[:, j], wc, permutations=2).I
94. gcarrc[i] = "%.5f" %pysal.Geary(Y[:, :, i], wc, permutations=2).C
95. 
96. miarrid[i] = "%.5f" %pysal.Moran(Y[:,:,i], wid, permutations=2).I
97. gcarrid[i] = "%.5f" %pysal.Geary(Y[:,:,i], wid, permutations=2).C 
98. 
99. histarr[:,[i]] = np.histogram([Ym[:,j,i]],pmax+1)[0].reshape(pmax+1,1)100. 
101. ## Only active cells 
102. ctarr[i] = np.ma.MaskedArray.count(Y1m[:,i])
103. sumarr[i] = np.ma.MaskedArray.sum(Y1m[:,i])
104. meanarr[i] = "%.5f"%sp.stats.mstats.describe(Y1m[:,i]).mean
105. sdarr[i] = "%.5f"%np.sqrt(sp.stats.mstats.describe(Y1m[:,i]).variance
106. cvarr[i] = "%.5f"%sp.stats.mstats.variation(Y1m[:,i])
107. skewarr[i] = "%.5f"%sp.stats.mstats.skew(Y1m[:,i]) 
108. kurtarr[i] = "%.5f"%sp.stats.mstats.kurtosis(Y1m[:,i]) 
109. 
110. ## FIRST ORDER GRADIENT 
111. diffy[:,:,i] = abs(np.diff(Ym[:,:,i], axis=0))112. diffx[:, :, i] = abs(np.diff(Ym[:, :, i], axis=1))113. 
114. histdiffxarr[:,[i]] = np.histogram(diffx[:,:,i].compressed(),pmax+1, [0,pmax])[0].
          reshape(pmax+1,1) 
115. histdiffyarr[:,[i]] = np.histogram(diffy[:,:,i].compressed(),pmax+1, [0,pmax])[0].
         reshape(pmax+1,1)
```
116. 117. gradprobdistrx[:,[i]] = histdiffxarr[:,[i]]/np.sum(histdiffxarr[:,[i]]) 118. gradprobdistry[:,[i]] = histdiffyarr[:,[i]]/np.sum(histdiffyarr[:,[i]]) 119. 120. gradcontrastx[i] = np.sum(gradprobdistrx[:,[i]]\*(np.arange(pmax+1). reshape(pmax+1,1))\*\*2) 121. gradcontrasty[i] = np.sum(gradprobdistry[:,[i]]\*(np.arange(pmax+1). reshape(pmax+1,1))\*\*2) 122. 123. gradsecmomentx $[i] = np.sum(gradprobability[:[i]]**2)$ 124. gradsecmomenty[i] = np.sum(gradprobdistry[:,[i]]\*\*2) 125. 126. gradentropyx[i] = sp.stats.entropy(gradprobdistrx[:,[i]], base=2)[0] 127. gradentropyy[i] = sp.stats.entropy(gradprobdistry[:,[i]], base=2)[0] 128. 129. gradmeanx $[i] = np.sum(gradprobability[:[i]]*(np.arange(pmax+1).reshape(pmax+1,1)))$ 130. gradmeany[i] = np.sum(gradprobdistry[:,[i]]\*(np.arange(pmax+1).reshape(pmax+1,1))) 131. 132. invdiffmomx[i] = np.sum(gradprobdistrx[:,[i]]/((np.arange(pmax+1). reshape(pmax+1,1))\*\*2+1)) 133. invdiffmomy[i] = np.sum(gradprobdistry[:,[i]]/((np.arange(pmax+1). reshape(pmax+1,1))\*\*2+1)) 134. 135. ## SECOND ORDER CENTRAL GRADIENT 136. grady[:,:,i] = np.gradient(Ym[:,:,i], edge\_order=1, axis=0) 137. gradx $[:, j] = np$ .gradient $(Ym[:, j]$ , edge order=1, axis=1) 138. 139. ########################### SECOND ORDER STAT FEATURES ########## 140. 141. #Removing first 0 pressure column 142. gcm2 = np.float64(sf.greycomatrix(np.uint16(np.round(Ym[:,:,i])),[1],[0, np.pi/2], levels=pmax+1, symmetric=True)[1:,1:,:,:]) 143. gcm2[:,:,0,0] = gcm2[:,:,0,0]/np.sum(gcm2[:,:,0,0]) 144.  $\text{gen2}[:,:,0,1] = \text{gen2}[:,:,0,1] / np.sum(\text{gen2}[:,:,0,1])$ 145. 146. glsd\_energyx[i] = (sf.greycoprops(gcm2, "energy")\*\*2)[0,0] 147. glsd\_energyy[i] = (sf.greycoprops(gcm2, "energy")\*\*2)[0,1] 148. 149. glsd\_contrastx[i] = sf.greycoprops(gcm2, "contrast")[0,0] 150. glsd\_contrasty[i] = sf.greycoprops(gcm2, "contrast")[0,1] 151. 152. glsd\_correlationx[i] = sf.greycoprops(gcm2, "correlation")[0,0] 153. glsd\_correlationy[i] = sf.greycoprops(gcm2, "correlation")[0,1] 154. 155. glsd entropyx $[i] = sp.$ stats.entropy(np.reshape(gcm2,(-1,2)), base=2) [np.newaxis][0,0] 156. glsd entropyy $[i] = sp.$ stats.entropy(np.reshape(gcm2,(-1,2)), base=2) [np.newaxis][0,1] 157. 158. glsd\_homogeneityx[i] = sf.greycoprops(gcm2, "homogeneity")[0,0] 159. glsd\_homogeneityy[i] = sf.greycoprops(gcm2, "homogeneity")[0,1] 160. 161. **print**('Processing Indexes Time: ', (time.time() - start)) 162. 163. #### WRITE RESULTS IN EXCEL ################################### 164. 165. filenames = Y1.columns 166.

```
167. resvarlist = ['filenames', 'miarrq', 'gcarrq', 'miarrc', 'gcarrc', 'miarrid',
    'gcarrid', 'ctarr', 'sumarr','meanarr', 'sdarr', 'cvarr', 'skewarr', 'kurtarr'] 
168. 
169. labvarlist = ['Sample', "Moran's I (Q)", "Geary's C (Q)", "Moran's I (CD)",
   "Geary's C (CD)", "Moran's I (ID)", "Geary's C (ID)", 'Contact Cells',
    'Sum of Pressure', 'Mean Pressure', 'Standard Deviation', 'Coefficient of Variation',
    'Skewness', 'Kurtosis'] 
170. 
171. resvarlistx = ['gradcontrastx', 'gradsecmomentx', 'gradentropyx', 'gradmeanx',
    'invdiffmomx', 'glsd_energyx', 'glsd_contrastx', 'glsd_correlationx', 'glsd_entropyx', 'gl
   sd homogeneityx']
172. 
173. labvarlistx = ['GLD - Gradient Contrast X', 'GLD - Gradient Second Moment X',
    'GLD - Gradient Entropy X', 'GLD - Gradient Mean X',
    'GLD - Inverse-Difference Moment X', 'GLSD - Energy X', 'GLSD - Contrast X',
    'GLSD - Correlation X', 'GLSD - Entropy X', 'GLSD - Homogeneity X'] 
174. 
175. resvarlisty = ['gradcontrasty', 'gradsecmomenty', 'gradentropyy', 'gradmeany',
    'invdiffmomy', 'glsd_energyy', 'glsd_contrasty', 'glsd_correlationy', 'glsd_entropyy',
    'glsd_homogeneityy'] 
176. 
177. labvarlisty = ['GLD - Gradient Contrast Y', 'GLD - Gradient Second Moment Y',
    'GLD - Gradient Entropy Y', 'GLD - Gradient Mean Y',
    'GLD - Inverse-Difference Moment Y', 'GLSD - Energy Y', 'GLSD - Contrast Y',
    'GLSD - Correlation Y', 'GLSD - Entropy Y', 'GLSD - Homogeneity Y'] 
178. 
179. Results = pd.DataFrame(columns=labvarlist + labvarlistx + labvarlisty) 
180. 
181. for var, lab in zip(resvarlist + resvarlistx + resvarlisty,labvarlist + labvarlistx
                         + labvarlisty): 
182. Results[lab] = eval(var) 
183. 
184. from excelappend import append_df_to_excel 
185. append df to excel(f'Data\\{Dataset} data subset\\{sheet}\Results\{Dataset}
    Pressure Parameteres Results.xlsx', Results, sheet name=sheet)
186. 
187. corr = Results.corr(method='pearson') 
188. c = corrplot.Corrplot(corr) 
189. c.plot(method='ellipse', shrink=0.8, rotation=45, upper='text', lower='pie') 
190. fig = plt.get()191. fig.set_size_inches(20, 16); 
192. plt.title(f'{Dataset} Data Subset - Pressure Parameters Correlations') 
193. plt.savefig(f'Data\\{Dataset} data subset\\{sheet}\\{Dataset} Pressure Parameters
    Correlations.tif', dpi=200, bbox_inches='tight') 
194. 
195. append df to excel(f'Data\\{Dataset} data subset\\{sheet}\Results\{Dataset} Pressure
    Parameteres Correlations.xlsx', corr, sheet name=sheet)
196. 
197. 
198. ######## INDEXES MAPS & PLOTS ############################## 
199. start = time.time()200. dpishow = 100 
201. dpisave = 200 
202. 
203. i = 0204. for i in range(nindex): 
205. plt.clf() 
206. plt.figure(figsize=(5, 4), dpi=200) 
207. plt.imshow(Ym[:,:,i], cmap=cmap);
```

```
208. plt.clim(0,pmax) 
209. plt.colorbar() 
210. plt.title(f'%s, Pressure Map (mmHg) [CV = %.3f]' %(filenames[i],cvarr[i])) 
211. #plt.show() 
212. plt.savefig(f'Data\\{Dataset} data subset\\{sheet}\Plots\Pressure Map -
        Sample %s.tif' %filenames[i], dpi=dpisave, bbox_inches='tight')
213. 
214. plt.clf() 
215. plt.figure(figsize=(5, 2), dpi=dpishow) 
216. plt.hist(Y1m[:,i].compressed(),pmax+1,[0,pmax]) 
217. plt.xlabel('Pressure (mmHg)', fontsize=12) 
218. plt.title(f'%s, {sheet} Pressure Histogram' %filenames[i]) 
219. #plt.show() 
220. plt.savefig(f'Data\\{Dataset} data subset\\{sheet}\Plots\Histogram -
         Sample %s.tif' %filenames[i], dpi=dpisave, bbox_inches='tight') 
221. 
222. plt.clf() 
223. fig, (ax1, ax2) = plt.subplots(1, 2, dpi=dpishow)224. im1=ax1.imshow(gradx[:,:,i], cmap='seismic', vmin=-pmax, vmax=pmax);<br>225. ax1.set title('[0°, X-axis]')
         ax1.set\_title('[0°, X-axis]')226. im2=ax2.imshow(grady[:,:,i], cmap='seismic', vmin=-pmax, vmax=pmax);
227. ax2.set_title('[90°, Y-axis]') 
228. fig.subplots adjust(right=1.2)
229. cbar ax = fig.add axes([1, 0.15, 0.05, 0.7])
230. fig.colorbar(im2, cax=cbar_ax) 
231. plt.suptitle(f'%s, {sheet} Second Order Central Gradient Map (mmHg)' %filenames[i],
         horizontalalignment='center') 
232. fig.tight_layout(rect=[0, 0.03, 1, 0.95]) 
233. #plt.show() 
234. plt.savefig(f'Data\\{Dataset} data subset\\{sheet}\Plots\Central Gradient Map -
         Sample %s.tif' %filenames[i], dpi=dpisave, bbox_inches='tight') 
235. 
236. plt.clf() 
237. fig, (ax1, ax2) = plt.subplots(1,2, dipi=dpishow)238. gim1=ax1.imshow(diffx[:,:,i], cmap='YlOrRd', vmin=0, vmax=pmax);
239. ax1.set_title('[0°, X-axis]') 
240. im2=ax2.imshow(diffy[:,:,i], cmap='YlOrRd', vmin=0, vmax=pmax);
241. ax2.set_title('[90°, Y-axis]') 
242. fig.subplots_adjust(right=1.2) 
243. cbar_ax = fig.add_axes([1, 0.15, 0.05, 0.7]) 
244. fig.colorbar(im2, cax=cbar_ax) 
245. plt.suptitle(f'%s, {sheet} First Order Absolute Gradient Map (mmHg)' %filenames[i],
         horizontalalignment='center') 
246. fig.tight_layout(rect=[0, 0.03, 1, 0.95]) 
247. #plt.show() 
248. plt.savefig(f'Data\\{Dataset} data subset\\{sheet}\Plots\Absolute Gradient Map -
         Sample %s.tif' %filenames[i], dpi=dpisave, bbox_inches='tight') 
249. 
250. plt.clf() 
251. fig, (ax1, ax2) = plt.subplots(1,2, figsize=(8,3), dpi=dpishow, sharey=True) 
252. im1=ax1.hist(diffx[:,:,i].compressed(),pmax+1,[0,pmax]); 
253. ax1.set_title('[0°, X-axis]') 
254. ax1.set_xticks(np.arange(0, pmax+1, 50)) 
255. ax1.set_xlabel('Pressure (mmHg)', fontsize=10) 
256. im2=ax2.hist(diffy[:,:,i].compressed(),pmax+1,[0,pmax]); 
257. ax2.set_title('[90°, Y-axis]') 
258. ax2.set_xticks(np.arange(0, pmax+1, 50)) 
259. ax2.set_xlabel('Pressure (mmHg)', fontsize=10)
```

```
243
```

```
260. plt.suptitle(f'%s, {sheet} First Order Absolute Gradient Histogram (mmHg)'
         %filenames[i], horizontalalignment='center') 
261. fig.tight_layout(rect=[0, 0.03, 1, 0.95]) 
262. #plt.show()<br>263. plt.savefig
         263. plt.savefig(f'Data\\{Dataset} data subset\\{sheet}\Plots\Absolute Gradient
 Histogram - Sample %s.tif' %filenames[i], dpi=dpisave, bbox_inches='tight') 
         plt.c1f()265. 
266. #### Create TIF files 
267. with tifffile.TiffWriter(f'Data\\{Dataset} data subset\\{sheet}\{Dataset} Data Subset 
                             Pressure Maps.tif') as stack: 
268. for fname in sorted(glob.glob(f'Data\\{Dataset} data subset\\{sheet}\Plots\
          Pressure Map - Sample*.tif'), key=os.path.getmtime): 
269. stack.save(tifffile.imread(fname), compress=6) 
270. 
271. with tifffile.TiffWriter(f'Data\\{Dataset} data subset\\{sheet}\{Dataset} Data Subset
                                      Pressure Histograms.tif') as stack: 
272. for fname in sorted(glob.glob(f'Data\\{Dataset} data subset\\{sheet}\Plots\
 Histogram - Sample*.tif'), key=os.path.getmtime): 
             stack.save(tifffile.imread(fname), compress=6)
274. 
275. with tifffile.TiffWriter(f'Data\\{Dataset} data subset\\{sheet}\{Dataset} Data Subset,
                               Central Gradient Map.tif') as stack: 
276. for finame in sorted(glob.glob(f'Data\\{Dataset} data subset\\{sheet}\Plots\
          Central Gradient Map - Sample*.tif'), key=os.path.getmtime): 
277. stack.save(tifffile.imread(fname), compress=6) 
278. 
279. with tifffile.TiffWriter(f'Data\\{Dataset} data subset\\{sheet}\{Dataset} Data Subset
                                Absolute Gradient Map.tif') as stack: 
280. for fname in sorted(glob.glob(f'Data\\{Dataset} data subset\\{sheet}\Plots\Absolute
          Gradient Map - Sample*.tif'), key=os.path.getmtime): 
281. stack.save(tifffile.imread(fname), compress=6) 
282. 
283. with tifffile.TiffWriter(f'Data\\{Dataset} data subset\\{sheet}\{Dataset} Data Subset
                                Absolute Gradient Histogram.tif') as stack: 
284. for fname in sorted(glob.glob(f'Data\\{Dataset} data subset\\{sheet}\Plots\
         Absolute Gradient Histogram - Sample*.tif'), key=os.path.getmtime): 
285. stack.save(tifffile.imread(fname), compress=6) 
286. 
287. print('Processing Plots Time: ', (time.time() - start))
```
Appendix E

Python Code: Image Registration and Similarity/Dissimilarity Coefficients

```
1. # -*- coding: utf-8 -*- 
2. """
3. Created on Mon Aug 5 10:22:04 2019
4.
5. @author: Joan Martinez
6. """ 
7. 
8. import numpy as np 
9. import pandas as pd 
10. import scipy as sp 
11. import matplotlib.pyplot as plt 
12. import matplotlib as mpl 
13. import time 
14. import glob 
15. import os 
16. from skimage.external import tifffile 
17. from scipy.ndimage import rotate, shift 
18. import SimpleITK as sitk 
19. 
20. # create colormap 
21. upper = mpl.cm.jet(np.arange(int(256/4.5),256)) 
22. cmap = mpl.colors.ListedColormap(upper, name='myColorMap', N=upper.shape[0]) 
23. 
24. # ############################################################################# 
25. # Load data 
26. 
27. Dataset = "Synthetic" 
28. sheet = 'Seatpan' 
29. sheet2 = 'Template' 
30. 
31. Y1 = pd.read_excel(f'Data\\{Dataset} data subset.xlsx', sheet_name=sheet) 
32. Y2 = pd.read_excel(f'Data\\{Dataset} data subset.xlsx', sheet_name=sheet2) 
33. 
34. Y1m = np.ma.masked_where(Y1 == 0, Y1) ## unactive cells = 0 mmHg
35. Y2m = np.ma.masked where(Y2 == 0, Y2) ## unactive cells = 0 mmHg
36. 
37. nindex1 = np.size(Y1.iloc[1, :])
38. nindex2 = np.size(Y2.iloc[1, :])
39. 
40. res1 = 32 
41. res2 = 32 
42. pmax = 300 
43. 
44. X1 = np.float32(Y1.values.reshape(res1,res2,nindex1)) 
45. X1m = np.ma.masked where(X1 == \theta, X1) ## unactive cells = 0 mmHg
46. 
47. X2 = np.float32(Y2.values.reshape(res1,res2,nindex2)) 
48. X2m = np.ma.masked where(X2 == \theta, X2) ## unactive cells = \theta mmHg
49. 
50. 
51. ############################################################################## 
52. ############################################################################## 
53. 
54. i = 055. i = 056. eps = 157. 
58. filename1 = Y1.columns[i] 
59. filename2 = Y2.columns[j]
```

```
60. if Dataset == "Synthetic": 
61. # Apply transformation 
62. hloc = 1
63. vloc = -1 
64. rot = -15 
65. 
66. template = shift(X2[:,:,j], [-vloc,hloc],order=0,prefilter=False) 
67. template = rotate(template, rot, reshape=False)
68. else:
69. [hloc,vloc,rot] = (0 for _ in range(3))
70. template = X2[:, :, j]71. 
72. plt.imshow(X1[:,:,i]) 
73. plt.show() 
74. plt.imshow(template) 
75. print("\n",filename1," vs ", filename2) 
76. 
77. os.makedirs(f'Data\{Dataset} data subset\\' + filename1 + ' vs ' + filename2 , 
               exist_ok=True) 
78. 
79. dpishow = 100 
80. dpisave = 200 
81. 
82. for method in ["MI","MSE"]: 
83. 
84. # Callback invoked when the StartEvent happens, sets up our new data. 
85. def start_plot(): 
86. global metric values, multires iterations
87. 
88. metric values = []
89. multires_iterations = [] 
90. 
91. # Callback invoked when the EndEvent happens, do cleanup of data and figure. 
92. def end_plot(): 
93. global metric values, multires iterations
94. 
95. del metric_values 
96. del multires_iterations 
97. # Close figure, we don't want to get a duplicate of the plot latter on.
98. plt.close() 
99. 
100. # Callback invoked when the IterationEvent happens, update our data and 
101. # save an image that includes a visualization of the registered images and 
102. # the metric value plot.
103. def save plot(registration method, fixed, moving, transform, file name prefix):
104. 
105. # 
106. # Plotting the similarity metric values, resolution changes are marked with 
107. # a blue star.
108. # 
109. global metric_values, multires_iterations, ref, trans, regmetric, iterreg
110. 
111. metric_values.append(registration_method.GetMetricValue()) 
112. 
113. 
114. moving_transformed = sitk.Resample(moving, fixed, transform, 
115. sitk.sitkLinear, 0.0, 
116. moving_image.GetPixelIDValue()) 
117.
```

```
118. http://web.ack.org/mark.formage(fixed)))<br>119. http://web.ack.org/mark.org/mark.org/mark.formage(movin
119. trans = np.dstack((trans,sitk.GetArrayFromImage(moving_transformed))) 
             regmetric = np.append(regmetric,registration method.GetMetricValue())
121. iterreg = [index for index in multires_iterations] 
122. 
123. # Callback invoked when the sitkMultiResolutionIterationEvent happens, update the
          Index into the metric_values list. 
124. def update_multires_iterations(): 
125. global metric_values, multires_iterations 
126. multires iterations.append(len(metric values))
127. 
128. if __name__ == '__main__': 
129. 
130. # Read the images
131. factor = 10 
132. ref = np.zeros(shape = (res1*factor,res2*factor,0)) 
133. trans = np.zeros(shape = (res1*factor,res2*factor,0))
134. regmetric = np{\cdot}zeros(\theta)135. iterreg = np{\text{.}zeros}(\theta)136. 
137. fixed_image = sitk.Expand(sitk.GetImageFromArray(X1[:,:,i]),[factor]*2, sitk.s
                           itkLinear) 
138. moving_image = sitk.Expand(sitk.GetImageFromArray(template),[factor]*2, sitk.si
                           tkLinear) 
139. 
140. fig, (ax1, ax2) = plt.subplots(1, 2, dpi=dpishow) 
141. im1 = ax1.imshow(np.ma.masked where(sitk.GetArrayFromImage(fixed image) < 1, si
                             tk.GetArrayFromImage(fixed_image)), cmap=cmap, vmax = pmax) 
142. ax1.set title(f'[Reference Image]')
143. ax2.imshow(np.ma.masked_where(sitk.GetArrayFromImage(moving_image) < 1, sitk.Ge
                       tArrayFromImage(moving_image)), cmap=cmap, vmax = pmax) 
144. ax2.set_title(f'[Template Image]') 
145. fig.subplots adjust(right=1.2)
146. cbar_ax = fig.add_axes([1, 0.15, 0.05, 0.7]) 
147. fig.colorbar(im1, cax=cbar ax)
148. plt.suptitle(f'{method} Image Registration: {filename1} vs {filename2}, Scaling
     Factor: {factor}', horizontalalignment='center') 
149. fig.tight_layout(rect=[0, 0.03, 1, 0.95]) 
150. plt.savefig(f'Data\{Dataset} data subset\{filename1} vs {filename2}\{method} Im
              age Registration, {filename1} vs {filename2} Template.tif', dpi=200,
              bbox_inches='tight') 
151. 
152. # Multi-resolution rigid registration 
153. registration_method = sitk.ImageRegistrationMethod() 
154. 
155. # Initial alignment of the two volumes 
156. transform = sitk.CenteredTransformInitializer(fixed_image, 
157. moving image,
158. sitk.Euler2DTransform(), 
159. sitk.CenteredTransformInitializer
                                                     Filter.MOMENTS)
160. 
161. 
162. if method == "MI": 
163. registration_method.SetMetricAsJointHistogramMutualInformation(numberOfHisto
                                  gramBins=50, varianceForJointPDFSmoothing = 1.5) 
164. elif method == "MSE": 
165. registration_method.SetMetricAsMeanSquares() 
166.
```


```
216. props = dict(boxstyle='round', facecolor='wheat', alpha=0.3) 
217. for x in range(len(ref[0,0,:])): 
218. 
219. ## PRESSURE PARAMETERS 
220. ct_ireg[x] = np.ma.MaskedArray.count(refm1d[:,x]) 
221. sum_ireg[x] = np.ma.MaskedArray.sum(refm1d[:,x])<br>222. mean ireg[x] = sp.stats.mstats.describe(refm1d[:
              222. mean_ireg[x] = sp.stats.mstats.describe(refm1d[:,x]).mean ## Only active cells
223. cv ireg[x] = sp.stats.mstats.variation(refm1d[:,x])224. cpx_ireg[x] = sp.ndimage.measurements.center_of_mass(refm2d[:,:,x])[0] 
225. cpy ireg[x] = sp.ndimage.measurements.center of mass(refm2d[:,:,x])[1]
226. 
227. ct_jreg[x] = np.ma.MaskedArray.count(transm1d[:,x]) 
228. sum_jreg[x] = np.ma.MaskedArray.sum(transm1d[:,x]) 
229. mean_jreg[x] = sp.stats.mstats.describe(transm1d[:,x]).mean # Only active cells
230. cv_jreg[x] = sp.stats.mstats.variation(transm1d[:,x])
231. 
232. if ct_jreg[x]>0: 
233. cpx_jreg[x] = sp.ndimage.measurements.center_of_mass(transm2d[:,:,x])[0] 
234. cpy_jreg[x] = sp.ndimage.measurements.center_of_mass(transm2d[:,:,x])[1] 
235. 
236. ct_regdiff[x]=abs(ct_ireg[x]-ct_jreg[x]) 
237. cp_regdiff[x]=((cpx_ireg[x]-cpx_jreg[x])**2+(cpy_ireg[x]-
                           cpy_jreg[x])**2)**0.5 
238. 
239. 
240. # SIMILARITY MEASURES ###################################################### 
241. #Person Correlation Coefficient 
242. pcc2imgreg[x] = np.ma.corrcoef(refm1d[:,x],transm1d[:,x])[0,1] #Masked
243. pcc3imgreg[x] = np.corrcoef(refm1d[:,x].data,transm1d[:,x].data)[0,1] #Non-
                                                                             Masked 
244. 
245. #Tanimoto Measure 
246. tm1imgreg[x] = np.ma.sum(refm1d[:,x]*transm1d[:,x])/(np.ma.sum((refm1d[:,x]-
                         transm1d[:,x])**2)+np.ma.sum(refm1d[:,x]*transm1d[:,x])) #Masked 
247. tm2imgreg[x] = np.sum(refm1d[:,x].data*transm1d[:,x].data)/(np.sum((refm1d[:,x]
                         .data-transm1d[:,x].data)**2)+np.sum(refm1d[:,x].data*
                         transm1d[:,x].data)) #Non-Masked 
248. 
249. #Min-Ratio 
250. minr1reg = np.ma.minimum([refm1d[:,x]/transm1d[:,x]],[transm1d[:,x]/refm1d[:,x]
                                    ]).reshape(-1,1) 
251. minr1reg = np.ma.array(minr1reg,mask=np.logical_or(refm1d[:,x].mask,transm1d[:,
                                  x].mask)) 
252. minr1imgreg[x] = np.ma.mean(minr1reg) #Masked 
253. 
254. Y1epsreg = refm1d[:,x] +eps255. Y2epsreg = transm1d[:,x] +eps256. minr2reg = np.minimum([Y1epsreg/Y2epsreg],[Y2epsreg/Y1epsreg]).reshape(-1,1) 
257. minr2reg = np.ma.array(minr2reg, mask = np.logical_and(Y1epsreg.mask,
                                  Y2epsreg.mask)) 
258. minr2imgreg[x] = np.mean(minr2reg) #Non-Masked () 
259. 
260. # DISSIMILARITY MEASURES ######################################################
261. #L1 Norm 
262. l1n1imgreg[x] = np.ma.sum(abs(refm1d[:,x]-transm1d[:,x])) #Masked
263. l1n2imgreg[x] = np.sum(abs(refm1d[:,x].data-transm1d[:,x].data)) #Non-Masked 
264. 
265.
```

```
266. #L2 Norm 
267. l2n1imgreg[x] = np.ma.sum((refm1d[:,x]-transm1d[:,x])**2) #Masked
268. l2n2imgreg[x] = np.sum((refm1d[:,x].data-transm1d[:,x].data)**2) #Non-Masked 
269. 
270. #Intensity-Ratio Variance 
271. irvar1imgreg[x] = np.ma.var(refm1d[:,x]/transm1d[:,x]) #Masked 
272. 
273. irvar2reg = np.ma.array(Y1epsreg/Y2epsreg, mask = np.logical_and(Y1epsreg.mask,
                                  Y2epsreg.mask)) 
274. irvar2imgreg[x] = np.var(irvar2reg) #Non-Masked
275. 
276. plt.clf() 
277. fig = plt.figure() 
278. ax1 = fig.addsubplot(111)279. #fig, (ax1, ax2) = plt.subplots(1, 2, dpi=dpishow) 
280. im1=ax1.imshow(refm2d[:,:,x], cmap=cmap,alpha=.5,vmax=pmax); 
281. #ax1.set_title(f'{filename1}, Index %i, [Reference Image]' %i) 
282. im2=ax1.imshow(transm2d[:,:,x], cmap=cmap, alpha=.5, vmax=pmax); 
283. pstrm = (f'__________________________\nPCC:\t\t {pcc2imgreg[x]:.3f}\nTanimoto:
                      \t{tm1imgreg[x]:.3f}' 
284. f'\nMin-Ratio:\t {minr1imgreg[x]:.3f}\nL1 Norm:\t{l1n1imgreg[x]:.2f}
                       \nL2 Norm:\t{l2n1imgreg[x]:.2f}' 
285. f'\nInt-Ratio Var:\t{irvar1imgreg[x]:.3f}').expandtabs() 
286. pstrnm = (f'________NON-MASKED_______\nPCC:\t\t {pcc3imgreg[x]:.3f}\nTanimoto:
                      \t{tm2imgreg[x]:.3f}' 
287. f'\nMin-Ratio:\t {minr2imgreg[x]:.3f}\nL1 Norm:\t{l1n2imgreg[x]:.2f}
                    \nL2 Norm:\t{l2n2imgreg[x]:.2f}' 
288. f'\nInt-Ratio Var:\t{irvar2imgreg[x]:.3f}').expandtabs() 
289. pstrmet = (f' OTHER METRICS \nContact Diff:\t\t {ct_regdiff[x]:.0f}'
290. f'\nCP-CP Distance:\t\t {cp_regdiff[x]:.2f}').expandtabs()
291. plt.text((res1 + 1.5)*factor, 1*factor, pstrm, fontsize=7,verticalalignment='to
                     p', bbox=props) 
292. plt.text((res1 + 1.5)*factor, 13*factor, pstrnm, fontsize=7,verticalalignment='
                     top', bbox=props) 
293. plt.text((res1 + 1.5)*factor, 24*factor, pstrmet, fontsize=7,verticalalignment=
                     'top', bbox=props) 
294. plt.title(f'{method} Image Registration: {filename1} vs {filename2}, Iteration
                       {x}\nMetric: {regmetric[x]}\n', horizontalalignment='center') 
295. cbar_ax = fig.add_axes([0, 0.145, 0.04, 0.6]) 
296. cbar = plt.colorbar(im1, cax=cbar_ax) 
297. cbar.ax.yaxis.set_ticks_position('left') 
298. fig.tight_layout(rect=[-0.2, 0.03, 1, 0.95]) 
299. plt.savefig(f'Data\{Dataset} data subset\{filename1} vs {filename2}\{method}
                        Image Registration, {filename1} vs {filename2}, Iteration {x}.tif',
                        dpi=200, bbox_inches='tight') 
300. 
301. for x in range(len(ref[0,0,:])): 
302. plt.clf() 
303. fig = plt.figure() 
304. ax1 = fig.add subplot(111)
305. clim = max(np.abs(np.min(diffm2d[:,:,x])),np.max(diffm2d[:,:,x]))
306. im1=ax1.imshow(diffm2d[:,:,x], cmap='seismic', vmin=-clim, vmax=clim) 
307. plt.title(f'{method} Image Registration: {filename1} vs {filename2}, Iteration
                   {x}\n[Reference - Transformed] (mmHg)\n', horizontalalignment='center')
308. cbar_ax = fig.add_axes([0.70, 0.145, 0.04, 0.6]) 
309. fig.colorbar(im1, cax=cbar_ax) 
310. fig.tight_layout(rect=[-0.2, 0.03, 1, 0.95])
311. 
312.
```


Appendix F

Cluster Data Subset: Samples with Outliers

















Appendix G

Cluster Data Subset: Samples without Outliers



 $0 -$ 

5

 $10\,$ 

 $15<sub>1</sub>$ 

20

25

30

 $\mathbf 0$  -

5

 $10$ 

15

20

25

30

 $\mathbf 0$ 

 $\mathsf S$ 

 $10\,$ 

15

20

25

30

 $\mathbf 0$ 

 $\mathsf S$ 

 $10\,$ 

 $15\,$ 

20

25

 $30\,$ 

 $\mathbf 0$ 

 $\dot{o}$ 

 $\ddot{\mathbf{0}}$ 

 $\dot{o}$ 





 $\mathbf 0$ 

 $10\,$ 

 $\mathbf 0$  -

 $\mathbf 0$ 

 $\mathsf S$ 

 $10\,$ 

 $\mathbf 0$ 

 $\mathsf S$ 

 $10\,$ 

 $15\,$ 

 $30\,$ 



Appendix H

Static Data Subset: Samples based on CV levels
$250$ 

 $-200$ 

 $-150$ 

 $100$ 

50

 $\mathbf 0$ 

250

 $-200$ 

 $-150$ 

 $-100$ 

50

 $\overline{\mathbf{0}}$ 

 $-250$ 

 $-200$ 

 $-150$ 

100

50

 $\mathsf{o}\xspace$ 

 $-250$ 

200

 $-150$ 

100

50

 $\mathbf 0$ 











Appendix I

Static Data Subset: Spatial Autocorrelation



Appendix J

Paired Data Subset: Samples based on Contact, Pressure and CV levels







 $\overline{\mathbf{0}}$ 

5  $10\,$ 

 $15 -$ 

20

 $25 -$ 

30

 $\ddot{\mathbf{0}}$ 



Appendix K

Paired Data Subset: Pressure Measures Results





















Appendix L

Transformed Data Subset: Upscaled Samples and Transformations





Transformation 1 [Horizontal: +3, Vertical: −3, Rotation: +15°]



MI Image Registration: 144-1-940 vs 144-1-940T, Scaling Factor: 10

Transformation 2 [Horizontal: −2, Vertical: −1, Rotation: −6°]



MI Image Registration: 144-1-940 vs 144-1-940T, Scaling Factor: 10





Transformation 1 [Horizontal: +4, Vertical: −7, Rotation: −20°]

MI Image Registration: 115-1-852 vs 115-1-852T, Scaling Factor: 10



Transformation 2 [Horizontal: +3, Vertical: −2, Rotation: +8°]



MI Image Registration: 115-1-852 vs 115-1-852T, Scaling Factor: 10





Transformation 1 [Horizontal: +2, Vertical: −4, Rotation: −60°]

MI Image Registration: 126-2-2177 vs 126-2-2177T, Scaling Factor: 10





300 [Reference Image] [Template Image]  $\mathbf 0$  $\mathbf 0$ 250 50 50 200 100 100 150  $150 -$ 150 200 200  $-100$  $250 \cdot$  $250 -$ 50 300 300 100  $\ddot{\mathbf{0}}$ 200 300  $\ddot{\mathbf{0}}$ 100 200 300

MI Image Registration: 126-2-2177 vs 126-2-2177T, Scaling Factor: 10





Transformation 1 [Horizontal: −1, Vertical: −3, Rotation: +17°]

MI Image Registration: 145-1-2589 vs 145-1-2589T, Scaling Factor: 10



Transformation 2 [Horizontal: +4, Vertical:+1, Rotation: −7°]



MI Image Registration: 145-1-2589 vs 145-1-2589T, Scaling Factor: 10





Transformation 1 [Horizontal: −1, Vertical: −6, Rotation: +35°]

MI Image Registration: 175-3-1142 vs 175-3-1142T, Scaling Factor: 10



Transformation 2 [Horizontal: +3, Vertical:−2, Rotation: −5°]



MI Image Registration: 175-3-1142 vs 175-3-1142T, Scaling Factor: 10





Transformation 1 [Horizontal: −1, Vertical: −3, Rotation: +36°]

MI Image Registration: 109-2-265 vs 109-2-265T, Scaling Factor: 10



Transformation 2 [Horizontal: +4, Vertical:−1, Rotation: −5°]



MI Image Registration: 109-2-265 vs 109-2-265T, Scaling Factor: 10





Transformation 1 [Horizontal: −2, Vertical: −3, Rotation: +22°]

MI Image Registration: 117-1-1193 vs 117-1-1193T, Scaling Factor: 10



Transformation 2 [Horizontal: +3, Vertical:0, Rotation: −9°]



MI Image Registration: 117-1-1193 vs 117-1-1193T, Scaling Factor: 10





Transformation 1 [Horizontal: +2, Vertical: −5, Rotation: +25°]

MI Image Registration: 158-3-2200 vs 158-3-2200T, Scaling Factor: 10



Transformation 2 [Horizontal: 0, Vertical:−3, Rotation: −10°]



MI Image Registration: 158-3-2200 vs 158-3-2200T, Scaling Factor: 10





Transformation 1 [Horizontal: +2, Vertical: −1, Rotation: +30°]

MI Image Registration: 137-3-2640 vs 137-3-2640T, Scaling Factor: 10



Transformation 2 [Horizontal: −3, Vertical:+1, Rotation: −6°]



MI Image Registration: 137-3-2640 vs 137-3-2640T, Scaling Factor: 10





Transformation 1 [Horizontal: −1, Vertical: −4, Rotation: −12°]

MI Image Registration: 183-2-599 vs 183-2-599T, Scaling Factor: 10



Transformation 2 [Horizontal: +4, Vertical:0, Rotation: +9°]



MI Image Registration: 183-2-599 vs 183-2-599T, Scaling Factor: 10

Appendix M

Transformed Data Subset: Registration Results



Appendix N

Registration Data Subset: Center of Pressure Distances



295

Appendix O

Registration Data Subset: Upscaled Sample Pairs



Image Registration: 152-1-1986 vs 152-1-1990, Scaling Factor: 10

Image Registration: 114-2-1826 vs 114-2-1836, Scaling Factor: 10



Image Registration: 180-2-2584 vs 180-2-2592, Scaling Factor: 10





Image Registration: 141-1-2658 vs 141-1-2668, Scaling Factor: 10

Image Registration: 148-1-3551 vs 148-1-3557, Scaling Factor: 10



Image Registration: 145-1-2811 vs 145-1-1449, Scaling Factor: 10





Image Registration: 185-1-1610 vs 185-1-1620, Scaling Factor: 10





Image Registration: 164-3-3886 vs 164-3-3896, Scaling Factor: 10





Image Registration: 182-1-2048 vs 182-1-2058, Scaling Factor: 10

Image Registration: 174-3-958 vs 174-3-970, Scaling Factor: 10



Image Registration: 129-2-1842 vs 129-2-1852, Scaling Factor: 10





Image Registration: 124-1-705 vs 124-1-719, Scaling Factor: 10

Image Registration: 112-2-1696 vs 112-2-1708, Scaling Factor: 10



Image Registration: 169-2-1993 vs 169-2-2009, Scaling Factor: 10




Image Registration: 181-1-3436 vs 181-1-3446, Scaling Factor: 10





Image Registration: 123-1-2504 vs 123-1-2524, Scaling Factor: 10





Image Registration: 132-1-1990 vs 132-1-2002, Scaling Factor: 10

Image Registration: 183-3-2335 vs 183-3-2342, Scaling Factor: 10



Appendix P

Registration Data Subset: Registration Results



Appendix Q

Registration Data Subset: Optimality Registration Results Maps





Image Registration: 152-1-1986 vs 152-1-1990, Scaling Factor: 10



[Reference - Transformed] (mmHg)



MSE Image Registration: 152-1-1986 vs 152-1-1990, Iteration 15 Metric: 317.74378949193886



Visual feedback: **MSE** registration produced better correspondence in tuberosities and legs.





Image Registration: 114-2-1826 vs 114-2-1836, Scaling Factor: 10



[Reference - Transformed] (mmHg)



MSE Image Registration: 114-2-1826 vs 114-2-1836, Iteration 26 Metric: 366.45105250150675



Visual feedback: **MSE** registration produced better correspondence in tuberosities and legs.





Image Registration: 180-2-2584 vs 180-2-2592, Scaling Factor: 10



[Reference - Transformed] (mmHg)



MSE Image Registration: 180-2-2584 vs 180-2-2592, Iteration 35 Metric: 417.1289682029448



Visual feedback: Both MI and MSE did similar and appropriate registrations.



Image Registration: 141-1-2658 vs 141-1-2668, Scaling Factor: 10







MSE Image Registration: 141-1-2658 vs 141-1-2668, Iteration 65 Metric: 421.1983560491936



Visual feedback: **MSE** registration produced slightly better correspondence in the left tuberosity.



Image Registration: 148-1-3551 vs 148-1-3557, Scaling Factor: 10





MSE Image Registration: 148-1-3551 vs 148-1-3557, Iteration 12 Metric: 296.7339329343426

[Reference - Transformed] (mmHg)



Visual feedback: Both MI and MSE did similar and appropriate registrations.



Image Registration: 145-1-2811 vs 145-1-1449, Scaling Factor: 10





MSE Image Registration: 145-1-2811 vs 145-1-1449, Iteration 23 Metric: 193.98973170359204



Visual feedback: **MSE** produced slightly better correspondence in tuberosities and top buttocks.



Image Registration: 185-1-1610 vs 185-1-1620, Scaling Factor: 10





MSE Image Registration: 185-1-1610 vs 185-1-1620, Iteration 29 Metric: 155.58457493703472

[Reference - Transformed] (mmHg)



Visual feedback: Both MI and MSE did similar and appropriate registrations.

75

50

25

 $\overline{0}$ 

 $-25$ 

 $-50$ 

 $-75$ 

300





Image Registration: 130-1-232 vs 130-1-242, Scaling Factor: 10





MSE Image Registration: 130-1-232 vs 130-1-242, Iteration 33 Metric: 246.93081385073114

[Reference - Transformed] (mmHg)



Visual feedback: Both MI and MSE did similar and appropriate registrations.

150

100

50

 $\mathsf 0$ 

 $-50$ 

 $-100$ 

 $-150$ 



Image Registration: 164-3-3886 vs 164-3-3896, Scaling Factor: 10









MSE Image Registration: 164-3-3886 vs 164-3-3896, Iteration 22 Metric: 1028.0708733939682





Visual feedback: **MSE** registration produced better correspondence in tuberosities and legs.



Image Registration: 182-1-2048 vs 182-1-2058, Scaling Factor: 10









MSE Image Registration: 182-1-2048 vs 182-1-2058, Iteration 15 Metric: 455.7476465676757





Visual feedback: **MSE** produced better correspondence in tuberosities, legs, and top buttocks.



Image Registration: 174-3-958 vs 174-3-970, Scaling Factor: 10





MSE Image Registration: 174-3-958 vs 174-3-970, Iteration 119 Metric: 856.9876533029358

[Reference - Transformed] (mmHg)



Visual feedback: While neither MI nor MSE produced a successful registration, MI is better.





Image Registration: 129-2-1842 vs 129-2-1852, Scaling Factor: 10









MSE Image Registration: 129-2-1842 vs 129-2-1852, Iteration 11 Metric: 301.51857126233944





Visual feedback: Both MI and MSE did similar and appropriate registrations.





Image Registration: 124-1-705 vs 124-1-719, Scaling Factor: 10



 $\mathbf 0$ 

 $\pmb{0}$ 

[Reference - Transformed] (mmHg)



MSE Image Registration: 124-1-705 vs 124-1-719, Iteration 20 Metric: 196.04343936230703





Visual feedback: Both MI and MSE did similar and appropriate registrations.



Image Registration: 112-2-1696 vs 112-2-1708, Scaling Factor: 10





[Reference - Transformed] (mmHg)



MSE Image Registration: 112-2-1696 vs 112-2-1708, Iteration 13 Metric: 330.35419711771317





Visual feedback: Both MI and MSE did similar and appropriate registrations.



Image Registration: 169-2-1993 vs 169-2-2009, Scaling Factor: 10



[Reference - Transformed] (mmHg)



MSE Image Registration: 169-2-1993 vs 169-2-2009, Iteration 7 Metric: 813.4337766317217







Image Registration: 181-1-3436 vs 181-1-3446, Scaling Factor: 10









MSE Image Registration: 181-1-3436 vs 181-1-3446, Iteration 21 Metric: 392.8030835469672





Visual feedback: Both MI and MSE did similar and appropriate registrations.



Image Registration: 110-2-1065 vs 110-2-1073, Scaling Factor: 10









MSE Image Registration: 110-2-1065 vs 110-2-1073, Iteration 17 Metric: 558.0103395043798





Visual feedback: Both MI and MSE did similar and appropriate registrations.



Image Registration: 123-1-2504 vs 123-1-2524, Scaling Factor: 10







MSE Image Registration: 123-1-2504 vs 123-1-2524, Iteration 39 Metric: 147.92235715335485





Visual feedback: Both MI and MSE did similar and appropriate registrations.



Image Registration: 132-1-1990 vs 132-1-2002, Scaling Factor: 10







MSE Image Registration: 132-1-1990 vs 132-1-2002, Iteration 63 Metric: 134.62633995980786





Visual feedback: Both MI and MSE did similar and appropriate registrations.



Image Registration: 183-3-2335 vs 183-3-2342, Scaling Factor: 10



 $\pmb{0}$ 

[Reference - Transformed] (mmHg)



MSE Image Registration: 183-3-2335 vs 183-3-2342, Iteration 19 Metric: 108.9091894101245



Visual feedback: Both MI and MSE did similar and appropriate registrations.

Appendix R

Case Study: Sequential Registration and Comparative Results









